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Optimization of sequential administration of bevacizumab plus cytotoxics in non-small cell lung cancer by combining in vivo experiments and mathematical modeling

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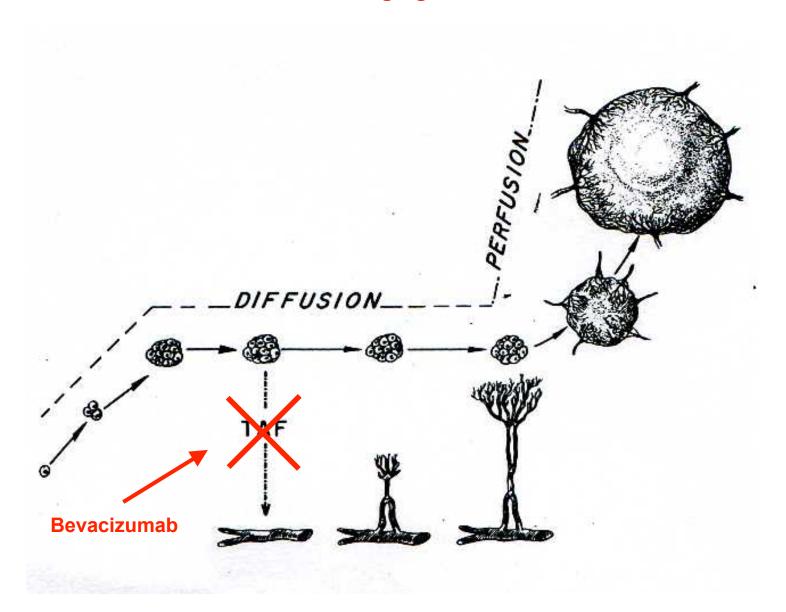
Mathematical perspectives in the biology and therapeutics of cancer

July 11, 2018



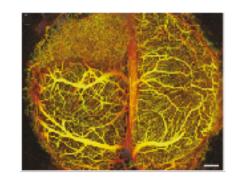


Angiogenesis



Vascular normalization: a time window for improved pharmacokinetics?

- Bevacizumab = anti-VEGF monoclonal antibody ⇒ anti-angiogenic action (first approved in 2004)
- Only proved clinical efficacy when combined (concomitantly) with cytotoxics
- Possible explanation: transient normalization of the otherwise abnormal (leaky, tortuous) vascular architecture



Vakoc et al., Jain, 2009, Nat Med

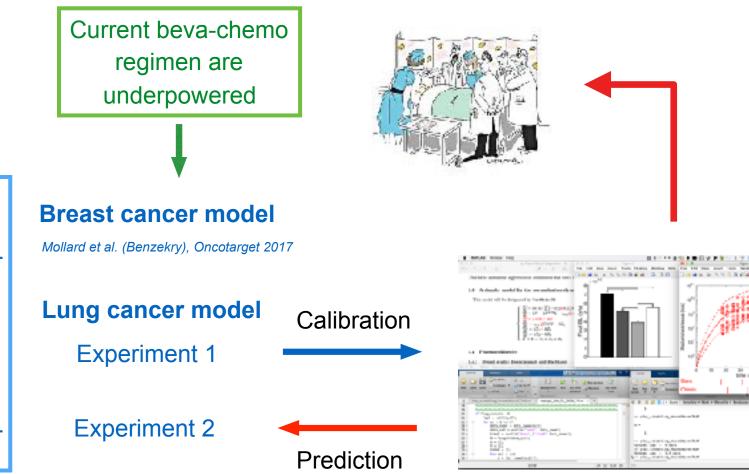


Jain, Nat Med, 2001

Question

What is the **optimal time gap** between administration of bevacizumab and cytotoxic chemotherapy? How to capture **inter-individual variability** for designing **personalized** therapies?

