

Profiling biomechanical abilities during sprint front-crawl swimming using IMU and functional clustering of variabilities

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43 Abstract :

44 This study aims to profile biomechanical abilities during sprint front-crawl by identifying 45 technical stroke characteristics, in light of performance level. Ninety-one recreational to world-

45 technical stroke characteristics, in light of performance level. Ninety-one recreational to world-46 class swimmers equipped with a sacrum-worn IMU performed 25m all-out. Intra and inter-

47 cyclic 3D kinematical variabilities were clustered using a functional double partition model.

- 48 Clusters were analyzed according to (1) swimming technique using continuous visualization
- 49 and discrete features (standard deviation and jerk cost) and (2) performance regarding speed
- and competition caliber using respectively one-way ANOVA and Chi-squared test as well as
- 51 Gamma statistics. Swimmers displayed specific technical profiles of intra-cyclic (*smoothy* and *jerky*) and inter-cyclic stroke regulation (*low, moderate* and *high repeatability*) significantly
- discriminated by speed (p<0.001, $\eta^2=0.62$) and performance caliber (p<0.001, V=0.53). We
- showed that combining high levels of both kinds of variability (*jerky+low repeatability*) are
- associated with highest speed (1.86±0.12 m/s) and competition caliber (γ =0.75, p<0.001). It
- highlights the crucial importance of variabilities combination. Technical skills might be driven
 by a specific alignment of stroke pattern and its associated dispersion according to the task
- 57 by a specific angliment of stroke pattern and its associated dispersion according to the task 58 constraints. This data-driven approach can assist eyes-based technical evaluation. Targeting the
- 59 development of an explosive swimming style with a high level of body stability should be
- 60 considered during training of sprinters.

61 Introduction

- 62 Performance analysis in swimming requires the identification of individual skills and the way
- 63 the best swimmers master their movement (Bartlett, 2001). Therefore, monitoring their
- biomechanical abilities through technical assessment is at the heart of the understanding of elite
- 65 performances. Swimming is a sequence of repeated but not identical body movements targeting
- 66 effective motor patterns to achieve optimal performance (Maglischo, 2003). Thus, variability
- 67 is inherent to swimming technique and occurs within a stroke cycle or across multiple stroke
- 68 cycles, respectively known as intra and inter-cycle variability (Fernandes et al, 2022a). Such
- variabilities are of crucial interest as it can affect the swimming speed (Figueiredo et al., 2013)
- and reflect underlying regulation of stroke mechanics. Hence, evaluation of both intra and inter-
- 71 cyclic kinematical variability, as well as their combination, may provide valuable insights on
- the relationship between movement variability and technical skills during swimming.

73 Previous research focused on intra-cycle variability and its relations with performance and expertise (Fernandes et al., 2022b). Nevertheless, associations between intra-cyclic aspects of 74 75 kinematical variability and technical skills remain unclear. Intra-cyclic velocity variations 76 (IVV) were primarily investigated leading to contradictory findings since opposite correlations 77 between IVV and performance were observed (Barbosa et al., 2012; Barbosa et al., 2005; Schnitzler et al., 2008). Moreover, divergent outcomes were pointed out regarding the impact 78 79 of expertise since better skilled swimmers can show higher, lower or similar IVV (Fernandes et al., 2023). Despite the identification of IVV as a relevant way to monitor swimming 80 biomechanical development (Vilas-Boas et al., 2011), inconsistency of literature leads to a 81 82 crucial lack of information on regulation of stroke variability. In that respect, considering other 83 variables than the forward linear velocity to assess intra-cyclic variability may be meaningful. 84 Indeed, the understanding of the stroke cycle effectiveness refers to the interplay between the propulsive and drag forces that produce body accelerations (Gonjo et al., 2021). Hence, this 85 86 dynamical interaction reflected by kinematics is considered as an efficiency estimator (Barbosa 87 et al., 2012; Figueiredo et al., 2012a). Therefore, analyzing the intra-cyclic acceleration may be of great interest as it provides relevant diagnostic of front-crawl technical skills (Ichikawa, 88 1999) and propelling actions (Buchner & Reischle, 2002) by a much direct evaluation of the 89

90 capacity to propel the body with minimal velocity variations (Gonjo et al., 2021). Acceleration 91 has been shown as a sensitive measure of swimming performance since correlation between 92 velocity and root mean square of acceleration was reported (Tella et al., 2008; Tella et al., 2010). Then, it may be considered as a consistent indicator of stroke mechanics performance 93 and expertise, reflecting a possible advantageous technique (Holmer., 1979) or higher stroke 94 95 efficiency (Gil et al., 2012). Moreover, time variation of acceleration (*i.e.* jerk) may also reflect important technical skills because it quantifies the smoothness that leads to a more efficient 96 97 movement (Hreljac, 1993). In that sense, smoothness is a universal feature of skilled movement 98 which may be used as a window into athletic coordinative proficiency (Kiely et al., 2019). Thus, the jerk cost has been recently used in swimming to evaluate the technique 99 (Ganzevles et al., 2019) and stroke regulations (Bouvet et al., 2023). Finally, the acceleration 100 101 pattern and its derivative may be valuable for intra-cyclic variability regulation assessment.

