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MULTIFRACTAL ANALYSIS FOR CUMULANT-BASED EPILEPTIC SEIZURE DETECTION IN EEG TIME SERIES

Omar D. Domingues⁽¹⁾, Philippe Ciuciu⁽¹⁾, Daria La Rocca⁽¹⁾, Patrice Abry⁽²⁾ and Herwig Wendt⁽³⁾

⁽¹⁾ CEA/NeuroSpin and INRIA-CEA Parietal, Univ. Paris-Saclay, France, philippe.ciuciu@cea.fr

⁽²⁾ Univ Lyon, Ens de Lyon, CNRS, Laboratoire de Physique, Lyon, France, patrice.abry@ens-lyon.fr

⁽³⁾ IRIT, CNRS, Univ. Toulouse, France, herwig.wendt@irit.fr

ABSTRACT

Multifractal analysis allows us to study scale invariance and fluctuations of the pointwise regularity of time series. A theoretically well grounded multifractal formalism, based on wavelet leaders, was applied to electroencephalography (EEG) time series measured in healthy volunteers and epilepsy patients, provided by the University of Bonn. We show that the multifractal spectrum during a seizure indicates a lower global regularity when compared to non-seizure data and that multifractal features, combined with few baseline features, can be used to train a supervised learning algorithm to discriminate well above chance ictal (i.e. seizure) versus healthy and interictal epochs ($\simeq 97\%$) and healthy controls versus patients ($\simeq 92\%$).

Index Terms— EEG, multifractal-analysis, seizure detection.

1. INTRODUCTION

Multifractal analysis is a useful tool to distinguish different behaviors of dynamic systems and stochastic processes. For instance, it has been applied to financial data for the comparison of price fluctuations of stocks and commodities [1], to texture classification [2] and the analysis of fetal heart rate variability [3], brain dynamics in functional neuroimaging [4, 5] among several other applications in physical and biological science. Multifractal analysis is intimately related to the notion of scale invariance of time series, which is often characterized by a Fourier power spectrum that behaves as a power law $|\nu|^{-\beta}$ in a range of frequencies $\nu \in [\nu_1, \nu_2]$, for $\beta > 0$, which is referred to as *power spectrum scale invariance*. In multifractal analysis, scale invariance is defined in a more comprehensive way: whereas the Fourier power spectrum depends only on second-order statistics of the time series, multifractal analysis studies the power law behavior of q -th order statistics of multiresolution quantities denoted by $S(j, q)$ for each scale j and for all $q \in \mathbb{R}$. Scale invariance is redefined as the power law behavior $S(j, q) \approx 2^{j\zeta(q)}$, which now

is described by a function $q \mapsto \zeta(q)$ instead of a single parameter β , providing a richer framework to scaling analysis. Moreover, the multifractal spectrum, which is theoretically estimated by a Legendre transform of $\zeta(q)$, can be shown to give us information regarding the overall pointwise regularity of a time series.

In this work, we used multifractal analysis - -based on the Wavelet Leader Multifractal Formalism (WLMF) [6] – to extract features from single channel EEG time series measured in healthy subjects and epileptic patients during seizure and seizure-free periods, using publicly available data provided by the University of Bonn [7]. We show that the average multifractal spectra are different between ictal (seizure) and interictal (between seizures) data, and also that multifractal features can be used to train a supervised learning algorithm to distinguish these two states with high accuracy. Also, these features were shown to be useful to discriminate healthy subjects and epileptic patients based on EEG data. Our approach does not focus on obtaining perfect classification scores: we aim to assess the usefulness of multifractal features in epileptic seizure detection, which may help understand neural dynamics during seizures.

In [8], the authors showed that multifractal features (also based on the WLMF) improved seizure prediction in mesial temporal lobe epilepsy using multi-channel intracranial EEG (iEEG) measurements, by training a classifier for each patient to discriminate preictal (state immediately before the seizure) and interictal epochs. The main advantages of the WLMF are: (i) it is theoretically well grounded and proved to be associated with the Hölder pointwise regularity and (ii) it is robust to smooth trends, since it is a wavelet-based method. Our contribution is the use of the WLMF to extract features from EEG and iEEG data measured from different subjects and different conditions to show that – even with this subject and measurement variability – multifractal features can discriminate well ictal versus healthy and interictal epochs and healthy subjects versus patients.

