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Taous-Meriem Laleg, Claire Médigue, François Cottin, Michel Sorine. Arterial blood pressure analysis based on scattering transform II. 29th Annual International Conference Sciences and Technologies for Health - EMBC 2007, IEEE Engineering in Medicine and Biology Society, Aug 2007, Lyon / France. inria-00139529v1

HAL Id: inria-00139529

<https://inria.hal.science/inria-00139529v1>

Submitted on 1 Apr 2007 (v1), last revised 20 Jun 2007 (v2)

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Arterial blood pressure analysis based on scattering transform II

Taous-Meriem Laleg, Claire Médigue, François Cottin and Michel Sorine

Abstract—"Arterial blood pressure analysis based on scattering transform I" introduces a new method based on the scattering transform for a one dimensional Schrödinger equation to reconstruct the arterial blood pressure waves and separate its systolic and diastolic parts. In this article, we propose to analyse the parameters computed from this technique in different clinical and physiological conditions. Two cases are considered : moderate chronic heart failure and high fit triathletes. The variability of these new parameters is compared to the variability of classical blood pressure indexes. Promising results are obtained.

I. INTRODUCTION

The analysis of mean values and beat-to-beat variability of cardiovascular (CV) time series has been widely used as a non invasive approach to study the control of the autonomic nervous system (ANS) on the CV function [1], [8]. Two main frequency bands are related to autonomic activity : an high frequency (HF), related to breathing activity, and a low frequency (LF), around 0.1Hz . The usual CV time series are the cardiac period (RR interval) or the systolic period (SP), the systolic and diastolic pressures (SBP& DBP). Standard measures are mean levels and global variability, spectral and time-frequency analysis such as the smoothed pseudo Wigner-Ville distribution (SPWVD), local harmonic analysis (the Complex Demodulation) [10] and the spectral RR/SBP gain. The general functioning of the ANS is relatively well described by these parameters in obvious physiological or pathological situations. But the early diagnosis of a degradation/improvement in pathological or physiological cases require very discriminating indexes.

In a recent article [7], an original Scattering-Based Signal Analysis (SBSA) method has been proposed. The latter has been applied in [6] for reconstructing the Arterial Blood Pressure (ABP) waves and separating its systolic and diastolic parts, an application that can be of a great interest. This approach is based on the scattering transform and consists in solving the spectral problem of a one dimensional Schrödinger equation [2], [3], [4] with a potential depending linearly upon the ABP signal [7]. This potential is then expressed with the discrete spectrum including negative eigenvalues and corresponds in fact to the interacting components of an N-soliton [5], [11].

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The aim of this study is to compare the SBSA parameters to classical CV parameters, and this, in two non obvious situations : discrimination between healthy subjects and moderate Chronic Heart Failure (CHF) patients for the pathological situation ; discrimination between two states for the physiological situation : High Fit Triathletes (HFT) before and after training. On top of classical variabilities (global, HF, LF), a third very high frequency (VHF) activity, near beat-to-beat variability was studied as its amplitude appears non negligible in the SBSA parameters.

In the next section, we present the experimental protocol. Then in section III, we introduce the SBSA parameters that will be analyzed. The results of the analysis are presented in section IV following by a discussion in section V. Finally, a conclusion summarizes the study.

II. EXPERIMENTAL PROTOCOL

The two pathological and physiological studies presented similar contexts : subjects were quiet, in supine position, under paced-breathing conditions. As breathing has a great influence on cardiovascular variability, this protocol presents the advantage to limit breathing in a narrow frequency band, homogeneous for all subjects. Non invasive blood pressure, sampled at 500Hz , was continuously recorded at the finger with a photoplethysmographic transducer (Finapres/Finometer) [13]. One/two minutes periods were selected in each recording, for computing mean levels and global variability (estimated by standard-deviation) from the classical parameters (SP, SBP and DBP) and the SBSA parameters that will be introduced in the next section. Results were expressed as means and Standard Error to Mean (SEM). Statistical analysis was made with non parametric tests : Mann-Whitney test for unpaired comparisons, Wilcoxon test for paired comparisons. For significance * : $P < 0.05$; ** : $P < 0.01$.