102 Swimming stroke analyses generally consider only intra-cyclic aspects of motor pattern in isolation of adjacent cycles that reduces the understanding of variability. However, considering 103 104 also the movement variability between cycles, may provide complementary information about performance and technical skills characterization (Fernandes et al., 2022b). Given the 105 106 traditional approach of movement variability as noise (Preatoni et al., 2013), swimmers with high inter-cyclic variability may exhibit a greater dispersion in their technique and a lower 107 repeatability in their kinematics leading to reduced performance. Fernandes et al., (2022a) 108 109 suggested that slowest swimmers displayed higher mean velocity oscillations between two 110 consecutive cycles with higher numbers of cycles presenting extreme variations than the fastest ones. However, Fernandes et al., (2022b) showed that elite swimmers' velocity in backstroke 111 112 were more unstable and complex despite similar intra-cycle variations. Thus, inter-cyclic 113 variability may contain important information about motor organization and not only refer to 114 deleterious limitations to performance which should therefore be eliminated.

Variability analysis has been achieved using a variety of devices, including video, speedometer, 115 116 motion capture and inertial measurement units (IMU) (Fernandes et al., 2023). Among them, 117 IMU is a relevant embedded tool to assess 3D swimming kinematics in a real environment (Mooney et al., 2016). Moreover, IMU directly measures the acceleration which is convenient 118 119 for movement variability analysis. Indeed, it may avoid errors on acceleration signals that can 120 arise using numerical derivatives from position and velocities. Therefore, IMU is suitable to 121 monitor intra-cyclic acceleration pattern allowing to track technical skills and changes in efficiency (e.g. Engel et al., 2022; Ganzevles et al., 2019; Tella et al., 2008). Furthermore, as 122 swimming is composed of translational and rotational motions, IMU may enable more insights 123 124 on movement variability because it also measures angular velocities. Since IMU data are 125 multivariate time series, it seems appropriate to consider their functional form by continuous 126 instead of discrete measures of variabilities (Ryan et al., 2006). To this end, motor control 127 methodologies present a useful framework for variability analysis based on nonlinear dynamics 128 in time series (Bravi et al., 2011). Among them, features of complexity, such as the approximate 129 and the sample entropy, allowed to quantify the temporal structure in the signals through the 130 unpredictability of its variations. This methodology was applied in swimming kinematics to provide new insights into variability (Barbosa et al., 2017; Fernandes et al., 2022b). However, 131 132 even if entropy features proceeds over the entire signal to capture temporal dynamics, and thus 133 could be considered as an easy-to-use continuous measure, they finally result in a restricted 134 scalar value (i.e., discretization of the information in a numeric feature), whereas variability 135 analysis could be improved by considering it as a function of the time. Indeed, function regression provided more informative and intuitive interpretations of function-valued data, as 136 time series, than conventional single scalar approaches (Yen et al., 2015). Moreover, entropy 137 138 features can't handle the multivariate nature of IMU data, referring to interactions between

- 139 dimensions of swimmers' motion variability. As a consequence, this kind of discrete parameters
- 140 neglect a part of the temporal and dynamical information in functional data leading to restricted
- 141 details on motricity (Richter et al., 2014). Then, numerous studies in swimming were limited to

142 these non-function-valued methodologies in process-driven approaches, mainly due to the

- absence in literature of a suitable statistical model capturing the functional nature of the IMU
- 144 swimming data. Thus, it leads to limited data-driven insights regarding kinematical variabilities
- 145 profiling and performance explanations. Therefore, taking into account the need to, on the one
- 146 hand, consider the entire sequence of data points, and on the other, directly model swimming
 147 variabilities through functional data analysis (EDA) applied to MUL data is erusial
- 147 variabilities through functional data analysis (FDA) applied to IMU data is crucial.

148 In order to better investigate the kinematical variability recorded by IMU and its relation with 149 technical skills and performance, FDA depicts a useful way. Actually, FDA can take into 150 account the shape of kinematical curves, by relying on statistical modeling of data, giving indications on the motor pattern and helping to classify behavior and relevant characteristics of 151 152 performance (Preatoni et al., 2013). Indeed, FDA can outpace traditional approaches relying on 153 process-driven analysis and computation of discrete features that leads to limited kinematical 154 information (Mallor et al., 2010). For example, it provides evidence on technical differences 155 in national and international race-walkers (Donà et al., 2009). Moreover, literature demonstrated the usefulness of FDA for motion pattern analysis and description of different 156 performance groups on cyclic biomechanical data such as gait, running and cycling (Andrade 157 158 et al., 2014; Forrester & Townend, 2015; Helwig et al., 2016). In this way, Barbosa et al., 2021 159 highlighted differences between international and national-level sprinters using a general FDA approach, without automatic classification of swimmers. Furthermore, these methods can be 160 161 extended, regarding the scope of application and the data specificities, to allow clustering of 162 functional data (Jacques & Preda, 2014) and then group similar time series of biomechanical or 163 performance parameters (Leroy et al., 2018). Then, functional data clustering has been 164 growingly applied in applications of various fields of science and gathering statistical methods 165 coming from FDA and clustering community (Zhang & Parnell, 2023). Hence, it may provide 166 identification of trends and features leading to new insights about technique and performance 167 profiles in sport applications. More generally, cluster analysis is a powerful data-driven tool for detect performance and technique patterns in various sport applications such as athletes' visual 168 search strategies (Murray & Hunfalvay, 2017), anthropometric attributes (Zhang et al., 2018) 169 and coordination pattern in swimming (Seifert et al., 2016; Bideault et al., 2013). Then, in its 170 171 functional extension, clustering may be a powerful approach to deal with IMU data in order to profile variabilities in swimming. However, such methodology of functional data clustering 172 generally required the use of a customized statistical model able to deal with both the specificity 173 174 of the input data and the aim of the analysis (Bouveyron et al., 2019). To this end, recent 175 developments in statistical literature provided an approach explicitly devoted to functional 176 clustering of swimmers through the modeling of kinematical variabilities recorded by IMU 177 (Bouvet et al., 2024). It embodies a promising way to perform profiling of biomechanical 178 abilities during swimming based on both intra and inter-cyclic kinematical variability.

