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Velocity-Pressure Loops for continuous assessment of ventricular afterload: Influence of pressure measurement site

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Authors' contribution

JJ, F.V., A.L.G., E.G., and A.Me. conception and design of research; F.V., A.L.G., O.P., J.M. and J.J. performed experiments; E.G. and A.L.G. analyzed data; A.L.G. and E.G. interpreted results of experiments; E.G., A.L.G. and SM prepared figures; F.V., A.L.G., E.G. and A.Me. drafted manuscript; F.V., A.L.G, E.G., and S.M edited and revised manuscript; F.V., A.L.G., J.J., O.P., J.M., S.M., A.Me. and E.G. approved final version of manuscript. JJ and FV equally contributed to this present study.

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Abstract

Purpose

VPloop, the graphical representation of pressure versus velocity, and its characteristics angles, GALA and β , can be used to monitor cardiac afterload during anesthesia. Ideally VPloop should be measured from pressure and velocity obtained at the same arterial location but standard of care usually provide either radial or femoral pressure waveforms. The purpose of this study was to look at the influence of arterial sites and the use of a transfer function (TF) on VPloop and its related angles.

Methods

Invasive pressure signals were recorded in 25 patients undergoing neuroradiology intervention under general anesthesia with transesophageal flow velocity monitoring. Pressures were recorded in the descending thoracic aorta, abdominal aorta, femoral and radial arteries. We compared GALA and β from VPloops generated from each location and in high and low risk patients.

Results

GALA was similar in the central locations (55° [49-63], 52° [47-61] and 54° [45-62] from descending thoracic to femoral artery, median[interquartile], $p=0.10$), while there was a difference in β angle (16° [4-27] to 8° [3-15], $p<0.0001$). GALA and β obtained from radial waveforms were different (39° [31-47] compared to 46° [36-54] and 6° [2-14] compared to 16° [4-27] for GALA and β angles respectively, $p<0.001$) which was corrected by the use of a TF (45° [32-55] and 17° [5-28], $p=ns$).

Conclusion

GALA and β are underestimated when measured with a radial catheter. Using pressure waveforms from femoral locations alters VPloops, GALA and β in a smaller extend. The use of a TF on radial pressure allows to correctly plot VPloops and their characteristic angles for routine clinical use.

Keywords: flow velocity, arterial pressure, left ventricular function, afterload, anesthesia, cardiac output,

Introduction

During general anesthesia, hypotension episodes are common events and have multiple, sometimes intricate causes like hypovolemia, hemorrhage, acute cardiac dysfunction or vasodilation. The latter is often due to anesthetic drugs. These events result in reduced organ perfusion and may affect the heart, the brain or the kidneys, increasing therefore peri-operative morbidity and mortality (1,2).

Consequently, current guidelines (3,4) emphasize a global approach to assess and treat hemodynamic risks including : (I) Preoperative evaluation of individual risk factors (preoperative consultation, use of prognostic scores, evaluation of surgical risk), (II) Hemodynamic optimization during surgery, and (III) fast post-operative recovery. To achieve this, scientific societies recommend, for high-risk patients, the use of continuous hemodynamic monitoring of invasive arterial pressure and cardiac output for a personalized patient approach and better care during surgery.

With an invasive arterial line associated with a trans-esophageal Doppler, our team was able to develop Velocity-Pressure (VP) loops which allow integrative analysis of aortic flow velocity (V) and pressure (P) (5,6). The VP Loops are the graphical representation of the pressure and velocity during one heart beat and are directly related to ventricular afterload and its different components : resistance, compliance and stiffness (6). Two remarkable angles, called β and GALA (Global AfterLoad Angle), were defined from the VP Loops and are described in figure 1. [Following the concept of arterial reflection waves, the \$\beta\$ angle corresponds to the beginning of the backward aortic wave and could be considered a marker of arterial stiffness \(19\). The GALA angle characterizes pressure-velocity relationship at peak systolic pressure and should be considered a global and integrative estimation of afterload.](#) These two angles can be used to identify patients with cardiovascular risk factors and are greatly modified by vasopressors (5,6).