Hypothesis: sequential use of bevacizumab associated with chemotherapy would achieve better efficacy and modeling support could help to define the optimal timewindow



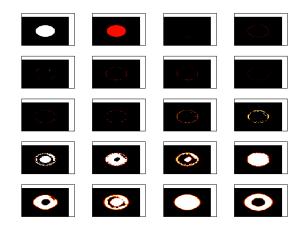
Modeling

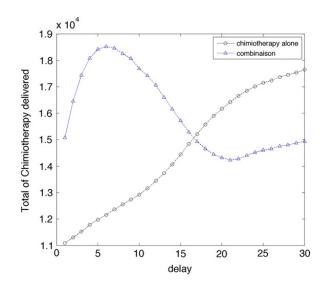
Simulation

A first theoretical and complex model

Entity	Model equation
Density of P_1	$\frac{\partial P_1}{\partial t} + \frac{\partial P_1}{\partial a} + \nabla \cdot (\mathbf{v}_{\mathbf{P}_1} P_1) = 0 \ P_1(a = 0) = 2P_2(a = a_{max, P_2})$
Density of P_2	$\frac{\partial P_2}{\partial t} + \frac{\partial P_2}{\partial a} + \nabla \cdot (\mathbf{v}_{\mathbf{P}_2} P_2) = -P_2(a = a_{max,P_2} \frac{E_{max,C}[C]}{C_{co} + [C]} P_2(a = 0) = fP_1(a = a_{max,P_1}) + [\partial_t f]^+ Q(t^-)$
Density of Q	$\frac{\partial Q}{\partial t} + \nabla \cdot (\mathbf{v_Q} Q) = \mathbf{g}(1 - f)P_1(a = a_{max, P_1}) - \left[\frac{\partial f}{\partial t}\right]^+ Q(t^-) + \left[\frac{\partial g}{\partial t}\right]^- Q(t^-)$
Density of A	$\frac{\partial A}{\partial t} + \nabla \cdot (\mathbf{v_A} A) = (1 - g) P_1(a = a_{max, P_1}) - \left[\frac{\partial g}{\partial t}\right]^{-} Q(t^{-})$
Density of H	$\frac{\partial H}{\partial t} + \nabla \cdot (\mathbf{v}_H H) = 0$
Density of mature vessel cells	$\frac{\partial Es}{\partial t} = \mu \mathcal{H}(E + Es - \tau_E)E - a_{ES}Es$
Density of immature vessel cells	$\frac{\partial E}{\partial t} + \nabla \cdot (\chi E(1 - \frac{E}{N_E}) \nabla [V]) = pE \left(1 - \frac{E + Es}{N_E}\right) - a_E E - \mu \mathcal{H}(E + Es - \tau_E) E$
Quality of the vasculature	$R = \frac{\int E}{Vol} \Pi = 1 - \frac{R^{v_n}}{R^{v_n} + R^{v_n}_{v_n}},$
Concentration of oxygen	$-\nabla (K_{[O_2]}\nabla [O_2]) = -\sum_{\phi} \alpha_{[O_2],\phi} \phi \ [O_2] = \Pi C_{max}$ where $Es \ge \tau_{\nu}$
Concentration of VEGF	$\frac{\partial [V]}{\partial t} - \nabla \cdot (K_{[V]} \nabla [V]) = \alpha_{[V]} Q_{[0_2] \le \tau_{1,h}} - \beta_{[V]} E[V] - \delta_{[V]} [V] - [V] \frac{Emax_{[AA]} [AA]}{[AA]_{50} + [AA]}$
Concentration of chemo.	$-\nabla \cdot (K\nabla[C]) = -\xi_{[C]}[C] [C] = \prod P_{[C]}(t) \text{ where } Es \ge \tau_v$
Concentration of antiangiogenic	$-\nabla \cdot (K\nabla[AA]) = -[V] \frac{Emax_{[AA]}[AA]}{\nu_{50} + [AA]} [AA] = \Pi P_{[AA]}(t) \text{where } Es \ge \tau_{\nu}$