The present study aimed at clustering intra and inter-cyclic variability considering the functional nature of 3D IMU data during sprint front-crawl swimming in order to identify technical strokes characteristics according to the performance level leading to biomechanical abilities profiling.

183 Materials and methods:

184 Participants

185 91 subjects (31 women, age: 18.7±3.20 y.o.; height: 170±6.37 cm; mass: 60.1±6.67 kg; FINA

- 186 points on 50m freestyle short course: 457 ± 175) and 60 men, age: 21.4±6.65 y.o.; height:
- 187 183 ± 8.01 cm; mass: 71.8±12.3 kg; FINA points on 50m freestyle short course: 527±195)
- 188 participated in this study including recreationally active to world-class swimmers (McKay et
- al., 2022). All participants signed an informed consent form in agreement with the French
 Ethical Committee (approval obtained under reference 2021-A00250-41).
- Elinical Committee (approval obtained under reference 2021-A00250-4
- 191
- **192**Data collection

193 Each swimmer performed a 25m wall-start in front-crawl at maximal intensity with the instruction to not perform underwater kicks and breathing. Participants were instrumented with 194 195 one waterproof 3D IMU (Xsens DOT, Movella, Enschede, The Netherlands) sampled at 60 Hz using a full scale set at 16 g for the accelerometer and 1000 deg/s for the gyroscope. The sensor 196 197 was placed on the sacrum, then fixed with double-sided tape and secured with waterproof medical adhesive (Tegaderm, 3M, Cergy-Pontoise, France). The IMU described a coordinate 198 system defined with x-axis pointing cranially, y-axis pointing laterally, and z-axis pointing 199 200 posteriorly.

201

202 IMU data preprocessing and functional data clustering model

Raw data were filtered using a second order Butterworth low-pass filter with a 10 Hz cut-off frequency. The algorithm of Delhaye et al., 2022 was used, on the one hand, to extract only the front-crawl frames from the signal based on the human activity recognition provided by the classifier, and to the other hand, to compute average swimming speed as the pool length (i.e., 25m) divided by the lap time automatically provided by the model.

- 208 In order to avoid kinematical disturbances in data during the first stroke after swimmer's 209 breakout and finish, one-second time windows before and after the first and the last front-crawl frame were removed. In order to prevent temporal drift in swimmer's time series, curve 210 alignment is performed to enable proper functional modeling. It is achieved by adjusting the 211 signal starting point at the frame corresponding to a common reference for all swimmers 212 213 (Bouvet et al., 2024). To do so, we used a specific and generalizable feature in the IMU signals, 214 defined as an operational definition of a stroke cycle beginning in swimming literature. The latter was identified as the first zero-crossing on the medio-lateral acceleration filtered with a 215 216 second-order Butterworth band-pass filter between 0.1 and 1 Hz (Ganzevles et al., 2019). For 217 each cycle, data were time normalized using the previously described zero-crossing detection. 218 This feature allows, through a highly filtered signal processing approach, to only extract the 219 waveform characteristics about that IMU axis. Consequently, the repeating elemental pattern 220 obtained is representative of the body roll during front-crawl (Mooney et al., 2016) and allowed 221 to both determine the periodicity of the signal as well as extracting the single-cycle data 222 (Zhuang & Xue, 2019). This method allows to identify the start and end of a stroke cycle while 223 dealing with high levels of intra and inter-subject kinematical variability as well as noise in sensor's measurement. Finally, its generalization ability defines consistent time within a stroke 224 225 cycle, which is a required step in the functional clustering of kinematics detailed below. Figure 226 1 shows the preprocessed data for two participants of different levels.
- 227

228

[FIGURE 1 NEAR HERE]

These data were then clustered using the double partition model of Bouvet et al., (2024). This
FDA framework enables a fully integrated curve clustering based on both kinds of variabilities

- and also considers dependency between both partitions. Modeling this dependency during the
- clustering process is mandatory since the difficulty of reproducing a swimming pattern (i.e.,
- inter-cyclic variability) depends on its shape (i.e., intra-cyclic variability). Then, this approach

235 is able to model and analyze the complex multivariate dynamics of swimming patterns by 236 aggregating the dependent kinematical variabilities linked to swimming technical skills into 237 interrelated partitions. As a consequence, this extended FDA approach belongs to the modelbased functional clustering (Jacques & Preda, 2014; Bouveyron et al., 2019), and has been 238 239 developed for taking into account all of the specificities of the kinematical swimming data 240 recorded by IMU through a powerful statistical model devoted to technical skills profiling 241 (Bouvet et al., 2024). Based on a multivariate functional decomposition of IMU signals as well 242 as squared residuals into Fourier basis, the model considers both the kinematical information 243 related to stroke pattern as well as the ability to reproduce it. Finally, it led to two partitions respectively related to intra and inter-cyclic variability clusters. The degrees of each Fourier 244 245 basis were selected between four and twenty using a leave-one-out cross-validation. Model selection was performed using Bayesian Information Criterion considering clusters values 246 between one and five. Visualization was performed by computing the mean cluster curves (*i.e.* 247 248 stroke pattern representing intra-cyclic variability) as well as credibility region (*i.e.* ability to reproduce the stroke pattern representing inter-cyclic variability). 249

250251 *Statistical analysis*

Statistical analyses were conducted using RStudio (Version 4.2.2, RStudio, Inc., Boston, MA,
USA). The level of significance was set at p<0.05.