2. WAVELET-LEADER MULTIFRACTAL ANALYSIS

The goal of multifractal analysis is to summarize the point-wise regularity of a time series $X(t)$ by estimating the Hausdorff dimension of the sets $\{t \in \mathbb{R} : h_X(t) = h\}$, denoted by $\mathcal{D}(h)$, where $h_X(t)$ is the Hölder exponent of $X(t)$ at time t . The function $h \mapsto \mathcal{D}(h)$ is called *multifractal spectrum*. In practice we only have access to $X(t)$ in a discrete set of time points, thus we cannot estimate $h_X(t)$ precisely, since it is a local quantity requiring the knowledge of $X(t)$ in arbitrarily small intervals centered at t . Multifractal formalisms allow us to estimate $\mathcal{D}(h)$ from multiresolution quantities which are easily computed for discretized signals. A theoretically well grounded formalism is based on wavelet leaders which are defined as follows: let $\psi_0(t)$ be a mother wavelet, let $\psi_{j,k}(t) = 2^{-j}\psi_0(2^{-j}t - k)$, for $j, k \in \mathbb{Z}$ be dilated, translated and scaled versions of the mother wavelet and let $d_X(j, k) = \int_{\mathbb{R}} X(t)\psi_{j,k}(t) dt$ be the wavelet coefficients of $X(t)$. The wavelet leaders of $X(t)$ at scale j and time k are defined as the supremum of the wavelet coefficients at scales inferior to j and in a time window around k :

$$L_X(j, k) = \sup_{j' \leq j, 2^{j'}k' \in 3\lambda_{j,k}} |2^{j'\gamma} d_X(j', k')| \quad (1)$$

where $\lambda_{j,k} = [k2^j, (k+1)2^j)$, $3\lambda_{j,k} = \lambda_{j,k-1} \cup \lambda_{j,k} \cup \lambda_{j,k+1}$ and $\gamma > 0$ is a parameter that ensures that minimum regularity assumptions on the data are met, cf. [2] for details. Multifractal analysis is related to the scale invariance of the structure functions $S(j, q)$, which are time averages of the q -th power of wavelet leaders at each scale. Scale invariance is defined as follows:

$$S(j, q) := \frac{1}{n_j} \sum_{k=1}^{n_j} |L_X(j, k)|^q \approx 2^{j\zeta(q)} \quad (2)$$

for $j \in [j_1, j_2]$, $q \in \mathbb{R}$, where n_j is the number of wavelet leaders available at scale j and $\zeta(q)$ is referred to as scaling function. It can be proven that the Legendre transform of $\zeta(q)$ is an upper bound of the multifractal spectrum $\mathcal{D}(h)$:

$$\mathcal{L}(h) := \inf_{q \in \mathbb{R}} (1 + qh - \zeta(q)) \geq \mathcal{D}(h). \quad (3)$$

The function $h \mapsto \mathcal{L}(h)$ is called *Legendre spectrum* and it is possible to estimate $\mathcal{L}(h)$ without computing a numerical Legendre transform. Consider the first two cumulants of $\log L_X(j, \cdot)$, denoted by $C_1(j)$ and $C_2(j)$, which are computed for all $j \in [j_1, j_2]$, the range of scales where we observe a scale-invariant behavior:

$$C_1(j) = \frac{1}{n_j} \sum_{k=1}^{n_j} \log_2 L_X(j, k) \quad (4)$$

$$C_2(j) = \frac{1}{n_j} \sum_{k=1}^{n_j} (\log_2 L_X(j, k))^2 - C_1(j)^2. \quad (5)$$

It has been shown [2] that if the cumulants behave linearly as a function of the scale j , i.e. $C_1(j) = a + c_1 j$ and $C_2(j) = b + c_2 j$, we have the approximation $\mathcal{L}(h) \approx 1 + (h - c_1)^2 / (2c_2)$ if $c_2 < 0$. Thus, if $c_2 < 0$ the time series presents a multifractal behavior. The coefficients c_1 and c_2 are called *log-cumulants*; c_1 represents the most frequent regularity parameter in the time series, whereas c_2 measures the amount of variability in this regularity.

3. EEG DATA AND EXPERIMENTAL DESIGN

An open source Python toolbox¹ was used to apply multifractal analysis to the publicly available EEG dataset provided by a research group at the University of Bonn [7]. This dataset consists of 5 sets (A, B, C, D and E) with 100 time series each. Sets A and B contain scalp-based EEG measurements collected in five healthy volunteers. Volunteers were kept with eyes open (set A) or closed (set B). Sets C, D and E contain presurgical intracranial EEG (iEEG) measurements recorded in five patients; time series in sets C and D were recorded during a seizure-free (interictal) interval whereas time series in set E were recorded during an epileptic seizure (ictal). According to [7], data in set D were measured from within the epileptogenic zone, whereas data in set C were measured from the hippocampal formation of the opposite hemisphere of the brain. All time series are 4097 time-point long with a sampling frequency of 173.61 Hz, corresponding to a recording duration of 23.6 seconds. Fig. 1 shows examples of one time series of each set.