Parameter	Description	Value	Unit
τ_0	Threshold of overcrowding	5 × 10 ⁴	cell
$\tau_{1,h}$	Threshold of moderate hypoxia	4×10^{-7}	M
$\tau_{2.h}$	Threshold of severe hypoxia	4×10^{-9}	M
N _{max}	Total density of tumor and/or healthy cells	10 ⁵	cell
$a_{max.P}$,	Maximum duration of phase P_1	5	time-unit
a_{max,P_2}	Maximum duration of phase P_2	8	time-unit
$\alpha_{[V]}$	Secretion rate of VEGF by quiescent cells	10^{-8}	M/cell
$\delta_{[V]}$	Consumption rate of VEGF by immature endothelial cells	0	M/cell
ξ _[V]	Degradation rate of VEGF	0	M^{-1}
N _E	Maximum number of endothelial cells	10 ⁵	cell
μ	Rate of maturation for endothelial cells	0.5	cell/time-unit
τ _Ε	Minimis quantity of immature EC leading to maturation	5×10^2	cell
γ_n	Sigmoidal coefficient for the computation of vasculature quality	0.5	cell/mm ²
R _{0.5}	Density of EC leading to half of the maximal vasculature quality	8×10^{-3}	cell/mm ²
τ_v	Number of EC needed to form a functional blood vessel	4×10^4	cell
C _{max}	Oxygen concentration in blood	2×10^{-2}	M
K	Diffusion coefficient of molecules in the tissue	1-5	mm ² /time-unit
$\beta_{[O_2], P_1}$	Oxygen consumption of the P_1 tumor cells	10^{-4}	M/cell
$\beta_{[O_2], P_2}$	Oxygen consumption of the P_2 tumor cells	10^{-4}	M/cell
$\beta_{[0_2], Q}$	Oxygen consumption of the quiescent tumor cells	0.25×10^{-4}	M/cell
, _[02] , ξ ζ[c]	Degradation rate of chemotherapy	1.25×10^{-4}	M/time-unit
Emax _[AA]	Maximal effect of the antiangiogenic drug on VEGF	1	None
v_{50}	Amount of antiangiogenic drug producing half of the maximal effect	0.5	M
E _{max, C}	Maximal effect of the chemotherapy on P_2 cells	0.75	None
C ₅₀	Amount of chemotherapy producing half of the maximal effect	0.2	M





Lignet, Benzekry et al. (Ribba), J Theor Biol, 2013

Simplified model for the anti-angiogenic therapy: the Hahnfeldt-Folkman approach

$$\begin{cases} \frac{dV}{dt} = aV \ln\left(\frac{K}{V}\right) \\ \frac{dK}{dt} = bV - dV^{2/3}K - eA(t)K \end{cases}$$

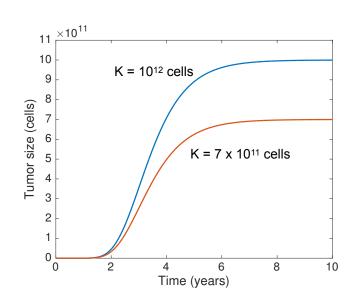
Hahnfeldt-Folkman effect: K = f(A(t))

Dynamics of *K* are governed by a balance between **angiogenic stimulation and inhibition** (both endogenous and exogenous)

Vasculature = carrying capacity

neo-angipgenesis

Dynamical carrying capacity K(t)