254

255 *Technical analysis of clusters*

To identify cluster technical profiles, classes were analyzed regarding clustering visualization and biomechanical parameters computed on each IMU axis. Indeed, considering clusters mean curves, standard deviation was calculated as a reflection of cycle variation (Dadashi et al., 2016) and jerk cost (for accelerometric dimension) as a practical evidence of stroke smoothness (Ganzevles et al., 2019). Regarding cluster credibility region curves, standard deviation was calculated as the amount of kinematical dispersion.

262

263 *Performance analysis of clusters*

264 To identify cluster performance profiles defining relevant biomechanical abilities, two analyses 265 were conducted considering different partitions: both single and the cross-partition (i.e. 266 combination of inter and intra-cyclic variability clusters for each subject, reflecting technical 267 skills profiling). Firstly, a one-way analysis of variance (ANOVA) or t-test was performed to 268 investigate the link between swimming speed and the partitions. If appropriate, post-hoc tests 269 were conducted with Tukey test and Bonferroni correction. The magnitude of differences was 270 interpreted using generalized eta-squared (η_g^2) for ANOVA or Cohen's d (d) for t-test with threshold values of respectively 0.01, 0.06, 0.14 and 0.20, 0.50 and 0.80 defining trivial, small, 271 272 medium and large effects (Cohen, 1988). Secondly, a Pearson's Chi-squared test was performed to investigate the dependence between a performance caliber ordinal variable (defined as Tier1, 273 Tier4-5 respectively for recreationally active (tier 1) 274 Tier2-3 and swimmers, 275 trained/developmental (tier 2) or highly trained/national level (tier 3) swimmers and 276 elite/international level (tier 4) or world class (tier 5) swimmers according to McKay et al., 2022) and the clusters ranked as ordinal variables based on speed. These modalities of the 277 278 performance caliber ordinal variables displayed FINA points on 50m freestyle short course of 308±128, 455±78 and 742±73 for respectively Tier1, Tier2-3 and Tier4-5. The magnitude of 279 280 differences was interpreted using V Cramer (V) and threshold values of 0.10, 0.20, 0.40, 0.60, 281 0.80 and 1 defining negligible, weak, moderate, relatively strong, strong and very strong effects 282 respectively (Cramer, 1946). The strength of the association between performance caliber and 283 clusters was measured using the Goodman Kruskal's Gamma statistic (y) (Goodman & Kruskal, 1954) with 95% confidence intervals and threshold value of 0.01, 0.10, 0.30, 0.60, 0.75 and 1 284

defining no association, negligible, low, moderate, strong, and very strong association
respectively (Rea & Parker, 2014).

287 288 **Results**

289 *Technical profiles according to cluster*

290 Mean cluster curves and credibility regions for the accelerometric and gyroscopic dimensions are presented on Figure 2 and Figure 3, respectively. The best model displayed two clusters of 291 292 stroke patterns defining intra-cyclic variability and three clusters of ability to reproduce the 293 stroke pattern defining inter-cyclic variability. Intra-cyclic variability clusters displayed a specific stroke pattern, especially discriminated by signal amplitude and number of peaks in 294 295 longitudinal and anteroposterior acceleration as well as signal amplitude in mediolateral acceleration. Then, clusters of intra-cyclic variability were named as the *jerky* and the *smoothy* 296 297 class. The biomechanical features for the accelerometric and gyroscopic dimensions are 298 displayed on Table 1 and Table 2, respectively. The *jerky* cluster displayed stroke pattern with higher variations of 74% and 178% on longitudinal and anteroposterior accelerations and of 299 300 181% and 8% on mediolateral and anteroposterior angular velocities, as well as lower variations of 15% on mediolateral acceleration and 11% on longitudinal angular velocity. The stroke 301 smoothness of the jerky cluster was lower of 830% and 1675% on longitudinal and 302 303 anteroposterior accelerations but lower of only 14% on mediolateral acceleration in comparison 304 with the *smoothy* cluster (see Table 1). Inter-cyclic variability clusters were ordered according 305 to the magnitude of stroke pattern dispersion. Thus, the resulting three kinds of inter-cyclic 306 variability were referred as low (LR), moderate (MR), and high (HR) repeatability clusters. Indeed both the credibility region around the mean cluster curve (see Figure 2 and Figure 3) 307 308 and the corresponding kinematical variation (see Table 2) were higher as clusters moved closer 309 to LR. For example, the dispersion in longitudinal acceleration was 633% higher in MR than HR and 117% in LR than MR clusters. 310 311

[FIGURE 2 NEAR HERE] [FIGURE 3 NEAR HERE] [TABLE 1 NEAR HERE]

[TABLE 2 NEAR HERE]