a) *CHF patients versus healthy subjects*: The study included nine moderate CHF patients, NYHA class II/III, and nine healthy control subjects, from 35 to 50 years old. For each subject, mean values and global variability were computed over a period of one minute, under 0.15Hz paced-breathing. The two groups were compared with the Mann-Whitney test.

b) *HFT before and after training*: The study included eight junior HFT, from 15 to 19 years old, recorded before training and five months later, after training, during competition. For each subject, mean values and global variability were computed over a period of two minutes under 0.25Hz paced-breathing, before and after training. On top of mean values and global variability, the amplitudes in LF,

$[0.03 - 0.15]Hz$, HF, $0.25Hz$, centered around the breathing frequency, and VHF, $[0.3 - 0.6]Hz$ were also computed using the SPWVD. The two situations were then compared with the Wilcoxon test.

III. NEW BLOOD PRESSURE PARAMETERS

We introduce here the SBSA parameters that we propose to analyse. For more details about the SBSA method, the reader can refer to [6], [7]. We recall that the main idea in the SBSA approach consists in solving the spectral problem for a one dimensional Schrödinger equation :

$$-\frac{\partial^2 \psi}{\partial t^2} + V\psi = \lambda \psi, \quad (1)$$

where λ and ψ are respectively the eigenvalues and the eigenfunctions of the Schrödinger operator. V is the Schrödinger potential given by :

$$V(\chi) = -\chi P(t), \quad (2)$$

χ is a positive parameter to determine and $P(t)$ the ABP signal. The idea is then to find χ that enables us to approximate the potential with its discrete spectrum only including negative eigenvalues. The ABP signal is then approximated by :

$$\hat{P}(t) = 4\chi^{-1} \sum_{n=1}^N \kappa_n \psi_n^2. \quad (3)$$

where $\lambda_n = -\kappa_n^2$, $n = 1, \dots, N$ are the N negative eigenvalues and ψ_n , $n = 1 \dots, N$ the associated L^2 -normalized eigenfunctions. Each component $4\kappa_n \psi_n^2$ of the previous sum refers to a one soliton [5], [7]. Only 5-10 components are sufficient for a good reconstruction of the ABP [7].

Therefore, the first parameters that seem to be interesting to analyse are the negative eigenvalues. In this study, we restrict the analysis on the two first negative eigenvalues. However, there are other parameters that can contain meaningful physiological information for example the conserved quantities (or invariants), related to an N-soliton solution of a Korteweg-de Vries equation [5], [9]. We consider here the two first invariants which are related to the κ_n , $n = 1, \dots, N$ by the following expressions :

$$INV_1 = 4\chi^{-1} \sum_{n=1}^N \kappa_n, \quad INV_2 = \frac{16}{3}\chi^{-2} \sum_{n=1}^N \kappa_n^3. \quad (4)$$

We precise that INV_1 represents the mean ABP.

As introduced in [6], [7], the SBSA technique can be used to separate the systolic and diastolic parts of the ABP. For each phase, we can define the corresponding invariants. Then, the two first systolic invariants are :

$$INVS_1 = 4\chi^{-1} \sum_{n=1}^2 \kappa_n, \quad INVS_2 = \frac{16}{3}\chi^{-2} \sum_{n=1}^2 \kappa_n^3, \quad (5)$$

and the two first diastolic invariants are given by :

$$INVD_1 = INV_1 - INVS_1, \quad INVD_2 = INV_2 - INVS_2. \quad (6)$$

As an illustration, fig. 1 and fig. 2 show time series of the classical and SBSA parameters, extracted from our two

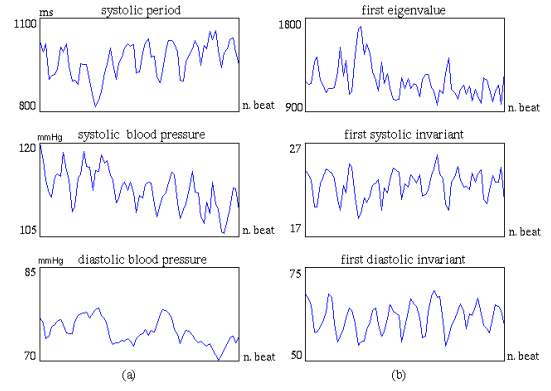


Fig. 1. Time series of ABP parameters in a healthy subject, under $0.15Hz$ paced breathing, during one minute analysis. Direct classical parameters in (a) and three of the SBSA parameters in (b).