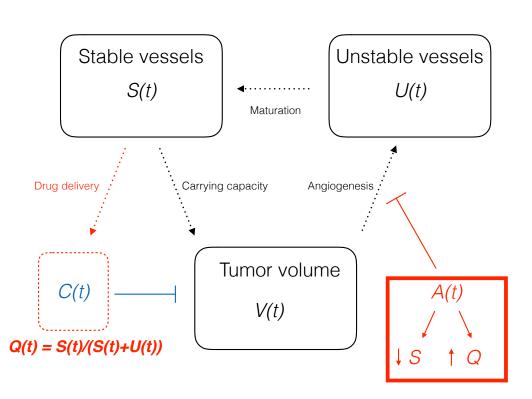


Modeling the combination of chemotherapy and bevacizumab

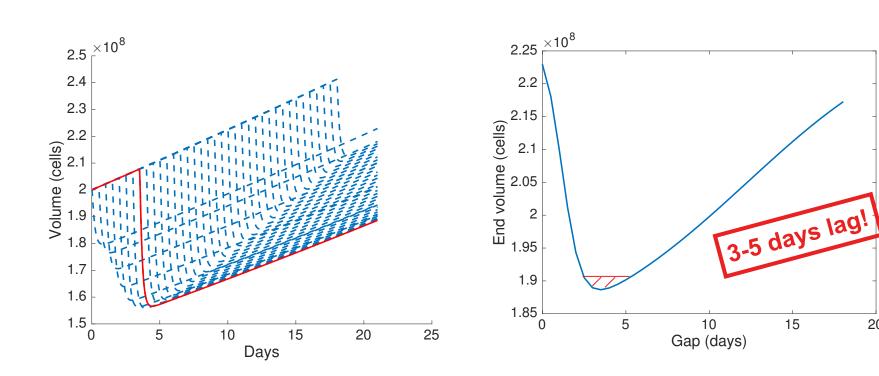
Idea: define a dynamical index of quality of the vasculature **Q** by dividing the vasculature into **stable** and unstable compartments

$$\begin{cases} \frac{dV}{dt} = aV \ln\left(\frac{S}{V}\right) - e_{CT}QSC(t)V \\ \frac{dU}{dt} = bV - dV^{2/3}U - \chi U - e_{AA}QSA(t)U \\ \frac{dS}{dt} = \chi U - \tau S \end{cases}$$

$$Q = \frac{S}{S + U}$$



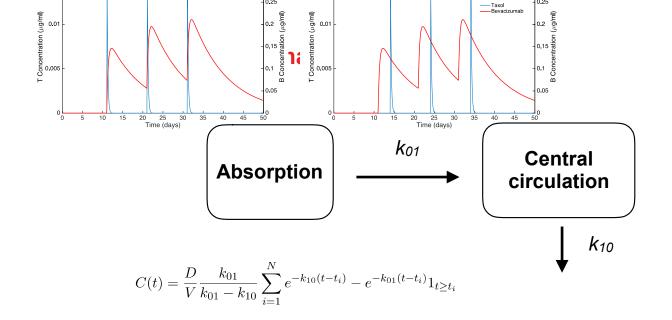
A priori simulations of the model suggest optimal sequence

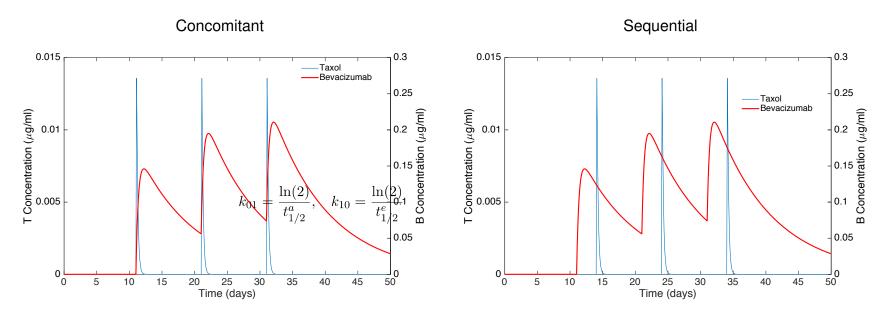


Anti-angiogenics first, then cytotoxics

15

20



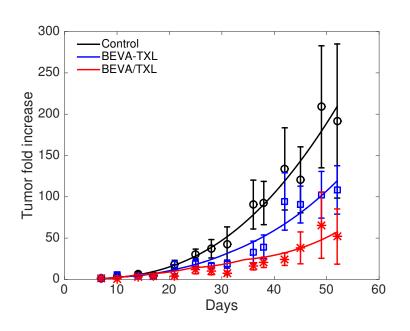


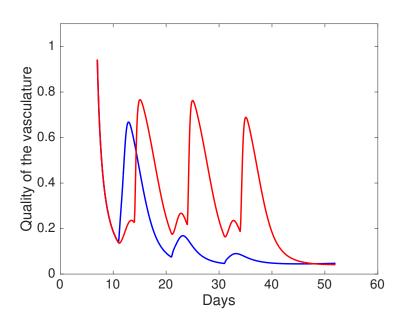
Innocenti F. et al., Drug Metab Dispos Biol Fate Chem, 1995