In this previous study, arterial pressure was measured in the descending abdominal aorta just above the iliac bifurcation from the standard of care 20cm-long femoral catheter. It has been however largely shown that arterial pressure waveforms and values can be considerably different depending on arterial measurement sites (7). Due to wave propagation, reflection and Windkessel effect, there is a wave amplification phenomenon as the pressure waveform travels further away from the heart (8–10), resulting in higher systolic blood pressure (SBP) as well as very slightly reduced diastolic (DBP) and mean blood pressure (MBP) at the periphery. Systolic pressure amplification is not negligible and has varying magnitude across patient population (8). Several studies have shown that central aortic pressure is a stronger predictor of cardiovascular morbidity and mortality than peripheral pressure (11). This phenomenon is also likely to influence the shape and angles of VP Loops, especially if the pressure is measured at the peripheral level such as at the radial artery.

Ideally, VP Loops should be built from velocity and pressure waveforms measured at the same arterial site. However invasive measurements of thoracic aortic pressure are not possible in everyday procedures. During routine anesthesia, the most used invasive pressure site is the radial artery. Femoral access is also common to a lesser extent. The aim of this study was to assess the influence of pressure measurement site on VP Loops, β and GALA angles by comparing VP Loops obtained from invasive radial pressure, from invasive aortic pressure and from reconstructed aortic pressure obtained by applying a transfer function on peripheral pressure.

Material and Methods

Population

Between January 2015 and March 2016, patients scheduled for elective or emergency neuroradiology intervention under general anesthesia in our department were screened for this

prospective observational study. Patients were included if their perioperative risk required an invasive arterial line as well as cardiac output monitoring. Patients less than 18 years old, pregnant women and patients who refused to provide informed consent were not included. The study protocol was approved by the research ethics committee (CE SRLF 11-356).

Data collection

Patient demographic data was collected during the preoperative consultation. Hydroxyzine (1 mg/kg) was administered orally, one hour before the interventional neuroradiology procedure. General anesthesia was induced and maintained with Propofol (75-150 µg/kg/min) and Remifentanyl (0,2-0,5 µg/kg/min). All patients were intubated after paralysis with Atracurium (0,5 mg/kg) and mechanically ventilated with a tidal volume of 6 ml/kg. Respiratory rate was adjusted in order to obtain an EtCO₂ between 35 and 38 mmHg. Radial artery was then cannulated and esophageal Doppler probe CardioQ-ODM+ (Deltex Medical, Chichester, UK) was inserted through the mouth. Position and gain of the Doppler probe were adjusted according to manufacturer instructions to obtain maximal peak velocity and best Doppler spectrum definition respectively. During their interventional neuroradiology procedure, all patients had standard of care monitoring consisting of ECG, heart rate, pulsated oxygen saturation (SpO₂), non-invasive cuff blood pressure, as well as end tidal CO₂, respiratory rate, tidal volume. Administration of fluids and vasoconstrictors was decided by the physician in charge based on patient needs and independently of the study.

Cardiac output monitoring

Cardiac output was measured using the transesophageal Doppler CardioQ-ODM+ (Deltex Medical, Chichester, UK) which measures instant blood velocity in the descending thoracic aorta from a continuous Doppler probe inserted inside the esophagus. Blood velocity is closely related to blood

flow via the formula $Q(t) = V(t) * A(t)$ where $Q(t)$ is blood flow as a function of time, $V(t)$ is blood velocity as a function of time and $A(t)$ is the aorta cross section as a function of time. Stroke volume (SV) and cardiac output (CO) are then calculated from the beat to beat measure of blood flow and an approximation of $A(t)$ proprietary to Deltex incorporating patient demographics. In this study, we used digitalized continuous raw velocity $V(t)$ data.

