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# Regularizing parameter estimation for Poisson noisy image restoration\*

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## ABSTRACT

Deblurring images corrupted by Poisson noise is a challenging process which has devoted much research in many applications such as astronomical or biological imaging. This problem, among others, is an ill-posed problem which can be regularized by adding knowledge on the solution. Several methods have therefore promoted explicit prior on the image, coming along with a regularizing parameter to moderate the weight of this prior. Unfortunately, in the domain of Poisson deconvolution, only a few number of methods have been proposed to select this regularizing parameter which is most of the time set manually such that it gives the best visual results. In this paper, we focus on the use of  $l^1$ -norm prior and present two methods to select the regularizing parameter. We show some comparisons on synthetic data using classical image fidelity measures.

## 1. INTRODUCTION

Deblurring noisy Poisson images is a task that has recently been subject of an increasingly amount of works in many areas [1, 2, 5, 6, 7, 10]. It could be modeled as follows. If we consider a discrete version of a scene  $x \in \mathbb{R}^n$  ( $n$  being the number of pixels of the image) observed as an image  $y \in \mathbb{R}^n$  through an optical system with a Point Spread Function (PSF)  $h$  and corrupted by a Poisson noise process  $\mathcal{P}$ , then the image formation model can be written as:

$$y = \mathcal{P}(Hx + b), \quad (1)$$

where  $b \in \mathbb{R}^n, b \geq 0$  is a known constant modeling the background and  $H : \mathbb{R}^n \rightarrow \mathbb{R}^n$  stands for the matrix notation of the convolution of the PSF  $h$ . We assume moreover that  $Hx \geq 0 \forall x \geq 0$  and that  $H$  is normalized:

$$H\xi_n = \xi_n, \quad (2)$$

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where  $\xi_n$  is a  $n$ -size vector whose components are all 1.

Using a bayesian approach, we want to retrieve the image  $x$  which maximizes the likelihood probability of (1). This probability can be expressed as:

$$p(y|x) = \prod_{i \in \Omega} \left( \frac{[(Hx + b)_i]^{y_i} \exp[-(Hx + b)_i]}{y_i!} \right), \quad (3)$$

where  $\Omega$  is a 2D finite discrete lattice holding  $n$  pixels. Maximizing (3) with respect to  $x$  is equivalent to minimize  $-\log p(y|x)$  that is to minimize (up to a constant):

$$J_L(x, y) = \sum_{i \in \Omega} (Hx + b)_i - y_i + y_i \log(y_i) - y_i \log[(Hx + b)_i]. \quad (4)$$

The function  $J_L$  is convex with respect to  $x$  and can be minimized using an iterative algorithm such as the well-known Richardson-Lucy (RL) algorithm [9] also known as the Expectation Maximization (EM) algorithm in the biomedical imaging community [4, 8].

As the inverse problem is ill-posed, the noise is amplified on such solution and many works promote the introduction of explicit prior on the solution to regularize the inverse problem. Common priors are defined upon the  $l^1$ -norm of a linear transform  $W : \mathbb{R}^n \rightarrow \mathbb{R}^p$  ( $p \geq n$ ) to promote the regularity of the image  $x$  in some domain such as Total Variation (TV) [5] or wavelet frame transforms ([6, 10] and references therein). Therefore, by maximizing the a posteriori probability  $p(x|y) = p(y|x) \frac{p(x)}{p(y)}$ , where  $p(x)$  is the prior model on the object given by  $p(x) = \alpha \exp[-\tau J_R(x)]$  ( $\alpha$  is a normalization constant and  $J_R(x) = \|Wx\|_1$  is the regularizing term), one gets that the problem of deblurring Poisson noisy images can be written as:

$$x_\tau^* = \arg \min_{x \in \mathbb{R}^n, x \geq 0} \{J(x, y) := J_L(x, y) + \tau J_R(x)\}, \quad (5)$$

$\tau$  being the regularizing parameter. This function is a proper, lower-semi continuous, and convex function. If the intersection of the null spaces of  $H$  and  $W$  is zero then  $J$  is coercive and a solution  $x_\tau^*$  exists [7].