Lin et al., J Pharmacol Exp Ther. 1999

TXL I I I I TXL I I I

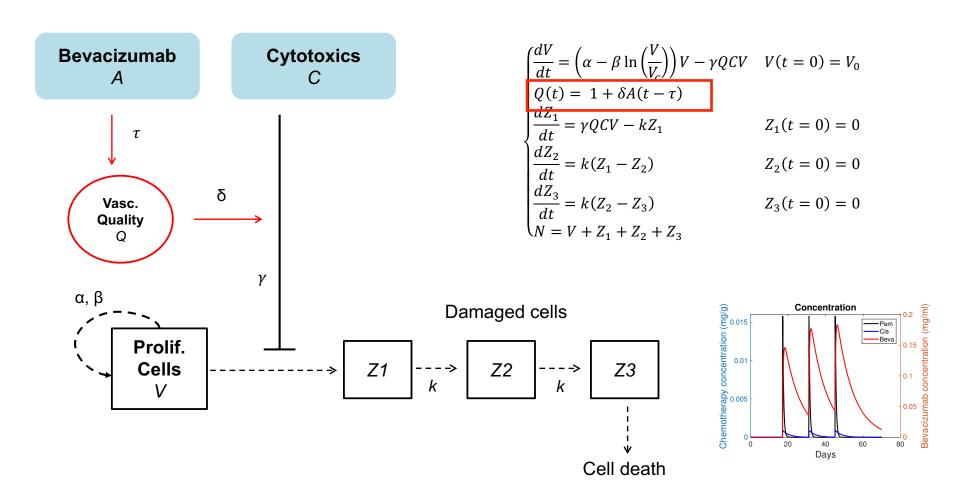
Confrontation to experimental data





Par.	Unit	Estimate	SE (%)		
a	day-1	0.0703	0.0328		
b	day-1	86.8	463		
d	day-1	0.0745	0.508		
χ	day-1	0.00203	0.0164		
τ	day-1	0	-		
U_0	-	5	50.5		Identifiability issues
S_0	-	82.4	116	_	
$e_{_{\mathrm{TXL}}}$	ml·mg ⁻¹ ·day ⁻¹	13.9	84.3		
k	day-1	8.45x10 ⁻⁹	0.552		
$e_{_{\mathrm{BEVA}}}$	ml·mg ⁻¹ ·day ⁻¹	0.494	2.73		

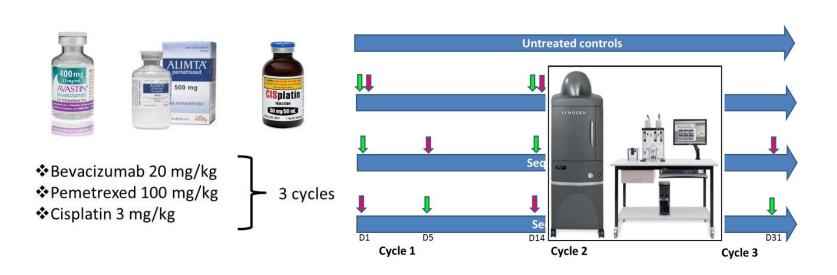
Semi-mechanistic mathematical model



Simeoni et al., Rocchetti, Cancer Res, 2004 Imbs et al., Benzekry, CPT: Pharmacometrics Syst Pharmacol, 2018

+ PK models for beva A(t) and CT C(t) concentrations

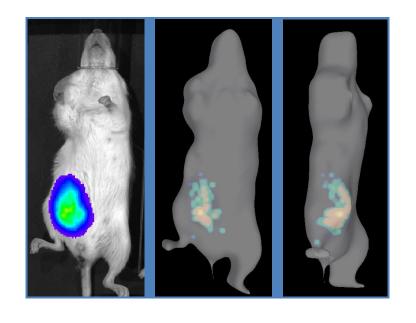
Tumor volume
$$\frac{dS}{dt} = vV - dV + C - \chi C - \epsilon_{AA} \otimes A(t) + C - \chi C - \chi C - \epsilon_{AA} \otimes A(t) + C - \chi C - \chi C - \epsilon_{AA} \otimes A(t) + C - \chi C - \chi C - \epsilon_{AA} \otimes A(t) + C - \chi C -$$