319320 *Performance profiles according to cluster*

Swimming speeds according to the different classes coming from the intra and inter-cyclic 321 322 variability clustering are presented on Figure 4, as well as the classes coming from the crosspartition on Figure 5. Regarding clustering of mean stroke pattern (*i.e.* intra-cyclic variability), 323 the jerky class showed a significantly higher swimming speed of 29.6% compared to the 324 325 smoothy class with a large effect size $(1.84 \ [1.79; 1.89] \pm 0.12 \ vs. 1.42 \ [1.38; 1.47] \pm 0.18$, 326 t(68.0)=12.8, p<0.001, d=2.72). Regarding clustering the ability to reproduce the stroke pattern (*i.e.* inter-cyclic variability), there was a large significant swimming speed difference between 327 328 the three clusters (F(2.88)=21.7, p<0.01, η_s^2 =0.33). Regarding the cross-partition, there was a large significant swimming speed difference between the five clusters (F(4.86)=34.6, p<0.01, 329 330 $\eta_{g}^{2}=0.62$). Table 3 presented the significant pairwise comparisons for both the inter-cyclic 331 variability partition and the crossing partition, with all p<0.01. 332 333 **[TABLE 3 NEAR HERE]**

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335	[FIGURE 4 NEAR HERE]
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338	[FIGURE 5 NEAR HERE]
339 340	Performance caliber distribution according to the different classes coming from the intra and inter-cyclic variability clustering are presented on Figure 6, as well as the classes coming from
341	the cross-partition on Figure 7. Clusters of mean stroke pattern are strongly dependent on
342	performance caliber ($\chi^2(2)$ =49.9, p<0.001, V=0.74) with a very strong significant association
343	between the more the stroke pattern is <i>jerky</i> , the higher is the performance caliber (γ =0.97 [0.93]
344	; 1.00], p<0.001). Clusters of ability to reproduce the stroke pattern are moderately dependent
345	of performance caliber ($\chi^2(4)=28.0$, p<0.001, V=0.39) with a strong significant association
346	between the more there is low repeatability stroke pattern, the higher is the performance caliber
347	$(\gamma=0.63 [0.42; 0.84], p<0.001)$. Clusters of the cross-partition are relatively strongly dependent
348	of performance caliber ($\chi^2(10)=51.5$, p<0.001, V=0.53) with a very strong significant
349	association between the more the stroke pattern is <i>jerky+low repeatability</i> the higher is the
350	performance caliber (γ =0.75 [0.60; 0.89], p<0.001).
351	IFICUDE (NEAD HEDE)
352	[FIGURE 0 NEAR HERE]
357	FIGURE 7 NEAR HEREI
355	[FIGURE / NEAR HERE]
356	Discussion and Implication
357	This study aimed at clustering intra and inter-cyclic 3D kinematics during sprint front-crawl to
358	identify technical strokes characteristic according to performance level based on an embedded
359	IMU on the sacrum. To this end, a data-driven process based on a large database and including
360	an heterogeneous level, ranging from recreationally active to world-class swimmers, was
361	applied for multivariate functional clustering considering the specificities of IMU swimming
362	data. Specific profiles of technique variability were identified. Indeed, two clusters of intra-
363	cyclic stroke regulation (smoothy and jerky) and three clusters of inter-cyclic stroke regulation
364	(<i>LR</i> , <i>MR</i> , and <i>HR</i>) were identified. All of them were analyzed according to swimming speed
365	and performance caliber supporting the identification of relevant biomechanical abilities for
366	front-crawl sprint.
367	Descriptions the intro evaluation defining magnitude of veriability, the smoothy class presents
360	a more fluent acceleration pattern than the <i>jarky</i> one with continuity of propulsive actions. It is
370	characterized by a lower acceleration variation along the longitudinal and anteronosterior axes
371	and a higher variation of longitudinal angular velocity in addition to mediolateral acceleration.
372	The <i>ierky</i> class includes a more explosive and rough stroke pattern leading to a higher ierk cost
373	along longitudinal and anteroposterior reflecting degradation of stroke smoothness. Indeed,
374	smooth swimming movements referring to a low jerk cost, are those without abrupt, intermittent
375	and discontinuous changes in accelerations, whereas non-smooth stroke patterns reflect
376	abruptness and erratic discordance (Kiely et al., 2019). A higher jerk cost might lead to a faster
377	swimming (Ganzevles et al., 2019) as it implies greater intra-cycle acceleration and deceleration
378	that can be converted into higher speed with appropriate technical skills. Indeed, our results are
379	in line with such behavior because the jerky participants swim significantly faster than the
380	swimmers of the <i>smoothy</i> cluster while being the ones demonstrating the higher performance
381	caliber. Thus, the <i>jerky</i> cluster gathers almost all of the elite and world-class swimmers, whereas
382	the <i>smoothy</i> cluster includes all the recreationally active swimmers and the majority of the
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trained and highly trained swimmers. It may be explained by a larger speed curve amplitude in
faster sprinters (Barbosa et al., 2021) as well as higher peaks in speed with similar minimal