In most of the Poisson deconvolution methods proposed in the literature, the regularizing parameter  $\tau$  has to be chosen such that it gives the best visual results. However, the interpretation of an image may be difficult in biology for ex-

ample, specially as we do not have the ground truth. Several estimators of the distance to the unknown true image  $x$  have then been proposed. We present two of these estimators in the next section and show how to improve their results by taking advantage of the properties of the Poisson noise.

## 2. REGULARIZING PARAMETER ESTIMATION

### 2.1 Gaussian discrepancy principle

The regularizing parameter  $\tau$  in (5) is, most of the time, estimated using methods designed for Gaussian noise. Recently, [1] developed a method to select the regularizing parameter using this kind of approximation. They wrote that the Poisson noise could be modeled as an additive Gaussian noise, that is:

$$y = \mathcal{P}(Hx + b) \simeq (Hx + b) + e, \quad (6)$$

where  $e$  is an additive Gaussian noise with mean 0 and multidimensional variance  $y$ . If one set (here, the division must be understood component-wise):

$$r(x) = (Hx - (y - b)) / \sqrt{y}, \quad (7)$$

then  $r(x)$  is a Gaussian random variable with mean 0 and variance  $I$  (the  $n$ -size identity matrix). In this case, a standard result gives:

$$\|r(x)\|_2^2 \sim \chi^2(n), \quad (8)$$

where  $\chi^2(n)$  is the chi-square distribution with  $n$  degree of freedom which has a mean equal to  $n$ . Therefore:

$$E(\|r(x)\|_2^2) = n. \quad (9)$$

Let  $x_\tau^*$  be one solution of (5) for a given  $\tau$ , the authors of [1] have also shown that a good value of  $\tau$  should verify:

$$\|r(x_\tau^*)\|_2^2 = E(\|r(x)\|_2^2). \quad (10)$$

Therefore, following this last equation and (9), [1] proposed to select the regularizing parameter  $\tau$  such that it verifies:

$$\tau_{opt} = \arg \min_{\tau \in \mathbb{R}^+} \{\Psi_y(x_\tau^*) - 1\}^2, \quad (11)$$

where:

$$\Psi_y(x) = \frac{1}{n} \|r(x)\|_2^2 = \frac{1}{n} \left\| (Hx - (y - b)) / \sqrt{Hx + b} \right\|_2^2 \quad (12)$$

Note that  $y$  in (7) has been actually replaced by  $Hx + b$  as it seems to give better results [1].

### 2.2 Poisson discrepancy principle

Although the above Gaussian approximation is well established for high intensity image, it does not work for applications where images have low intensities like astronomy or biology. One then need to really take into account the Poisson statistics of the noise and to the best of our knowledge, only the recent work of [2] has been focussed on this aspect. The authors of [2] proposed a discrepancy principle for Poisson noise that we recall in the following lines. Let us consider that  $Y_\lambda \in \mathbb{R}$  is a Poisson random variable with mean  $\lambda$  (which actually stands for  $(Hx + b)_i$  for some  $i$  in (1)):

$$Y_\lambda = \mathcal{P}(\lambda). \quad (13)$$

They set:

$$F(\lambda, Y_\lambda) = 2 \left( Y_\lambda \log \left( \frac{Y_\lambda}{\lambda} \right) + \lambda - Y_\lambda \right), \quad (14)$$

and showed that, by taking the expected value of this function, one get, for large  $\lambda$ :

$$E(F(\lambda, Y_\lambda)) = 1 + O\left(\frac{1}{\lambda}\right). \quad (15)$$

So, back to (1), if the true image  $x$  has sufficient high intensities, it is reasonable to write that:

$$E(J_L(x, y)) = \frac{1}{2} \sum_{i \in \Omega} E(F(x_i, y_i)) \simeq \frac{1}{2} \text{card}(\Omega) = \frac{n}{2}, \quad (16)$$

and thus, the regularizing parameter  $\tau$  should be chosen as:

$$\tau_{opt} = \arg \min_{\tau \in \mathbb{R}^+} \{\Upsilon_y(x_\tau^*) - 1\}^2, \quad (17)$$

where:

$$\begin{aligned} \Upsilon_y(x) &= \frac{2}{n} J_L(x, y) \\ &= \frac{2}{n} \sum_{i \in \Omega} (Hx + b)_i - y_i + y_i \log(y_i) - y_i \log[(Hx + b)_i]. \end{aligned} \quad (18)$$

### 2.3 Comparisons of these two estimators

In this section, we compare the two previous estimators on the synthetic images (a) and (b) of the figure 1. For each simulation, the regularizing term is the TV regularization and the PSF is a  $7 \times 7$  Gaussian kernel (in other words, 95% of the Gaussian is holded in a square of size  $7 \times 7$  pixels). The value of the estimated regularizing parameter  $\tau$  is compared to the value given by the minimization of the I-Divergence [3]:

$$\tau_{div} = \arg \min_{\tau \in \mathbb{R}^+} \left\{ \sum_{i \in \Omega} x_i \log \left( \frac{x_i}{x_\tau^*} \right) - (x_i - x_\tau^*) \right\}, \quad (19)$$

and by the minimization of the Mean Square Error (MSE) as it is usually done:

$$\tau_{mse} = \arg \min_{\tau \in \mathbb{R}^+} \left\{ \frac{1}{n} \|x - x_\tau^*\|_2^2 \right\}. \quad (20)$$

where  $x$  is the given synthetic original image. Figure 2 and table 1 show the estimation of the regularizing parameter for the image (a). This image is a high intensity image with a constant background  $b = 1$ . On this image, the estimators (11) and (17) give values which are actually very close to the value given by the minimization of the I-Divergence (see table 1). They are a little higher than the value given by the minimization the MSE, this is however still acceptable as the obtained restored images only slightly differ.

Figure 3 and table 1 show the estimation of the regularizing parameter for the image (b). This image is also a high intensities image but with a null background which is a frequent property of biomedical and astrophysics images for example. In this configuration, the constraint  $x \geq 0$  in the restoration algorithm (5) is changed to  $x \geq \epsilon$ , where  $\epsilon$  is a small constant, to prevent numerical issues in the computation of the estimators (11) and (17). We will show in the next section

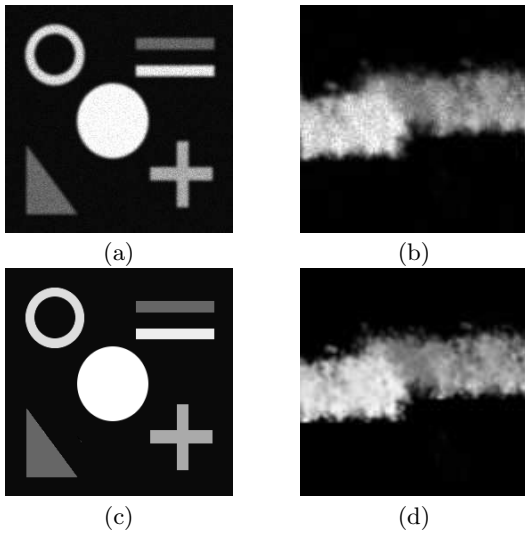


Figure 1: Synthetic 2D images. The first row is the observed images (Poisson noise and blur) while the second row is the original images.