Radial and aortic pressure measurements

A radial intra-arterial catheter (SAC 00520 20GA, Arrow International, Reading, PA, USA) was used to record SBP, DBP, MBP values and to collect raw continuous pressure waveforms during the entire procedure. As required by the standard of care of the interventional neuroradiology procedure, the neuroradiologist also cannulated the femoral artery using the Seldinger technique and inserted a catheter (Mach1 5F, Boston Scientific, Marlborough, MA, USA) through an 5 cm-introducer (Radiofocus Introducer II 6F, Terumo Europe, Leuven, Belgium). The radial and aortic catheters were connected to the same type of pressure transducer (TruWave, Edwards Lifesciences, Irvine, CA, USA). Both transducers were placed at the same medio-thoracic level. The femoral catheter was advanced through the aorta up to the intracranial arteries in order to complete the programmed intervention. At the end of the procedure, during catheter withdrawal, pressure waveforms were recorded at 3 predefined aortic locations: in the descending thoracic aorta just in front of the esophageal Doppler probe, in the abdominal aorta at the level of the renal arteries (as in our previous study (6)) and in the femoral artery just outside the introducer. At each location, we obtained 15 to 20 seconds of simultaneous invasive aortic pressure, esophageal Doppler flow velocity and invasive radial pressure signals. During signal acquisition, no surgical stimulation occurred, no change of anesthetic drug regiments was performed, no vasoconstrictor was administered and no ventilatory maneuver was conducted in order to have hemodynamic stability.

VP Loop Construction

Digitalization of pressure and esophageal Doppler signals was performed with the IntelliVue MP60 monitor (Philips, Eindhoven, The Netherlands) at a sampling frequency of 125 Hz and saved using ixTrend software (ixellence, Wildau, Germany) on a computer. Due to electronic within the equipment, there was a variable time delay between pressure and flow velocity signals. To plot VP Loops, pressure and velocity need to be synchronized so we developed a method to automatically detect the beginning of the cardiac cycle based on the local maxima of the second pressure derivative (d^2P/dt^2_{\max}) (13) and inspired by ECG cycle detection algorithm (14). After re-alignment, VP Loops were plotted for each time point of the whole cardiac cycle. β and GALA angles were calculated as explained previously (6) and shown on figure 1. In short, β angle represents the angle between the lines from the onset of pressure and flow (point A on figure 1) to the point of maximal flow (point B) and the point of maximal pressure (point C). GALA is defined from the angle formed by the line from the beginning of the heartbeat (point A) to the peak pressure (point C) with the horizontal line. It represents a global estimation of ventricular afterload (6).

VP Loops constructed from descending thoracic aorta (and noted VP Loop_{ref}) were chosen as the reference as they were plotted from pressure waveforms recorded at the same arterial location than velocity recording. VP Loops obtained from radial, abdominal or femoral pressure waveforms were respectively called VP Loop_{rad}, VP Loop_{abd} and VP Loop_{fem}.

Radial to thoracic transfer function

From the data of the 22 patients with simultaneous radial and descending thoracic pressures signals, we generated a transfer function (TF) using a similar method as described previously (7,14,15). We used an auto-regressive filter to mathematically transform the invasive radial waveform into descending

thoracic waveforms. Calculations relative to the transfer function were done using Matlab 8.5 (The MathWorks, Inc., Natick, MA, USA). VP Loops obtained from radial waveforms with transfer function were called VP Loop_{TF}.

Statistical Analysis

Patients included in the study were separated into two groups according to their cardiovascular risk factors (CVRF): low risk (LR) patients presented no or only 1 CVRF. High risk (HR) patients were patients with at least 2 CVRF. The following CVRF were considered: age > 55 years, active smoking, hypertension, dyslipidemia, diabetes mellitus, history of myocardial infarction [16,17].

Statistical analysis was performed using GNU R(19). Continuous variables were expressed as median [interquartile range]. Qualitative variables were expressed as n (%). P-value less than 5% was considered significant. Angles of VP Loop_{rad}, VP Loop_{abd} and VP Loop_{fem} and VP Loop_{TF} were compared to angles obtained from VP Loop_{ref} using a paired Wilcoxon signed-rank test.

Results

Population

Forty-five consecutive patients were included in this study. Ten patients were excluded because monitoring of the invasive aortic pressure could not be obtained due to technical difficulties. Three patients were excluded because they were subject to significant hemodynamic modifications during the procedure as defined by a mean blood pressure variation greater than 10%. Four patients were excluded because the quality of the esophageal Doppler signal was insufficient. Three patients waived consent. The characteristics of the remaining 25 patients are shown in table 1. Ten belonged to the low

cardiovascular risk (LR) group and 15 belonged to the HR group. Two patients from the LR group and one patient from the HR group did not have an invasive radial artery line.