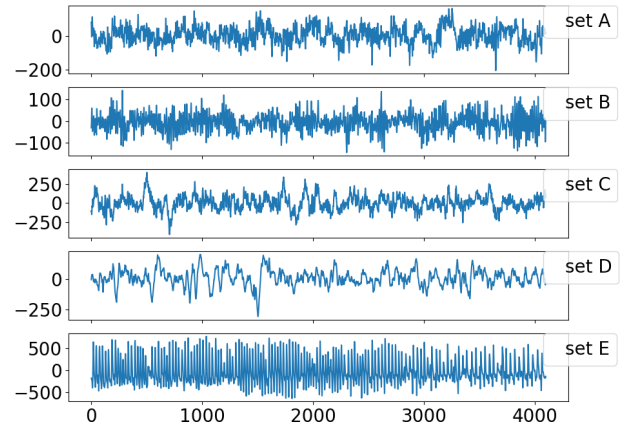


Fig. 1. Examples of time series in Bonn dataset. Sets A and B: EEG of healthy volunteer; sets C and D: iEEG for a patient during a seizure-free interval; set E: iEEG for a patient during epileptic seizure.

The wavelet leaders were computed over each of the 500 time series. We observed that the relation (2) holds in the range of scales $[j_1, j_2] = [5, 9]$, which corresponds to time scales between 0.1 s and 3 s approximately. In this range of scales, we used the relations (4)-(5) to compute the log-cumulants c_1

¹<https://github.com/neurospin/mfanalysis>, see also [5]

and c_2 . The parameter γ was set to 1.6 to ensure minimum regularity assumptions for all time series.

The cumulants c_1 and c_2 were then used as features to train a random forest classifier² for three classification problems:

- **ABCD vs. E:** Discriminate seizure (set E) from non-seizure (sets A, B, C and D) time series;
- **AB vs. CDE:** Discriminate EEG of healthy subjects (sets A and B) from EEG of epilepsy patients (sets C, D and E);
- **AB vs. CD vs. E:** Discriminate between healthy subjects, patients in seizure-free interval and patients during a seizure.

Other features were also used for comparison: peak-to-peak amplitude, skewness, kurtosis and line length [10], which were computed directly from each time series using the `mne-features` library for Python [11]. Precisely, we compared seven sets of features:

- **Feature set 1:** c_1 only;
- **Feature set 2:** c_2 only;
- **Feature set 3:** c_1 and c_2 ;
- **Feature set 4:** peak-to-peak amplitude;
- **Feature set 5:** peak-to-peak amplitude, skewness, kurtosis and line length;
- **Feature set 6:** c_1 , c_2 and peak-to-peak amplitude;
- **Feature set 7:** c_1 , c_2 , peak-to-peak amplitude, skewness, kurtosis and line length.

4. RESULTS AND DISCUSSION

Fig. 2 shows the average Legendre spectrum computed for all time series in each of the sets A-E. Interestingly, the average Legendre spectrum for set E is shifted to the left of all other average spectra, which reflects a lower global regularity in the data set E as compared to others. Fig. 3 shows the values of c_1 and c_2 for all time series, and we can see that the seizure (set E) and the non-seizure (sets A, B, C and D) data are approximately separated into two different clusters. Also, $c_2 < 0$ for 88% of seizure data and for 96% of seizure-free data, meaning that most time series presented a multifractal behavior.

For each classification problem and each set of features, we computed the accuracy and the area under the receiver operating characteristic curve (AUROC) for a 15-fold cross-validation scheme, in which data were randomly split 15 times into a training set containing 300 time series and a test set containing 200 time series. We report the average accuracy and AUROC and their standard deviations. We used a random forest consisting of 100 classification trees and no hyperparameter was optimized, to avoid possible over-optimistic results.

²Using the `scikit-learn` library for Python [9].

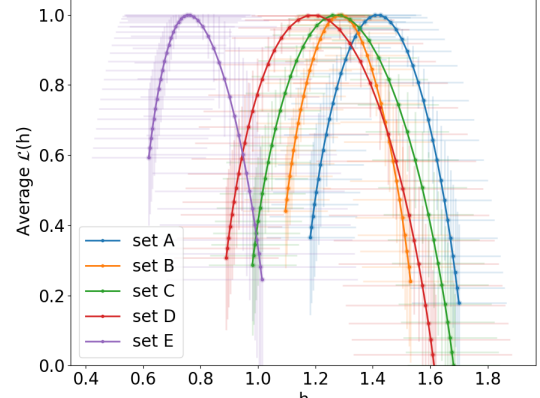


Fig. 2. Average Legendre spectrum $\mathcal{L}(h)$ for all time series in each data set. Error bars represent \pm one standard deviation.