speeds (Leblanc et al., 2007). However, the lower stroke smoothness induced by higher intra-385 cyclic variability in the *jerky* stroke pattern may also be associated with higher energy 386 387 expenditure leading to a lower stroke efficiency (Fernandes et al., 2023). Nevertheless, the jerky cluster displays reduced variations in both mediolateral acceleration and longitudinal angular 388 389 velocity than the smoothy one, reflecting more core stability and a better overall alignment of 390 the body by possibly a decrease of body roll. However, body roll is not directly assessed in this work. To the author's knowledge, only the biomechanical model of Bächlin & Tröster (2012) 391 392 tracked body roll angle from IMU data under strong mechanical assumptions. Indeed, body 393 angles assessment from IMU data requires a sensor-to-segment calibration, combined with a reliable computing of the sensor orientation, which involves very complex processings in the 394 395 water environment (Mangia et al., 2017). Hence, in this work, we consider the association between medio-lateral acceleration recorded from a sacrum IMU during front-crawl and body 396 397 roll previously used in literature (Mooney et al., 2016; Callaway, 2015). Since the medio-lateral acceleration with respect to the swimmer mainly reflects the roll movements during front-crawl 398 (Ganzevles et al., 2019), we use this indirect relationship as a proxy for interpretation of our 399 400 functional clustering. Then, the higher stability that could be induced by this reduced body roll 401 seems to especially occur during the critical propelling phases of the cycle (i.e., extrema of longitudinal acceleration). This finding is in line with previous literature pointing out a 402 403 reduction of whole-body roll, shoulder roll and hip roll amplitude in front crawl as pace 404 increases (Gonjo et al., 2021). It allows to improve stroke rate by reducing the stroke cycle 405 duration (Psycharakis & Sanders, 2008) while avoiding disturbance of propulsion caused by a 406 large amount of torque around longitudinal axis (Yanai, 2003). Then, the *jerky* stroke pattern 407 matches the requirements of the maximal exercise performed since reducing amplitude of body 408 roll is expected from sprinters as they use higher stroke frequency and a possible more 409 continuous inter-limb coordination (Seifert et al., 2010).

410 In summary, faster front-crawl sprinters display specific regulations of stroke pattern variability, reflected as *jerky*, targeting two goals. Firstly, producing high intra-cyclic 411 acceleration fluctuations along both forward and upward axes leading to a degradation in 412 413 overall stroke smoothness and an increase in energy expenditure. Secondly, presenting a higher 414 body stability during the critical instants of forward propulsion, that is the stroke cycle timings with the higher forward speed variations (i.e., peaks and valleys on longitudinal acceleration), 415 416 might lead to faster swimming. More precisely, it may be enabled by reducing body roll in order 417 to increase the stroke rate.

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419 Regarding the inter-cyclic clusters defining the structure of variability, three profiles arise from 420 two characteristics. On the one hand, the non-constant credibility regions (as depicted on Figure 421 2 and Figure 3) refer to unequal variance in inter-cyclic kinematics. It indicates various stroke pattern dispersions and uneven variability according to the instant within the stroke cycle. More 422 423 precisely, the highest dispersion occurs during the peaks on accelerations that lead to swimming 424 velocity generation. Thus, such findings are in line with previous outcomes showing that the 425 higher velocity oscillations in extreme cycles occurred mainly during propulsive phases of the 426 cycle (Fernandes et al., 2022a). On the other hand, faster swimmers display significantly lower 427 repeatability of stroke pattern indicating that higher kinematical inter-cyclic variation is 428 associated with better sprint performance. Indeed, 62% of the LR cluster is composed of elite 429 to world class swimmers. Fernandes et al., (2022b) showed that elite swimmer's kinematics 430 (*i.e.* velocity variability) in sprint backstroke were more unstable than non-elite's ones which 431 is in line with our result as the LR cluster is the fastest. However, these authors assess the inter-432 cyclic variability in a process-driven approach, using features of nonlinear dynamics (i.e., 433 sample entropy and Largest Lyapunov Exponent) that captures the notion of stability and 434 complexity in the raw kinematical signal. Nevertheless, in the present approach, relying on

435 multivariate functional clustering, inter-cyclic variability is assessed through a modeling of the ability to reproduce the swimming pattern. This methodology presents relevant advantages in 436 437 comparison to discrete features of nonlinear dynamics (Bouvet et al., 2024). Indeed it allows, 438 on the one hand, to deal with multivariate time series in order to consider at the same time all 439 the IMU dimensions as well as their interactions, and on the other hand, to quantify both the 440 magnitude of inter-cyclic variability as well as the the timings in stroke cycle at which it occurs. 441 It opens the door to data-driven approach by applying curve clustering in sport settings (Chu et 442 al., 2020 ; Leroy et al., 2018). By gathering of FDA tools and clustering tools, respectively 443 towards suitable functional basis decomposition of the swimming IMU signals and double partition of multivariate data allowing for dependency, the methodology used in this work 444 445 enable the identification of heterogeneous morphological patterns in swimming kinematics (Zhang & Parnell, 2023). Despite the inherent methodological differences with features of 446 447 nonlinear dynamics, that could lead to further works comparing or combining them with specific FDA approach to help in the understanding of the inter-cyclic variability (Barbosa et 448 al., 2017), congruent results are highlighted regarding the association between inter-cyclic 449 450 variability of kinematics and sprint swimming performance. Nonetheless, it seems 451 counterintuitive as traditional approaches of literature generally perceive movement variability as noise indicating poor technique or inefficiencies in movement patterns detrimental to 452 453 performance (Abernethy et al., 2008). This apparent paradoxical effect of inter-cyclic 454 variability on performance could be explained by the specificity of our population and sprint 455 task. Indeed, we consider a large database with multiple skill levels. Actually, the impact of 456 expertise on kinematical variability management remains unclear and would imply an adaptation to the task constraints rather than reproducing a predetermined motor pattern 457 (Fernandes et al., 2022a). Thus, the inverse relationship between movement variability and 458 459 expertise, skills or performance is not fully acknowledged in the literature, leading to a 460 contentious role in sport technique (Preatoni et al., 2013 ; Glazier & Davids, 2009). Indeed, recent studies about swimming provided evidence that highly skilled athletes display larger 461 levels of movement variability to maximize their swimming speed during 50m freestyle 462 (Ganzevles et al., 2019; Morais et al., 2023). Moreover, Fernandes et al., 2022a demonstrated 463 464 that variability characterizes the sprint swimming. In that respect, sprint performance would be associated with kinematical variability since elite swimmers adopted strategies to manage it, 465 466 referring the movement variability as an emergent behavior under highly constrained aquatic 467 environment and sprint task (Fernandes et al., 2022b). Then, movement variability is not always detrimental to performance (Seifert et al., 2013). It can be adaptive as world class swimmers 468 469 must explore the environment to provide functional regulations of motor patterns leading to 470 effective outcomes (Seifert et al., 2016 ; Seifert et al., 2011). As a consequence, movement 471 variability is a way to distinguish elite athletes as previously shown in race walking (Preatoni et al, 2010), and may also contribute to human movement optimization to ensure success in 472 473 technique as highlighted in gymnastics (Hiley & Yeadon, 2013). Furthermore, swimming at high intensity in front-crawl implies biomechanical constraints leading to technical adaptations 474 475 of movement variability and coordination pattern (Seifert et al., 2016). The latter may be related 476 both to swimmer's speciality (*i.e.* sprint or distance swimming) and swimmer's characteristics (i.e. expertise level or gender) (Figueiredo et al., 2012b ; Bideault et al., 2013). However, 477 478 variability may also reflect fatigue which can negatively affect the performance. 479 Finally, it is crucial to monitor kinematical variability in a data-driven framework to identify