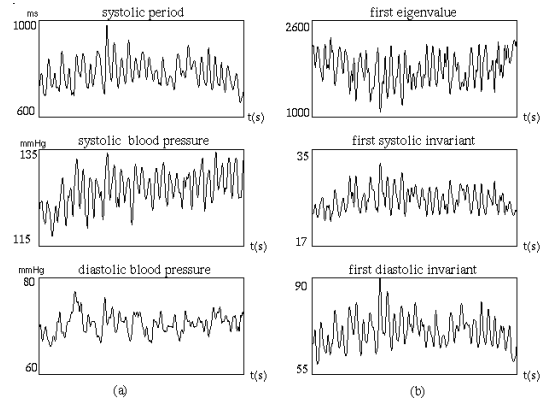


Fig. 2. Time series of ABP parameters in a healthy subject, under $0.25Hz$ paced breathing, during two minutes analysis. Direct classical parameters in (a) and three of the SBSA parameters in (b).

studies. The breathing influence appears clearly in the two cases. Fig. 3 points out the VHF, particularly important on the SBSA parameters, such as on the eigenvalues. The latter are effected by any change in the ABP waveform.

IV. RESULTS

A. CHF patients versus healthy subjects

Mean levels of the parameters are not significantly different between control and CHF subjects. However, while the global variability is not significant for the classical parameters, it is significantly lower for the SBSA parameters (Table I). Two representative time series of λ_1 , $INVS_1$ and $INVD_1$ in a control and a CHF subjects are shown in fig. 4.

B. HFT subjects before and after training

As shown in Table II, mean levels of the parameters are not significantly different between the two physiological situations : before and after training. The global variability of the parameters is also not significantly different except for the first normalized systolic and diastolic invariants (normalized by the total variability of the first invariant). This result led us to a deeper analysis of the systolic and diastolic invariants variability, by extracting HF, LF and VHF

TABLE I
MEAN LEVEL AND GLOBAL VARIABILITY OF THE ABP PARAMETERS IN 9 HEALTHY AND CHF SUBJECTS.

ABP parameters	Mean level		Global variability	
	Healthy subjects	CHF patients	Healthy subjects	CHF patients
Systolic period	804 ± 31	887 ± 51	50.18 ± 9.244	25.00 ± 3.494
Systolic blood pressure	113.3 ± 4.9	111.8 ± 6.2	4.286 ± 0.549	3.254 ± 0.301
Diastolic blood pressure	65.6 ± 4.3	63.9 ± 4.1	2.110 ± 0.422	1.348 ± 0.175
First eigenvalue	1898 ± 149	1683 ± 265	256.4 ± 44.30	140.2 ± 16.91 **
Second eigenvalue	1556 ± 114	1343 ± 227	214.0 ± 37.53	114.0 ± 15.66 **
First invariant	65.5 ± 4.3	68.5 ± 4.5	4.778 ± 0.649	2.492 ± 0.262 **
Second invariant	5648 ± 618	5670 ± 648	534.9 ± 95.7	283.7 ± 30.08 **
First systolic invariant	17.7 ± 1.1	18.7 ± 1.3	1.447 ± 0.192	0.916 ± 0.064 **
Second systolic invariant	2196 ± 229	2253 ± 273	230.3 ± 41.26	136.7 ± 12.06 *
First diastolic invariant	47.4 ± 3	47.9 ± 3.3	3.424 ± 0.47	1.940 ± 0.203 **
Second diastolic invariant	3255 ± 324	3362 ± 384	307.5 ± 56.59	175.0 ± 25.31 **

Data are expressed as means and SEM, * : $P < 0.05$; ** : $P < 0.01$.

