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Theoretical and Numerical Study of Cardiac Electrophysiology

Problems at the Microscopic Scale.

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We present a microscopic scale model for the propagation of electric waves in human ventricle cells. We achieved a mathematical analysis of this model and show the existence of a weak solution.

Summary

Context

- Modeling studies of cardiac electrophysiology essentially rely on homogenized models like monodomain and bidomain models [**?**];
- Homogenized models cannot take microscopic alterations into account, and cannot represent the nonlinear behaviour of gap junctions between the cells;
- Heart tissue cells constitute a network of cells connected via these gap junctions (see figure), which behave as ionic channels, but between two cells instead of one cell and the extracellular medium.

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- Dimensions for one cell: length: 175 μm , width: 20 μm , membrane thickness: 10 nm , spacing between neighbours: 1 nm . This leads to experimental and computational challenges;
- Malfunctions and inhomogeneities in heart tissue may lead to alterations in the wave propagation [**?**];
- Microscopic cardiac conduction has been studied experimentally [**?**] and numerically [**?**, **?**], but numerical studies have been limited to simplified 2-dimensional monodomain models.

We study the problem on a finite time interval $[0; T]$ at the cellular scale using the following sketch

- The ionic term I_{ion} is nonlinear, and also depends on gating variables;
- The boundary coupling conditions on the membrane include a time derivative, which is not proven to be defined.

Mathématiques de

B o r d e a u x

Purpose

- Develop a new 3-dimensional, structurally realistic model formulation with separate intracellular and extracellular domains.
- Get a better understanding of the consequences of microscopic alterations in the heart;

• I_{ion} is Lipschitz-continuous with coefficient λ and $I_{\text{ion}}(0) = 0$.

• Simulate the model efficiently, via domain decomposition methods.

for all $\varphi_j\,\in\, L^2(0,T;H^1(\Omega_j)),\ j\,=\,i,e$ and $\tilde\varphi\,:=\,(\varphi_i-\varphi_e)\,\mid_\Gamma\in\, L^2(0,T;H^{1/2}(\Gamma)),$ that is also solution of (1).

A first microscopic mathematical model

Model

- Use a time discretisation for the temporal term $\partial_t v$ on the interface in order to obtain an elliptic problem;
- Use the Lax Milgram theorem in order to obtain a unique solution;
- Calculate energy estimates especially on time increments of v ;
- Via a compacity argument, prove the weak convergence of a time-rebuilt solution;
- Pass to the limit in the rebuilt problem.

 σ_g being the conductivity of the gap junction, $v_g=u_{i1}-u_{i2}$ the voltage between the two cells at the gap junction, I_q a one or zero operator modelling the open/closed state of the gap junction.

$$
\begin{cases}\n-\nabla \cdot (\sigma_j \nabla u_j) = 0 \text{ in } [0; T] \times \Omega_j, \text{ with } j = i, e \\
\sigma_e \nabla u_e \cdot n_e = 0 \text{ on } [0; T] \times \Gamma_e, \\
-\sigma_i \nabla u_i \cdot n_i = \sigma_e \nabla u_e \cdot n_e \text{ on } [0; T] \times \Gamma, \\
= c_m \partial_t v + I_{\text{ion}}(v, w) \text{ on } [0; T] \times \Gamma.\n\end{cases}
$$
\n(1)
\n
$$
v(0, x) = v_0(x) \text{ on } \Gamma
$$

This model presents specific issues

Analysis of the microscopic model

Hypotheses

• Conductivity tensors σ_i and σ_e are uniformly continuous and coercive

 $\exists m_j,M_j>0,\ \forall (x,y)\in\mathbb{R}^3,\ m_j\|y\|^2<(\sigma_j(x)y,y)< M_j\|y\|^2$ for $j=i,e;$

Weak problem and main result

There exists a solution $(u_{\rm i},u_{\rm e})\in{\rm L}^2([0;T];{\rm H}^1(\Omega_{\rm i}))\times{\rm L}^2([0;T];{\rm H}^1(\Omega_{\rm e}))$ of

$$
\int_0^T \int_{\Omega_i} \sigma_i \nabla u_i \cdot \nabla \varphi_i dx dt + \int_0^T \int_{\Omega_e} \sigma_e \nabla u_e \cdot \nabla \varphi_e dx dt + \int_{\Gamma} c_m v_0 \tilde{\varphi}(t=0) dx - \int_0^T \int_{\Gamma} c_m v \partial_t \tilde{\varphi} dx dt + \int_0^T \int_{\Gamma} I_{\text{ion}}(v) \tilde{\varphi} dx dt = 0.
$$
 (2)

Sketch of a proof

Possible model enhancement

A representation of gap junctions (Credit: Mariana Ruiz, 2006) is given in the following figure

Gap junctions have a different conductivity. The penultimate line of equation (1) can be slightly modified on a Gap Junction to take this into account. If we denote Γ_q the set of all gap junctions, it would become

$$
-\sigma_{i1}\nabla u_{i1}\cdot n_{i1} = \sigma_g I_g \partial_t v_g + I_g I_{ion}(v) \quad \text{on } \Gamma_g,
$$

Conclusion and perspectives

Conclusion

 $\sigma_{\rm i}$ and $\sigma_{\rm e}$ are respectively intracellular and extracellular conductivity. $u_{\rm i}, u_{\rm e}$ intracellular/extracellular potential. I_{ion} is the ionic current per unit of membrane area. c_m is the electrical capacitance of the membrane per unit of area. With $v := u_i - u_e$, the model reads

• We have designed a basic model and proved existence of a unique solution;

• The hypotheses we made in this regard are consistent with the physics of the problem.

Perspectives

• Model enhancement with gap junctions and specificities of ionic channel (gating variables);

- Ongoing work on simulation, using a homemade framework;
- Enhance the model regarding what happens inside the cells;
- Discuss on the dimensions, especially the thickness of the membrane vs. the spacing between cells.

