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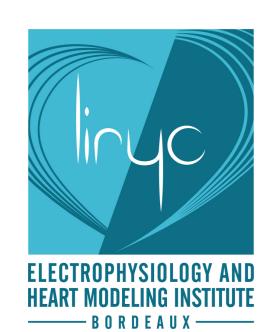
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Theoretical and Numerical Study of Cardiac Electrophysiology



Problems at the Microscopic Scale.



Pierre-Elliott Bécue

Florian Caro, Mark Potse, Yves Coudière

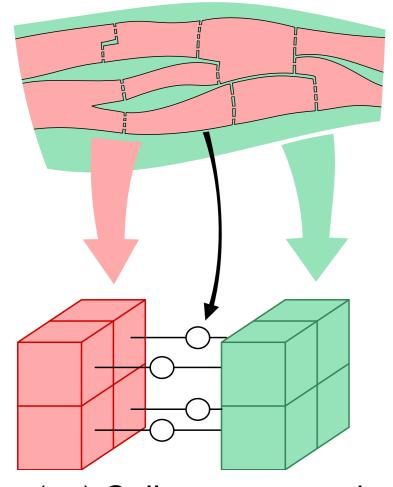
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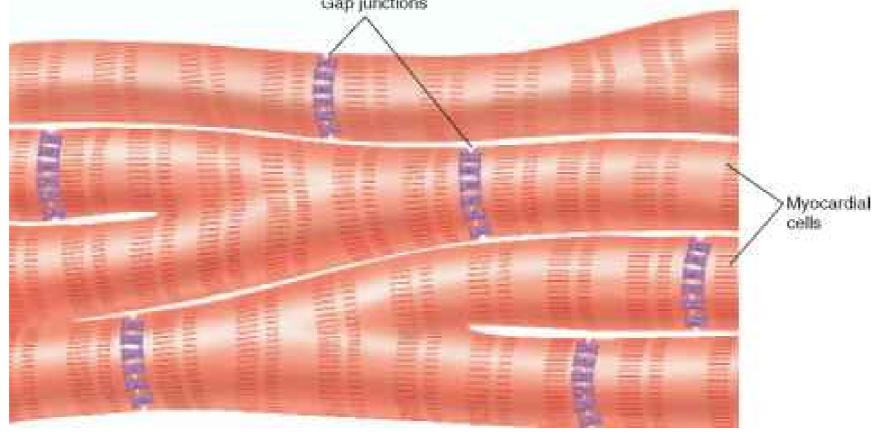
Summary

We present a microscopic scale model for the propagation of electric waves in human ventricle cells. We achieved a mathematical analysis of this model and show the existence of a weak solution.

Context

- Modeling studies of cardiac electrophysiology essentially rely on homogenized models like monodomain and bidomain models [?];
- Homogenized models cannot take microscopic alterations into account, and cannot represent the nonlinear behaviour of gap junctions between the cells;
- Heart tissue cells constitute a network of cells connected via these gap junctions (see figure), which behave as ionic channels, but between two cells instead of one cell and the extracellular medium.





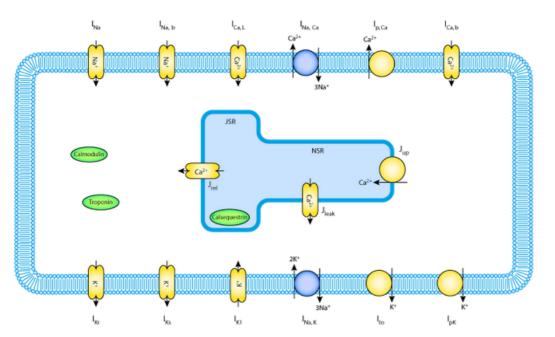
(a) Cells as a network

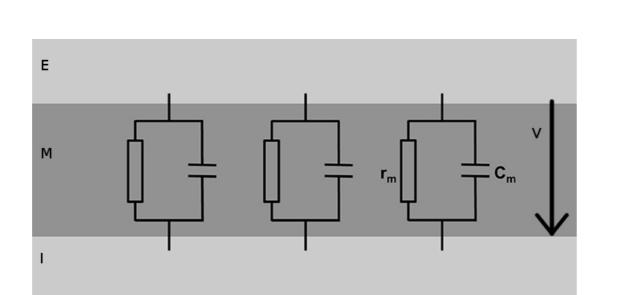
(b) Gap junctions highlight

- \bullet Dimensions for one cell: length: 175 μm , width: 20 μm , membrane thickness: 10 nm, spacing between neighbours: 1 nm. This leads to experimental and computational challenges;
- Malfunctions and inhomogeneities in heart tissue may lead to alterations in the wave propagation [?];
- Microscopic cardiac conduction has been studied experimentally [?] and numerically [?, ?], but numerical studies have been limited to simplified 2-dimensional monodomain models.

Purpose

- Develop a new 3-dimensional, structurally realistic model formulation with separate intracellular and extracellular domains.
- Get a better understanding of the consequences of microscopic alterations in the heart;
- Simulate the model efficiently, via domain decomposition methods.