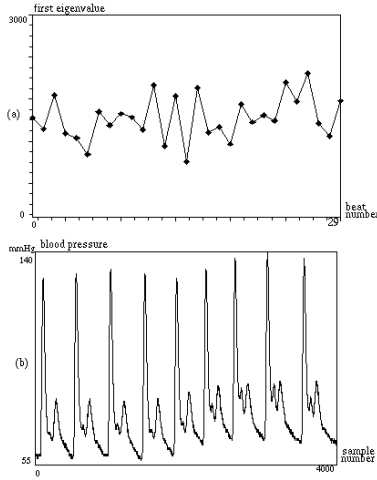


Fig. 3. (a) First eigenvalue time series of a healthy subjects under 0.25Hz paced-breathing during 29 beats. The signal exhibits a beat-to-beat variability, twice faster than the breathing rate. (b) A zoom on a few beats shows morphological changes in the blood pressure signal.

components. A significant diminution appears only for the VHF amplitude (Table III, fig. 5).

V. DISCUSSION

A. CHF patients versus healthy subjects

The results obtained in this study agree with previous ones obtained with the same data base [8] : lower variability in CHF patients. In the previous study, the significance depended on RR and SBP together. RR global variability, LF-RR, HF-SBP were significant with $P < 0.05$; the spectral RR/SBP gain alone was significant with $P < 0.01$. However, it needs a coherence function greater than 0.5 to verify linearity between RR and SBP, and 2 minutes analysis periods. These constraints limited the number of available data (seven/six subjects in the previous study versus nine/nine in the present study). In this study, near all the first and second SBSA parameters of the ABP were significant with $p < 0.01$. So, the SBSA parameters present the advantage of getting very significant differences between healthy and moderate CHF subjects ; and this, with such a simple measure as global variability (standard-deviation) and on a short analysis period

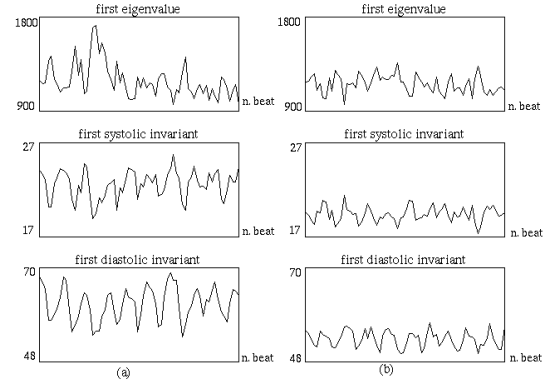


Fig. 4. Time series of the first blood pressure eigenvalues and invariants in, (a) a healthy and (b) a CHF subjects . The lower global variability in CHF is representative of the significant statistical difference over these two groups.

(one minute). This last point is important in the case of CHF, where patients present a lot of extra-systoles.

B. HFT patients before and after training

As the only significant difference on the first computations (means and global variability) depended on the global variability of the first systolic and diastolic normalized invariants, we were interested in their HF, LF and VHF components. Interestingly, only the VHF amplitude was significantly lower after training. A diminution in the beat-to-beat variability measured by the square root of the mean of the summed squared differences between adjacent beat-to-beat intervals in overtraining subjects was described in RR but not in the ABP [1]. A previous HF and LF analysis on RR-interval on the same data studied here (not published), as well as HF, LF, VHF on SP and SBP classical parameters did not show any significant differences. The aim of this kind of studies is to assess the quality of training, to avoid overtraining and to improve CV adjustment to exercise [1], [12].

VI. CONCLUSION

In the two cases, CHF and HFT training, early indexes to diagnosis and follow pathological and physiological situations is of a great interest. New parameters have been introduced in this study to analyse the ABP signal. The results on

TABLE II
MEAN LEVEL AND GLOBAL VARIABILITY OF THE ABP PARAMETERS IN 8 JUNIOR HFT BEFORE AND AFTER TRAINING.