VP Loop_{ref} Angles

The VP Loops obtained with pressure and flow measured in the descending thoracic aorta were used as reference in our study. In the entire population of 25 patients, GALA angle was of 46° [36-54] and β angle was of 16° [4-27]. HR patients had GALA and β angles significantly higher than those of LR patients: 55° [49-63] vs 38° [23-45] and 27° [20-36] vs 5° [1-14], $p < 0.0001$ for GALA and β respectively.

VP Loop_{ref} versus VP Loop_{abd} and VP Loop_{fem} comparison

In the whole population, GALA was similar on VP Loops constructed from descending thoracic aorta, abdominal aorta or femoral artery (55° [49-63], 52° [47-61] and 54° [45-62] for descending thoracic, abdominal and femoral artery respectively, $p = 0.10$, table 2). There was however a significant difference on β angle which was getting smaller as we progressed from descending thoracic to femoral artery (16° [4-27] to 8° [3-15], $p < 0.0001$). When decomposing into LR and HR groups, GALA was similar wherever the location of central pressure line used for VP Loops construction (table 2). β angle was significantly smaller when measured from VP Loop_{fem} than from VP Loop_{ref} and this difference was greater in the HR group than in the LR group (Table 2).

VP Loop_{ref} versus VP Loop_{rad} comparison

In the whole population, GALA and β angles were significantly smaller when VP Loops were plotted using radial artery pressure rather than descending thoracic pressure (39° [31-47] vs 46° [36-54], $p < 0.0001$ for GALA and 6° [2-14] vs 16° [4-27], $p < 0.0001$ for β). These differences hold true

when HR and LR group were taken separately. However, the difference was greater in the HR group compared to the LR group (Table 3). Graphical representation of the changes in VP Loops due to the use of descending thoracic aortic or radial pressure are shown on Figure 2 and 3.

VP Loop_{ref} versus VP Loop_{TF} comparison

As the use of radial waveforms was not suitable to correctly render VP Loop_{ref}, we calculated a transfer function to “transform” radial pressure waveforms into descending thoracic pressure waveforms. Radial line was unavailable in 3 of the patients of the cohort, so the TF was calculated from the remaining 22 subjects with simultaneous recording of descending thoracic and radial pressures. Upper panels of figure 2 and 3 show examples of reconstructed descending thoracic waveform in a LR and in a HR patient. Reconstructed waveform provided good estimation of the reference descending aorta waveform leading to similar VP Loop_{ref} and VP Loop_{TF} (figure 2 and 3, lower panel). While there are significant differences between GALA and β angles from VP Loop_{ref} and VP Loop_{rad} (7 [4 – 11] $^{\circ}$ and 10 [3 – 14] $^{\circ}$, $p < 0.001$ for GALA and β respectively), using the TF provided GALA and β angles similar to the descending aorta reference (1 [-2 – 1] $^{\circ}$ and 1 [0 – 3] $^{\circ}$, $p =$ NS for GALA and β respectively). This observation holds true whatever patient risk (Table 3).

Discussion

The results of this study show there are differences in GALA and β angles values whether the VP Loop is built using a radial pressure waveform rather than a pressure waveform measured in the descending thoracic aorta. Conversely, the changes in GALA and β angles along the aorta were smaller with significantly no changes for GALA. Construction of VP Loop from radial artery pressure results in an under-estimation of both GALA and β angles. This under-estimation is greater in patients with higher cardiovascular risks.

Cardiac afterload depends on arterial compliance, wave reflections and vascular tone (7) but it is difficult to monitor each of these parameters in real time during procedures. To simultaneously interpret both of pressure and flow velocity waveforms, we propose to plot them on the same graph across the cardiac cycle (5,6). The resulting VP Loops provides graphical representation of afterload. To numerically describe these loops, we defined the β and GALA angles (6). These angles are related to arterial stiffness, peripheral vascular compliance and to parameters such as the augmentation index which represents the contribution of reflected waves on pressure waveforms (6). In our previous study we observed different VP Loops in patients with low and high cardiovascular risks. Our present results confirm the previous ones, as both GALA and β angles were increased in the HR risk group. In other terms, high risk population leads to a counterclockwise rotation of the VP Loop axis as well as a widening of the loop.