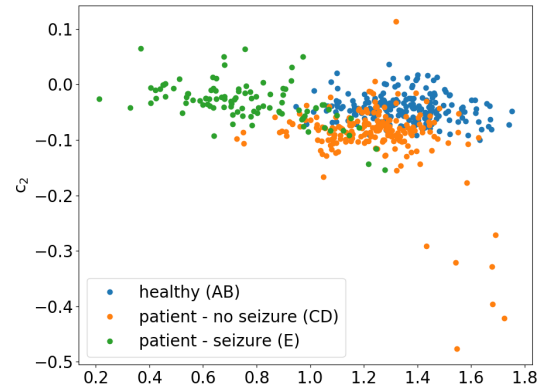


Fig. 3. Visualization of c_1 and c_2 for all time series in all sets A, B, C, D and E.

Table 1 shows the accuracy and the AUROC obtained for the classification of ABCD vs. E. Considering that the chance level accuracy of this problem is 80%, most feature sets perform well (accuracy $> 91.5\%$) when compared to chance. Using only c_1 and c_2 as features gives us a 94.37 % accuracy, compared to 93.57 % using only the peak-to-peak amplitude (feature set 4) and 96.87% using the peak-to-peak amplitude combined with the skewness, kurtosis and line length (feature set 5). When we add c_1 and c_2 to the features sets 4 and 5, the accuracy in both cases is increased to 97.03 (+3.46%) and to 97.40% (+0.53%), respectively. Although the accuracy and AUROC obtained with the feature set 5 (96.87% and 0.995) is not considerably increased when we add c_1 and c_2 (97.40% and 0.997), we obtain almost the same results with feature set 6 (97.03% and 0.994), which uses only c_1 , c_2 and the peak-to-peak amplitude, a very simple feature.

Table 2 shows the accuracy and AUROC obtained for the classification of AB (healthy subjects) vs. CDE (epilepsy patients). The chance level accuracy in this case is 60%, and we obtain a 84.90% accuracy and a 0.919 AUROC using c_1 and c_2 (feature set 3). With feature set 5 (peak-to-peak, skewness, kurtosis, line length) we obtain 88.40% and 0.959, which are increased to 92.57% (+4.17%) and 0.975 (+0.016) if we include c_1 and c_2 (feature set 7).

Table 1. ABCD vs. E - Accuracy and AUROC

Feature Set	Accuracy (%)	AUROC
1	91.53 ± 1.75	0.955 ± 0.017
2	79.37 ± 1.90	0.724 ± 0.033
3	94.37 ± 0.90	0.960 ± 0.025
4	93.57 ± 1.39	0.974 ± 0.008
5	96.87 ± 0.81	0.995 ± 0.002
6	97.03 ± 0.97	0.994 ± 0.005
7	97.40 ± 0.86	0.997 ± 0.002

Table 2. AB vs. CDE - Accuracy and AUROC

Feature Set	Accuracy (%)	AUROC
1	69.77 ± 1.91	0.774 ± 0.020
2	66.17 ± 2.30	0.727 ± 0.028
3	84.90 ± 1.75	0.919 ± 0.011
4	66.30 ± 1.43	0.724 ± 0.014
5	88.40 ± 3.27	0.959 ± 0.011
6	86.13 ± 1.90	0.934 ± 0.009
7	92.57 ± 1.97	0.975 ± 0.009

Table 3 shows the accuracy obtained for the classification of AB vs. CD vs. E³. The chance level accuracy in this case is 40%. Using c_1 and c_2 only, we obtain a 80.93% accuracy and 86.03% with feature set 5 (peak-to-peak, skewness, kurtosis, line length). With feature set 7, the accuracy is increased to 90.37% (+4.34% with respect to set 5).

Table 3. AB vs. CD vs. E - Accuracy

Feature Set	Accuracy (%)
1	61.13 ± 2.51
2	62.57 ± 1.99
3	80.93 ± 1.83
4	61.70 ± 2.06
5	86.03 ± 2.65
6	83.97 ± 1.70
7	90.37 ± 1.79

These results show that c_1 and c_2 perform well above chance when used to discriminate seizure versus non-seizure and healthy versus patient time series. Although feature set 5 (peak-to-peak, skewness, kurtosis, line length) performed better than the log-cumulants alone, c_1 and c_2 where shown to improve accuracy when combined to those features.

5. CONCLUSION AND PERSPECTIVES

Our results show that c_1 and c_2 , which are features that characterize the multifractal spectrum of a time series, are relevant for the detection of epileptic seizures as well as for dis-

criminating healthy volunteers from patients. These features can be seen as a way to summarize the dynamics of time series: c_1 represents the overall regularity of the signal while c_2 measures the variability around this global regularity. This suggests that the neural dynamics summarized by c_1 and c_2 can be modulated by seizure (ictal) activity and can be also different between healthy subjects and epileptic patients. Future work should investigate whether these conclusions can be extended to other data sets and whether we can propose computational neuroscience models that explain the modulation of multifractal properties, aiming to better understand the neural dynamics involved in epilepsy.

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³The AUROC was not computed for this multiclass classification problem.