when it reflects functional adaptations supporting performance versus when it indicates a need
for technical corrections. In that respect, the curve clustering framework used in the present
study can help on-field end-users for this purpose of technical profiling by using a functional
statistical model suited with the specificities of swimming kinematical data.

485 Regarding the cross-partition clusters defining technical skills profiling, both the *jerky+LR* and the *jerkv*+MR are the fastest clusters. Indeed, they are both composed of more than 70% by 486 487 elite to world-class swimmers with no one recreationally active. Such finding is consistent with 488 aforementioned results highlighting distinct association of intra and inter-cyclic variability clusters with performance. More precisely, specific congruence of variabilities by the 489 490 combination of both high levels of intra and inter-cyclic variability turns out to be a highly 491 discriminative aspect in the context of a sprint task. The present analysis did not reveal any 492 swimmers belonging to the *jerky*+*HR* cluster that represents a non-congruence of the two kinds 493 of variability (*i.e.* high level of intra but low level of inter-cyclic variability). Actually, a *jerky* but repeatable swimming may refer to a lack of technical skills to convert kinematical variations 494 495 to effective propulsion, while a *jerky* and unsteady swimming could refer to proficient functional adaptation to sustain the highest possible speed during sprint swimming. By this 496 497 way, it can be hypothesized that the biomechanical ability of swimmers to establish congruence between two kinds of stroke variabilities (*i.e.* mean stroke pattern and associated dispersion) 498 according to the constraints of the task (*i.e.* sprint swimming vs. long distance swimming) 499 500 define technical skills and swimming expertise. Indeed, the opposite cluster of congruent 501 variability (i.e. smoothy+HR) displays low performance level with only 2% of elite to world-502 class swimmers. Such results could be explained by the specificity of the sprint exercise 503 involving large constraints on swimmer's motricity through the requirement of maximal 504 propulsive forces by large kinematical variations at the expense of the swimming economy. 505 Indeed, swimmers are not concerned about saving energy during maximal trials and adopt a 506 strategy based on generating greater propulsive forces and less efficient technique (Lopes et al., 2023). Nevertheless, we may expect the smoothy+HR cluster to be a relevant technique for 507 508 other tasks including longer duration and lower intensity. Indeed, the technical requirements 509 are likely to be different between long, middle and short-distance events as resistive and propulsive forces differ between low and high speed in front-crawl (Takagi et al., 2021). For 510 example, longer distance swimming as open water races requires conservative strategy in order 511 to improve stroke efficiency by lowering energy cost from a given pace (Bouvet et al., 2023) 512 513 whereas overcoming a large drag by maximizing thrust force through mechanical power output 514 is essential in sprint swimming technique to achieve high velocities (Gatta et al., 2018). These specific task constraints can then widely affect the kinematics of swimmers by modifying the 515 516 management of movement variabilities. By the way, swimmers adapt their technique in order 517 to maximize performance.

In summary, it seems that the intra-cyclic variability is the most impacting kind of variability on performance for sprint swimming. Indeed, the present results do not highlight any significant differences in terms of speed for the different inter-cyclic pattern given the intra-cyclic pattern, albeit all of the three *smoothy* clusters are significantly different from the two *jerky* clusters. Therefore, it results in distinctive profiles combining intra and inter-cyclic variability and defining relevant biomechanical abilities.