Previously (6), we plotted VP Loops using pressure waveforms acquired from the standard central monitoring line i.e. from fluid filled catheter positioned in the abdominal aorta, just above the iliac bifurcation using a 20cm long femoral line. As pressure waveforms are greatly influenced by measurement site, there were concerns that these VP Loops might not reflected “gold standard” VP Loops: VP Loops plotted from flow velocity and pressure signals acquired both at the same location point. In the present study, we measured arterial pressure from the central line on 3 aortic points: at the

descending thoracic aorta (= the reference point), at the abdominal aorta (as in our previous study) and at the femoral artery. We did not observe any significant differences VP Loop for GALA angles at the abdominal aorta and at the descending thoracic aorta. These results confirmed that GALA can be measured and used from VP Loops obtained from standard of care aortic line, without the need to properly align the esophageal Doppler probe and the pressure catheter. However, β angle varied to a greater extent along the aorta. Further studies are required to fully conclude if these differences are clinically relevant.

The second objective of our study was to see if radial pressure waveforms could also be directly used to plot VP Loop. Such setting have been used by Thiele and coworkers (20). However waveforms as well as systolic pressure can vary a lot between the aortic root and the radial artery (7,21). As the pressure pulse propagates from the heart to the periphery, its peak (i.e. systolic pressure) increases while the waveform becomes “narrower”. This phenomenon is called pressure amplification and varies across age, gender and diseases(22). Reference ranges have been published and the average pressure amplification being about 10mmHg (8). In the present study, we simultaneously measured radial pressure, descending thoracic pressure and descending thoracic flow velocity. The mean pressure amplification between thoracic and radial systolic pressure was 2 ± 11 mmHg (data not shown). This relatively low amplification value can be explained by our population characteristics which mainly included patients with 2 or more cardiovascular risk (60% were high risk patients), The measurement site, descending thoracic instead of ascending aortic pressure used in previous papers (23,24), could also play a part. When we compare VP Loops constructed from radial pressure to VP Loops constructed from the “reference” descending aortic pressure, we observed marked difference with a clockwise tilt of the waveform. This is reflected on β and GALA angles which are underestimated when using radial waveforms. The difference on VP Loop morphology was even greater in patients in

the higher cardiovascular group while this is the group in whom we particularly wish to closely monitor cardiac afterload (25,26).

For over two decades, a methodology called general transfer function has been used to estimate central pressure from peripheral pressure (7,14,15). It has been first commercialized into the SphygmoCor device (AtCor Medical, Australia) followed by other manufacturers. The general TF approach has been extensively validated in coronary patients and can correctly estimate central systolic pressure value (23,24). There has been however some reserve about the accuracy of the general TF approach to render some high fidelity details such as the augmentation index (27). Existing TF are proprietary to the commercial device and depend on the input sensor. What is more they are all designed to estimate ascending aortic pressure. We hence calculate our own TF to be able to estimate descending aortic pressures from invasive radial waveform. As all signals were measured invasively, calibration was not an issue. Our results showed it is possible to apply a transfer function to reasonable accuracy for the construction of VP Loops and calculation of GALA and β angles. GALA and β angles obtained using the TF were similar to the ones obtained from the reference descending thoracic aorta.

Limits

The main limits of this study are related to the studied population and measurement techniques. Invasive pressure waveforms were measured using a fluid filled catheter as opposed to micro-manometer sensors which are considered gold standard. Artifacts from the fluid filled line are possible and have been described (28). Using high fidelity transducers might modify the VP Loop definition but we feel that would be negligible as long as great care is taken while handling fluid-filled catheters.

Patients included in this study had invasive measurements because their peri-operative risk required it. However, none presented acute decompensated heart failure or shock. It would be interesting to study VP Loops from the various aortic locations in this particular population where accurate hemodynamic monitoring is particularly useful.

We defined a TF from our cohort, Additional studies are required to refine it and test the TF approach during anesthesia on a larger population.

As opposed to our previous work, we did not measure VP Loop changes induced by vasopressor and fluid challenges (6). Indeed, we focused on stable hemodynamics to obtain comparable measure points along the aorta. Additional studies are needed to confirm our findings during vasopressors challenges.

And finally, as no sample size calculation was performed, the non-significance of certain results could be due to lack of power. Our results need to be confirmed in a larger cohort study.