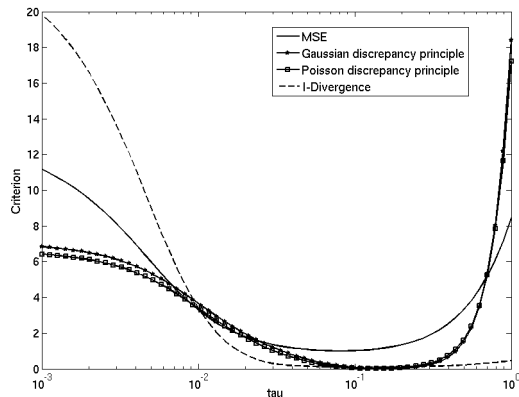


Figure 2: Estimation of  $\tau$  on the image (a) of the figure 1

how to deal with these images with still keeping the constraint  $x \geq 0$  in the restoration algorithm. On this image, estimators (17) and (11) fail to give acceptable estimation of the regularizing parameter (see table 1). The error of estimation is very important and this could be explained by the fact that this image actually contains many zero-valued pixels (about 65% of the whole number of pixels) and that the estimators (17) and (11) do not take into account this kind of property. We propose in the next section a modification of these estimators to address this issue.

### 3. PROPOSED METHOD

We show in the next lines that we can improve the accuracy of these estimators by taking into account the properties of the application. For example, images in biology often contain many pixels where the number of collected photons is zero. For this reason, we propose to split the domain  $\Omega$  in several sub-domains and to compute each estimator on

Criterion \ Image	(a)	(b)
Gaussian discrepancy principle (11)	0.153	0.626
Poisson discrepancy principle (17)	0.122	0.703
MSE (20)	0.076	0.026
I-Divergence (19)	0.121	0.108

Table 1: Values of the estimated regularizing parameter on images (a) and (b) of the figure 1 for the estimators (11), (17) and comparison to measures (20) and (19).

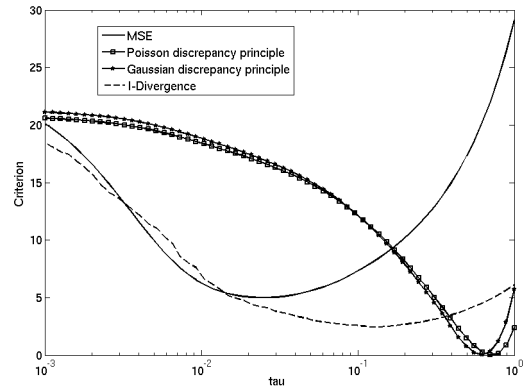


Figure 3: Estimation of  $\tau$  on the image (b) of the figure 1

these sub-domains.

### 3.1 Notations

We recall that our model writes:

$$y = \mathcal{P}(\lambda), \quad (21)$$

with  $\lambda = Hx + b$ . Let us define the index sets  $\Theta_1 = \{i \in \Omega | y_i > 0\}$  and  $\Theta_0 = \{i \in \Omega | y_i = 0\}$ . Same definitions are applied to  $\lambda$  and give the index sets  $\Lambda_1 = \{i \in \Omega | \lambda_i > 0\}$ ,  $\Lambda_0 = \{i \in \Omega | \lambda_i = 0\}$ . We have  $\Omega = \Theta_1 \cup \Theta_0 = \Lambda_1 \cup \Lambda_0$ . Let us also define any combination of these index sets :

- $S_0 = \Theta_0 \cap \Lambda_0$ ,
- $S_1 = \Theta_0 \cap \Lambda_1$ ,
- $S_2 = \Theta_1 \cap \Lambda_0$ ,
- $S_3 = \Theta_1 \cap \Lambda_1$ .

Firstly remark that  $S_2$  is empty by definition (21). Secondly, note that these sets do not overlap and that we also have  $\Omega = S_0 \cup S_1 \cup S_3$ .