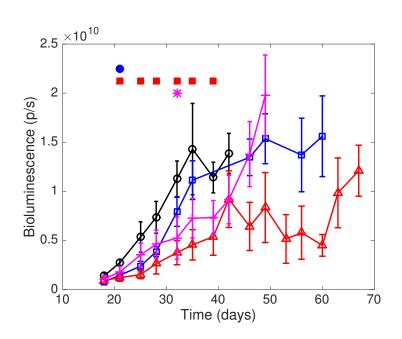
- **Human NSCLC** H460-Luc+ xenograft
 - Subcutaneous graft

Q(t) = S(t)/(S(t) + U(t))

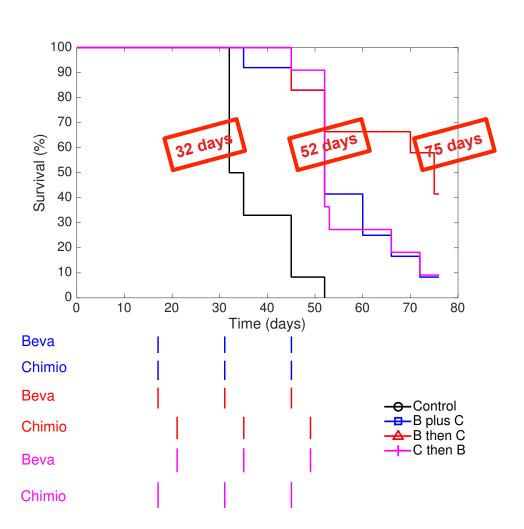
- Matrigel support
- Follow-up
 - Bioluminescence imaging
 - Weight monitoring



Sequential administration Beva then Chemo improves response and survival



-71.2% tumor size at study conclusion (day 60)



⇒ Sequential use increases survival by 44%

Population approach for model calibration: nonlinear mixed effects modeling

Classical nonlinear regression considers each time series independently

$$Y_i^j = M(t_i^j, \beta^j) + \varepsilon_i^j, \quad \varepsilon_i^j \sim \mathcal{N}(0, \sigma_i^j)$$

$$\text{Individual } 1 \leq j \leq N$$

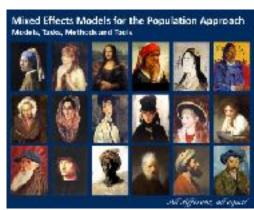
$$\hat{\beta}^j = \min_{\beta} \sum_{i=1}^{n} \left(y_i^j - M(t_i^j, \beta) \right)^2$$

$$\text{Time } t_i$$

 When only sparse data are available from subjects in the same population, one can fit the parameters distribution all-in-once

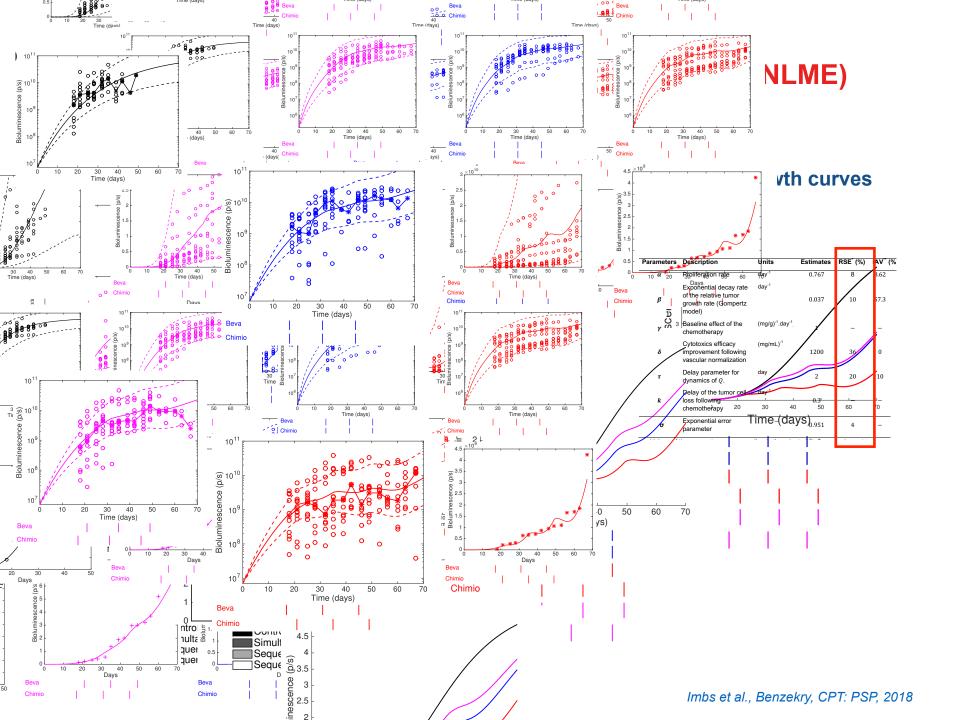
$$Y_i^j = M(t_i^j, \beta^j) + \varepsilon_i^j$$