Conclusion

VP Loop. Using pressures waveforms from various arterial sites alters VP Loops and its characteristics angles β and GALA. These differences seem small and might be clinically irrelevant along the aorta but using radial pressure waveforms greatly modify VP Loops, β and GALA angles. Using a radial artery to build VP Loops lead to underestimation of arterial stiffness and cardiac afterload parameters especially in high cardiovascular risk patients. This underestimation seems to be corrected with a transfer function estimation of aortic pressures from the radial catheter signal.

Conflict of Interest:

Fabrice Vallée, Arthur Le Gall, Etienne Gayat and Alexandre Mebazaa co-own the patent describing the PU Loop (WO 2015173785 A1 "Method for the continuous evaluation of the ventriculo-aortic coupling of at-risk patients by analysis of pressure-flow loops")

Alexandre Mebazaa has received speaker honoraria from Abbott, Novartis, Orion, Roche and Servier and fee as member of advisory board and/or steering committee from Cardiorentis, Adrenomed, MyCartis, ZS Pharma and Critical Diagnostics

Etienne Gayat has received consulting fees from Magnisense, research support from Sphingotec, Deltex Medical and Retia Medical.

Fabrice Vallée has received research support from Radiometer, Deltex Medical and Retia Medical.

Sandrine Millasseau has received consulting fees from Alam Medical, AtCor Medical, Mesi Medical and Omron.

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Table 1; Patients characteristics (median [IQR] or n(%))

	all (n=25)	LR (n=15)	HR (n=10)
Age (years)	52 [36 – 60]	43 [35 – 53]	57 [55 – 69]*
Male	13 (52%)	9 (60%)	4 (40%)*
Weight (kg)	69 [62 – 77]	70 [63 – 75]	69 [65 – 88]
Height (cm)	167 [160 – 173]	166 [160 – 175]	169 [160 – 170]
BMI (kg/m ²)	23.7 [22.8 – 28.3]	23.4 [22.9 – 25.9]	24.2 [22.7 – 29.5]
ASA score	2 [1 – 3]	2 [1 – 2]	2 [2 – 3]
MBP (mmHg)	80 [78 – 89]	83 [74 – 91]	80 [80 – 84]
HR (min-1)	66 [58 – 74]	66 [56 – 85]	65 [59 – 72]
SV (mL)	74 [62 – 88]	80 [67 – 89]	69 [60 – 83]*
CO (l/min)	4.6 [4.1 – 5.8]	4.9 [4.3 – 6.0]	4.3 [4.1 – 5.5]*
EtCO ₂ (mmHg)	33 [32 – 34]	33 [32 – 36]	33 [33 – 34]
Cardiovascular risk prevalence			
Age > 55 years	10 (40%)	3 (20%)	7 (70%)*
Hypertension	7 (28%)	3 (20%)	4 (40%)
Diabetes mellitus	2 (8%)	0 (0%)	2 (20%)*
Dyslipidemia	4 (16%)	1 (7%)	3 (30%)*
Smokers	4 (16%)	2 (13%)	2 (20%)
Ischemic heart disease	2 (8%)	1 (7%)	1 (7%)

LR: low cardiovascular risk group

HR: high cardiovascular risk group

*: p < 0.05 compared to LR groups.

Table 2: comparison of angles from VP Loop_{ref}, VP Loop_{abd} and VP Loop_{fem}, in all, low risk (LR) and high risk (HR) patients.

	GALA			β		
	VP Loop _{ref}	VP Loop _{abd}	VP Loop _{fem}	VP Loop _{ref}	VP Loop _{abd}	VP Loop _{fem}
All patients (n=25)	46° [36 - 54]	43° [34 - 49]	45° [34 - 53]	16° [4 - 27]	11° [2 - 20]*	8° [3 - 15]*
LR (n=10)	38° [23 - 45]	38° [27 - 45]	38° [28 - 46]	5° [1 - 14]	5° [2 - 10]	3° [1 - 11]*
HR (n=15)	55° [49 - 63]	52° [47 - 61]	54° [45 - 62]	27° [20 - 36]	21° [15 - 28]*	13° [9 - 16]*

*: $p < 0.05$ compared to VP Loop_{ref} using *paired Wilcoxon signed-rank test*.

Table 3: comparison of angles from VP Loop_{ref}, VP Loop_{rad} and VP Loop_{TF}, in all, low risk patients (LR) and high risk patient (HR).