ABP parameters	Mean level		Global variability	
	Before training	After training	Before training	After training
Systolic period	886 ± 32	935 ± 46	69.67 ± 8.466	65.04 ± 4.962
Systolic blood pressure	124.2 ± 10.2	121.3 ± 5.3	5.460 ± 0.756	7.074 ± 0.929
Diastolic blood pressure	64.6 ± 5.9	51.2 ± 3.8	3.385 ± 0.526	3.538 ± 0.429
First eigenvalue	1524 ± 97	1487 ± 158	259.0 ± 20.40	246.3 ± 28.99
Second eigenvalue	9810 ± 931	1161 ± 115	210.9 ± 20.81	178.9 ± 18.53
First invariant	91.0 ± 4.8	83.3 ± 4.6	8.104 ± 1.393	7.277 ± 0.654
Second invariant	9810 ± 931	7880 ± 703	1083.0 ± 249.0	912.0 ± 94.85
First systolic invariant	24.7 ± 1.2	22.9 ± 1.2	2.358 ± 0.340	2.160 ± 0.18
Second systolic invariant	3777 ± 303	3154 ± 257	434.6 ± 83.34	381.4 ± 38.68
First diastolic invariant	66.3 ± 3.6	60.3 ± 3.3	5.963 ± 1.038	5.315 ± 0.467
Second diastolic invariant	6032 ± 637	4725 ± 449	667.0 ± 165.6	544.5 ± 56.67
First systolic normalized invariant	0.272 ± 0.002	0.276 ± 0.001	8.80E + 04 ± 8.41E02	9.02E + 04 ± 7.52E02 *
Second systolic normalized invariant	0.388 ± 0.008	0.402 ± 0.005	9.51E + 04 ± 3.08E03	9.98E + 04 ± 3.15E03
First diastolic normalized invariant	0.728 ± 0.002	0.724 ± 0.001	8.80E + 04 ± 8.41E02	9.02E + 04 ± 7.52E02 *
Second diastolic normalized invariant	0.612 ± 0.008	0.598 ± 0.005	9.51E + 04 ± 3.08E03	9.98E + 04 ± 3.15E03

Data are expressed as means and SEM, * : $P < 0.05$.

TABLE III
VARIABILITY OF ABP INVARIANTS IN 3 FREQUENCY BANDS, BEFORE AND AFTER TRAINING IN 8 JUNIOR HFT.

Mean amplitude in	Before training	After training
HF		
First systolic invariant	2.132 ± 0.246	1.924 ± 0.2
Second systolic invariant	383.2 ± 54.94	305.4 ± 35.58
First diastolic invariant	5.202 ± 0.723	4.646 ± 0.441
Second diastolic invariant	529.9 ± 96.08	395.5 ± 39.72
LF		
First systolic invariant	1.838 ± 0.32	1.699 ± 0.192
Second systolic invariant	324.6 ± 61.01	317.9 ± 38.93
First diastolic invariant	4.679 ± 0.843	4.111 ± 0.513
Second diastolic invariant	502.0 ± 105.8	461.8 ± 59.07
VHF		
First systolic invariant	1.018 ± 0.048	0.814 ± 0.052*
Second systolic invariant	149.1 ± 11.54	105.2 ± 9.747*
First diastolic invariant	2.183 ± 0.234	1.555 ± 0.109*
Second diastolic invariant	166.7 ± 27.98	97.71 ± 9.367*

Data are expressed as means and SEM, * : $P < 0.05$.

the variability of these new ABP indexes are promising in particular which are related to their beat-to-beat variability. Moreover the SBSA parameters seem to contain meaningful physiological information, such as the first systolic invariant which could be proportional to the systolic ejection volume, difficult to estimate in a non invasive way.

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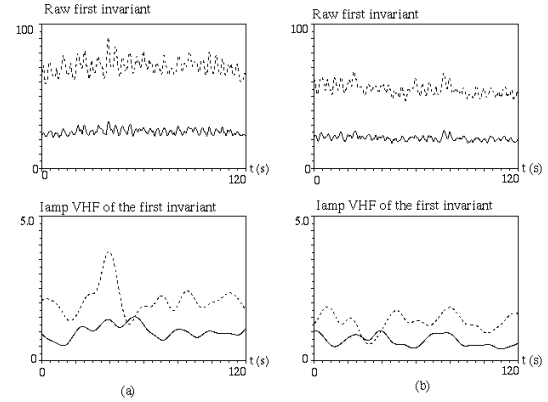


Fig. 5. First invariants of the ABP (top) and their VHF instantaneous amplitude (bottom) for a subject before (a) and after (b) training. Dotted lines stand for diastolic parameters, continuous lines stand for systolic ones. The decrease in VHF amplitude for diastolic and systolic invariants after training for this subject is representative of the significant statistical difference over the 8 subjects of the study.

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