### 3.2 Gaussian approximation

We first consider the Gaussian approximation (6). We recall that the authors of [1] have proposed to write:

$$y = \mathcal{P}(Hx + b) \simeq (Hx + b) + e, \quad (22)$$

with:

$$e = (e_i)_{i \in \Omega} \text{ and } e_i \sim \mathcal{N}(0, \sqrt{y_i}) \quad \forall i \in \Omega. \quad (23)$$

However, we may use the decomposition of  $\Omega$  over the index sets  $S_i$ ,  $i \in \{0, 1, 3\}$  to refine the previous assumption:

- $e_i = 0 \quad \forall i \in S_0$  by definition (1).
- On the domain  $S_1$ ,  $e_i$  is fully determinist and given by  $e_i = -(Hx + b)_i$  which unfortunately needs to be estimated from real data as the true image  $x$  is unknown.
- On  $S_3$ , the previous assumption is valid and writes  $e_i \sim \mathcal{N}(0, \sqrt{y_i})$ .

Observe that  $S_1$  actually represents elements with very low intensities which give zero-valued observed pixels and mostly appears on the object borders in the image, due to the convolution effect which spreads these borders giving very small intensities. Values of  $e_i$  on this domain should therefore be very small. Not taking into account this domain should not increase the estimation error too much for images with sufficient “large” objects as the number of disregarded components  $\text{card}(S_1)$  is very small with respect to  $\text{card}(S_3)$ . Note that this assumption is however false for images containing only thin structures like points or filaments. For all other images, we propose consequently to write that:

$$e = (e_i)_{i \in \Omega} \text{ and } \begin{cases} e_i \sim \mathcal{N}(0, \sqrt{y_i}) & \forall i \in S_3 \\ e_i = 0 & \text{otherwise} \end{cases}. \quad (24)$$

In this case  $r(x) \sim \mathcal{N}(0, \Sigma)$ :

$$\Sigma = (\Sigma_i)_{i \in \Omega} \text{ with } \Sigma_i = \begin{cases} \sqrt{y_i} & \text{if } i \in S_3 \\ 0 & \text{otherwise} \end{cases}, \quad (25)$$

such that we have:

$$r(x) = \begin{cases} (Hx - (y - b)) / \sqrt{y} & \text{if } i \in S_3 \\ 0 & \text{otherwise} \end{cases}. \quad (26)$$

Consequently, we rewrite (8) as:

$$\|r(x)\|_2^2 \sim \chi^2(\text{card}(S_3)) = \chi^2(\text{card}(\Theta_1)) = \chi^2(m), \quad (27)$$

where  $m = \text{card}(\Theta_1)$  actually represents the number of strictly positive pixels in the observation  $y$ . Following this last equation, we propose to select the regularizing parameter  $\tau$  such that it verifies:

$$\tau_{opt} = \arg \min_{\tau \in \mathbb{R}^+} \left\{ \tilde{\Psi}_y(x_\tau^*) - 1 \right\}^2, \quad (28)$$

where:

$$\tilde{\Psi}_y(x) = \frac{1}{m} \left\| (Hx - (y - b)) / \sqrt{Hx + b} \right\|_2^2. \quad (29)$$

Note that due to the splitting of the domain, we can maintain the constraint  $x \geq 0$  in the restoration algorithm as we compute the estimator only for strictly positive pixels values. We see in the next section how to apply the same idea to the Poisson discrepancy principle.

### 3.3 Poisson discrepancy principle

The authors of [2] have computed their estimator on the whole index set  $\Omega$  and have found that :

$$E(J_L(x, y)) = \frac{1}{2} \sum_{i \in \Omega} E(F(x_i, y_i)) \simeq \frac{1}{2} \text{card}(\Omega) = \frac{n}{2} \quad (30)$$

As previously, we may use the decomposition of  $\Omega$  over the index sets  $S_i$ ,  $i \in \{0, 1, 3\}$  to refine the computation of the expected value. Indeed :

$$E(J_L(x, y)) = \frac{1}{2} \sum_{i \in \Omega} E(F(x_i, y_i)) = \frac{1}{2} \left( \sum_{i \in S_0} E(F(x_i, y_i)) + \sum_{i \in S_1} E(F(x_i, y_i)) + \sum_{i \in S_3} E(F(x_i, y_i)) \right) = E_0 + E_1 + E_3. \quad (31)$$