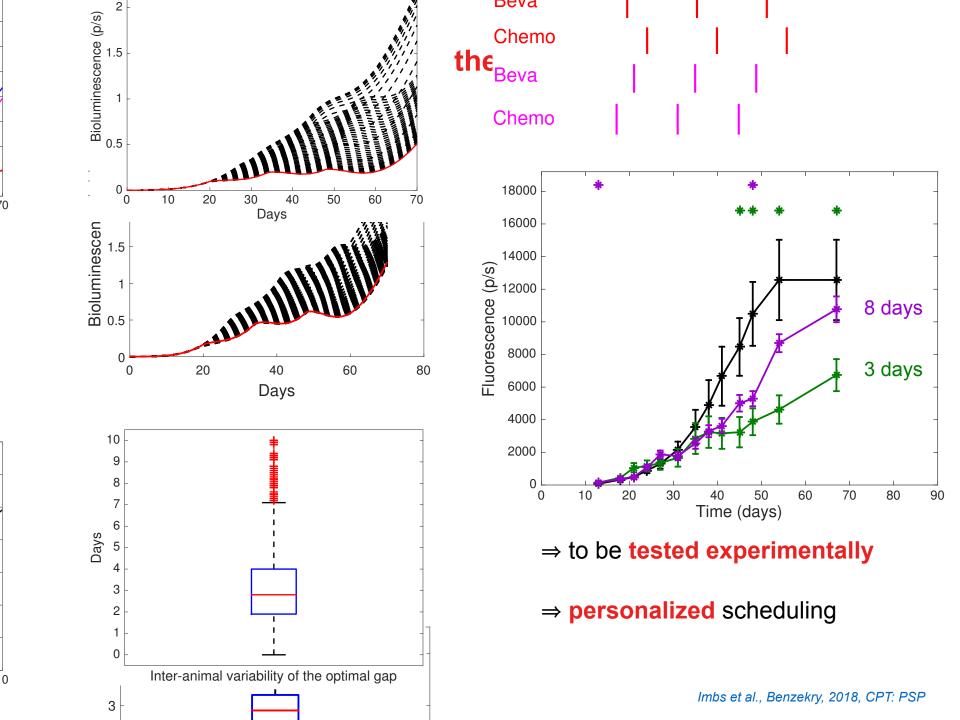
$$\beta^1, \ldots, \beta^N \sim \mathcal{LN}(\beta_\mu, \beta_\omega), \quad \beta_\mu \in \mathbb{R}^p, \ \beta_\omega \in \mathbb{R}^{p \times p}$$



Lavielle, CRC press, 2014

Reduces the number of parameters from pxN to p+p²





Conclusion

- In order to be confronted to empirical data and yield robust predictions, mathematical models must remain simple and well dimensioned with the data
- Mathematical modeling can be used to identify optimized drug regimen for combination therapies among a large number of scenarios that cannot be all tested experimentally
- This is of increasing relevance in modern oncology where an always larger arsenal of anticancer agents becomes available to oncologists (cf. immune-oncology in combination)
- Nonlinear mixed-effects modeling is a powerful statistical approach for pooling together population data that arise from studies in experimental and clinical oncology
- Subsequent patient-specific bayesian estimation of the parameters can be used for personalized scheduling



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Translational/Bench



Dr. J. Ciccolini



S. Giacometti Dr. S. Mollard



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