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525 Further assessment of variabilities regarding tasks constraints is necessary to fully understand 526 stroke regulations leading to swimming performance. Extending the current approach to longer 527 swimming duration can be a powerful way to interpret variabilities profiles according to race 528 distance and define effective swimming technical skills. A limitation of this study is the lack of anthropometric and gender data that may impact the preferential kinematics. Moreover, 529 530 combining present functional clusters of variabilities with conventional stroke parameters as stroke length, stroke rate and stroke index would contribute to the improvement of the 531 532 identification of relations between technical regulations and their spatio-temporal outcomes.. 533

534 In conclusion, the present study provided the first data-driven approach to profile technical 535 stroke profiles during sprint front-crawl based on kinematical curve profiling of both intra and 536 inter-cyclic variability. In this way, it provides a novel method, based on an adapted functional clustering model, for variabilities determination in swimming using embedded sensors, as it is 537 538 a hot topic in literature (Fernandes et al., 2023). This study demonstrates the importance of 539 variabilities combination through their congruence to adapt the swimming technique. Indeed, 540 technical skills might be driven by a specific management of both variabilities, in order to align 541 stroke pattern and its associated dispersion, according to the performance features required by 542 the task constraints. Therefore, sprint swimming requires both a high level of intra and inter-543 cyclic variability through a jerky and unsteady stroke pattern. In contrast, polarization of 544 variabilities seems dysfunctional. The contributions of this study can assist eyes-based technical evaluation using an automatic and non-invasive continuous method, explicitly devoted to 545 546 swimming kinematical clustering, to provide objective data on variabilities regulations. Consequently, it allows coaches to profile technical skills while providing benchmarks to target 547 the development of an explosive swimming style with a high level of body stability for their 548 549 sprinters.

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557 Declaration of interest statement

558 The authors have no conflict of interests.

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Table 1. Biomechanical features computed by IMU axis from the mean curves of the intra cyclic variability cluster. LON: longitudinal. MED: mediolateral. ANT: anteroposterior

Cluster	Acceleration standard deviation (x10 g)		Angular velocity standard deviation (deg/s)			Jerk cost (x10·g ² /s ²)			
	LON	MED	ANT	LON	MED	ANT	LON	MED	ANT
Jerky	15.4	47.7	9.12	101	11.9	18.1	17.3	22.8	7.10
Smoothy	8.84	56.3	3.28	113	4.23	16.7	1.86	20.0	0.40

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925 Table 2. Biomechanical features computed by IMU axis from the credibility regions of the 926 inter-cyclic variability cluster. LON: longitudinal. MED: mediolateral. ANT: anteroposterior. 927 *LR: low repeatability. MR: moderate repeatability. HR: high repeatability*

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	Cluster	Acceleration $(x10^2 g)$			Angular velocity (deg/s)		
		LON	MED	ANT	LON	MED	ANT
Standard deviation	LR	2.39	1.32	0.39	426	334	87.0
	MR	1.10	1.14	0.36	284	96.8	81.0
	HR	0.15	0.38	0.07	117	21.3	28.1

957	Table 3. Significant pairwise comparisons of clusters for both the inter-cyclic variability
958	partition and the crossing partition. LR: low repeatability. MR: moderate repeatability. HR:
959	high repeatability

Partition	Cluster pairwise comparisons	Mean±SD and 95% confidence intervals of swimming speed (m/s)	Difference (%)	Effect size (Cohen's d)
Inter-cyclic	LR vs. HR	1.75 [1.63;1.87]±0.27 vs. 1.40 [1.35;1.46]±0.17	+25.0	1.67
variability	MR vs. HR	1.62 [1.53;1.70]±0.21 vs. 1.40 [1.35;1.46]±0.17	+15.7	1.15
	<i>Jerky</i> +LR vs. <i>Smoothy</i> +HR	1.86 [1.80;1.92]±0.12 vs. 1.40 [1.35;1.46]±0.17	+32.9	2.86
	<i>Jerky</i> +LR vs. <i>Smoothy</i> +LR	1.86 [1.80;1.92]±0.12 vs. 1.30 [0.88;1.71]±0.26	+43.1	3.68
Crossing intra-	Jerky+LR vs. Smoothy+MR	1.86 [1.80;1.92]±0.12 vs. 1.50 [1.42;1.58]±0.15	+24.0	2.60
cyclic variability	Jerky+MR vs. Smoothy+HR	1.81 [1.72;1.90]±0.13 vs. 1.40 [1.35;1.46]±0.17	+29.3	2.49
	Jerky+MR vs. Smoothy+LR	1.81 [1.72;1.90]±0.13 vs. 1.30 [0.88;1.71]±0.26	+39.2	2.97
	Jerky+MR vs. Smoothy+MR	1.81 [1.72;1.90]±0.13 vs. 1.50 [1.42;1.58]±0.15	+20.7	2.15









1000 1001 1002 1003	Figure 1 . Preprocessed data of two participants with different levels (blue: world-class swimmer (tier 5), red: recreationally active swimmer (tier 2)). Performance caliber defined according to the classification of McKay et al., 2022
1004 1005	Figure 2. Intra-cyclic clustering (<i>jerky</i> and <i>smoothy</i> stroke patterns) and inter-cyclic clustering (<i>low</i> , <i>moderate</i> and <i>high repeatability</i> credibility regions) of 3D accelerations
1006 1007 1008	Figure 3. Intra-cyclic clustering (<i>jerky</i> and <i>smoothy</i> stroke patterns) and inter-cyclic clustering (<i>low, moderate</i> and <i>high repeatability</i> credibility regions) of 3D angular velocities
1009 1010 1011 1012	Figure 4 . Swimming speed according to the classes coming from the partitions of (A) intra- cyclic variability clustering, (B) inter-cyclic variability clustering
1013 1014	Figure 5. Swimming speed according to the classes coming from the cross-partition
1015 1016 1017	Figure 6 . Performance caliber distribution according to the classes coming from the partitions of (A) intra-cyclic variability clustering, (B) inter-cyclic variability clustering
1018 1019 1020	Figure 7. Performance caliber distribution according to the classes coming from the cross- partition