	GALA			β		
	VP Loop _{ref}	VP Loop _{rad}	VP Loop _{TF}	VP Loop _{ref}	VP Loop _{rad}	VP Loop _{TF}
All (n=22)	46° [36 - 54]	39° [31 - 47]*	45° [32 - 55]	16° [4 - 27]	6° [2 - 14] *	17° [5 - 28]
LR (n=8)	38° [23 - 45]	36° [25 - 46]	36° [21 - 44]	5° [1 - 14]	3° [1 - 6] *	7° [2 - 15]
HR (n=14)	55° [49 - 63]	45° [40 - 53] *	56° [50 - 62]	27° [20 - 36]	18° [8 - 23] *	29° [23 - 38]

*: $p < 0.05$ compared to VP Loop_{ref} using *paired Wilcoxon signed-rank test*.

Figure 1:

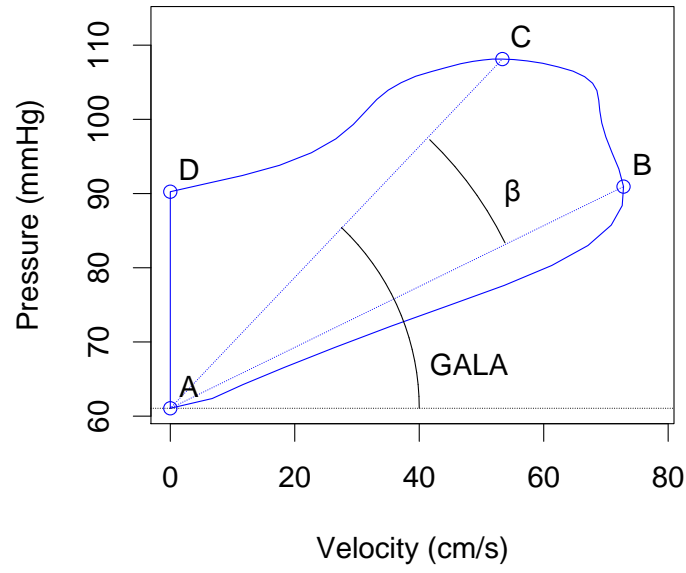


Figure 2 : Example of velocity, radial, thoracic and transformed radial waveforms in upper panel and their respective VP Loops in lower in an high risk patient

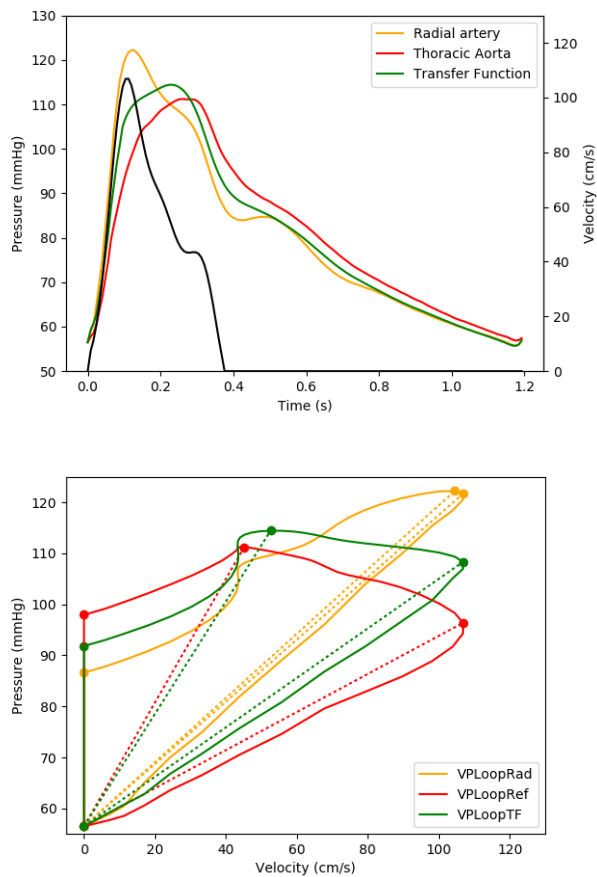


Figure 3 : Example of velocity, radial, thoracic and transformed radial waveforms in upper panel and their respective VP Loops in lower in an low risk patient