We now detail the computation of each term  $E_i$ ,  $i \in \{0, 1, 3\}$ :

- $E_0 = 0$  as  $F(x_i, y_i) = 0$  on the domain  $S_0$ .
- On the domain  $S_1$ , we have  $F(x_i, y_i) = (Hx + b)_i$  and thus  $E_1$  is given by:

$$E_1 = \frac{1}{2} \sum_{i \in S_1} (Hx + b)_i \triangleq \frac{\gamma}{2}, \quad (32)$$

which also needs to be estimated.

- And finally  $E_3$  is simply given by the result (16):

$$E_3 = \frac{1}{2} \sum_{i \in S_3} E(F(x_i, y_i)) \simeq \frac{1}{2} \text{card}(S_3) = \frac{1}{2} \text{card}(\Theta_1) = \frac{m}{2} \quad (33)$$

Therefore, we have:

$$E(J_L(x, y)) \simeq \frac{m + \gamma}{2} \quad (34)$$

Following the same approximation than the one in the section 3.2, we propose to disregard the effect of  $\gamma$  in front of  $m$  and propose:

$$E(J_L(x, y)) \simeq \frac{m}{2} \quad (35)$$

Finally, the regularizing parameter should be chosen as:

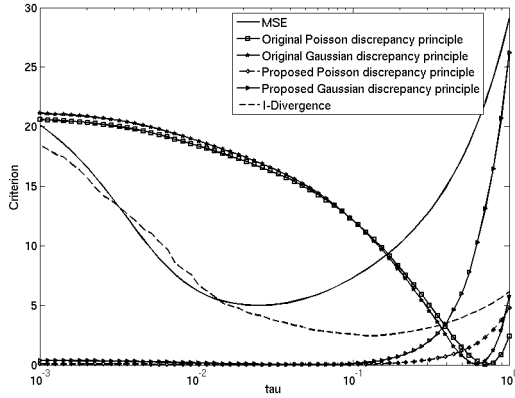
$$\tau_{opt} = \arg \min_{\tau \in \mathbb{R}^+} \left\{ \tilde{\Upsilon}_y(x_\tau^*) - 1 \right\}^2, \quad (36)$$

where:

$$\tilde{\Upsilon}_y(x) = \frac{2}{m} \sum_{i \in \Omega} (Hx + b)_i - y_i + y_i \log(y_i) - y_i \log[(Hx + b)_i]. \quad (37)$$

### 3.4 Results

Figure 4 and table 2 show the estimation of the modified estimators for the image (b) of the figure 1. Values are compared to original estimators [1] and [2]. We see that the estimation error has been strongly reduced using the proposed estimators. On this image, estimated values are now in between the values given by the MSE and the I-Divergence.



**Figure 4: Estimation of  $\tau$  on the image (b) of the figure 1**

Gaussian discrepancy principle (11)	0.626
Poisson discrepancy principle (17)	0.703
Proposed Gaussian discrepancy principle (28)	0.042
Proposed Poisson discrepancy principle (36)	0.037
MSE (20)	0.026
I-Divergence (19)	0.108

**Table 2: Values of the estimated regularizing parameter on image (b) of the figure 1 for the estimators (11), (17), the proposed modifications (28), (36) and comparison to measures (20) and (19).**

## 4. CONCLUSIONS

We have proposed two estimators to select the regularizing parameter for the deconvolution of images corrupted by blur and Poisson noise. Values given by these estimators have been compared to classical image fidelity measures and have shown promising results. Future works will be focused on the accuracy of the estimators and on the validity of the approximations made for images containing only thin objects like points or filaments.

## 5. ACKNOWLEDGMENTS

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