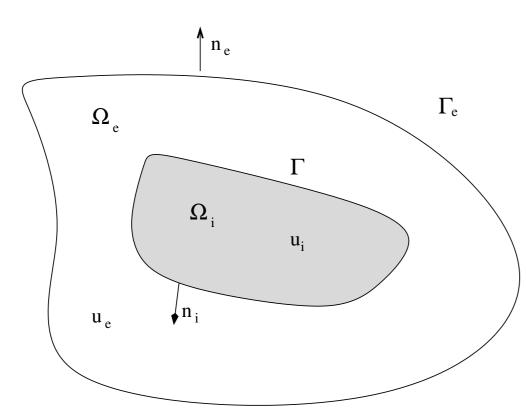
(a) Cell model (Ten Tusscher, Noble, Noble, Panfilov – 2004)

(b) Ionic channels as circuits

A first microscopic mathematical model

Model

We study the problem on a finite time interval [0;T] at the cellular scale using the following sketch



 $\sigma_{\rm i}$ and $\sigma_{\rm e}$ are respectively intracellular and extracellular conductivity. $u_{\rm i}, u_{\rm e}$ intracellular/extracellular potential. I_{ion} is the ionic current per unit of membrane area. c_m is the electrical capacitance of the membrane per unit of area. With $v:=u_i-u_e$, the model reads

$$\begin{cases} -\nabla \cdot (\sigma_{j} \nabla u_{j}) = 0 \text{ in } [0;T] \times \Omega_{j}, \text{ with } j = i, e \\ \sigma_{e} \nabla u_{e} \cdot n_{e} = 0 \text{ on } [0;T] \times \Gamma_{e}, \\ -\sigma_{i} \nabla u_{i} \cdot n_{i} = \sigma_{e} \nabla u_{e} \cdot n_{e} \text{ on } [0;T] \times \Gamma, \\ = c_{m} \partial_{t} v + I_{ion}(v,w) \text{ on } [0;T] \times \Gamma. \end{cases}$$

$$v(0,x) = v_{0}(x) \text{ on } \Gamma$$
 (1)

This model presents specific issues

• The ionic term I_{ion} is nonlinear, and also depends on gating variables;

• The boundary coupling conditions on the membrane include a time derivative, which is not proven to be defined.

Analysis of the microscopic model

Hypotheses

 \bullet Conductivity tensors σ_i and σ_e are uniformly continuous and coercive

$$\exists m_j, M_j > 0, \ \forall (x, y) \in \mathbb{R}^3, \ m_j ||y||^2 < (\sigma_j(x)y, y) < M_j ||y||^2 \text{ for } j = i, e;$$

• I_{ion} is Lipschitz-continuous with coefficient λ and $I_{\text{ion}}(0) = 0$.

Weak problem and main result

There exists a solution $(u_i, u_e) \in L^2([0; T]; H^1(\Omega_i)) \times L^2([0; T]; H^1(\Omega_e))$ of

$$\int_{0}^{T} \int_{\Omega_{i}} \sigma_{i} \nabla u_{i} \cdot \nabla \varphi_{i} dx dt + \int_{0}^{T} \int_{\Omega_{e}} \sigma_{e} \nabla u_{e} \cdot \nabla \varphi_{e} dx dt + \int_{\Gamma} c_{m} v_{0} \tilde{\varphi}(t=0) dx \\
- \int_{0}^{T} \int_{\Gamma} c_{m} v \partial_{t} \tilde{\varphi} dx dt + \int_{0}^{T} \int_{\Gamma} I_{ion}(v) \tilde{\varphi} dx dt = 0.$$
(2)

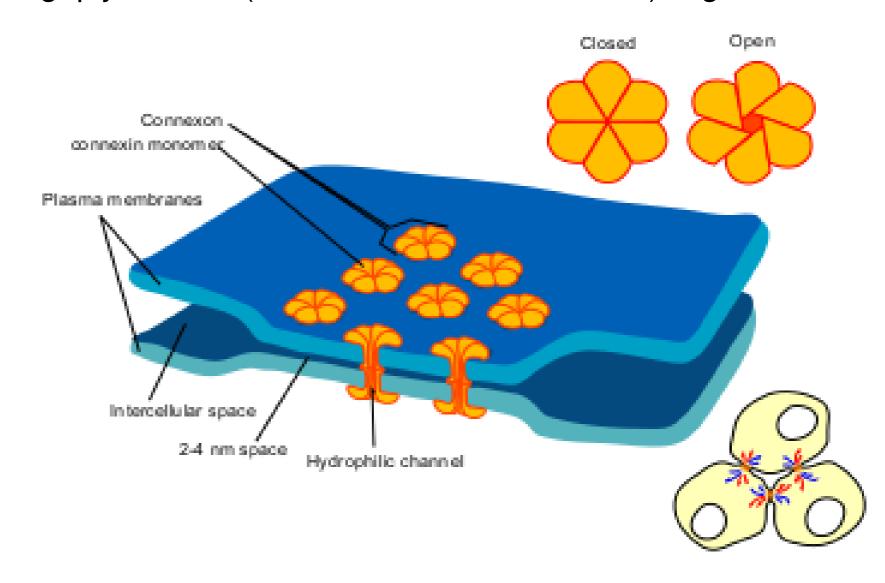
 $\text{for all } \varphi_j \in L^2(0,T;H^1(\Omega_j))\text{, } j=i,e \text{ and } \tilde{\varphi}:=(\varphi_i-\varphi_e) \mid_{\Gamma} \in L^2(0,T;H^{1/2}(\Gamma))\text{, that is also } 1\leq i\leq n$ solution of (1).

Sketch of a proof

- Use a time discretisation for the temporal term $\partial_t v$ on the interface in order to obtain an elliptic problem;
- Use the Lax Milgram theorem in order to obtain a unique solution;
- ullet Calculate energy estimates especially on time increments of v;
- Via a compacity argument, prove the weak convergence of a time-rebuilt solution;
- Pass to the limit in the rebuilt problem.

Possible model enhancement

A representation of gap junctions (Credit: Mariana Ruiz, 2006) is given in the following figure



Gap junctions have a different conductivity. The penultimate line of equation (1) can be slightly modified on a Gap Junction to take this into account. If we denote Γ_q the set of all gap junctions, it would become

$$-\sigma_{i1} \nabla u_{i1} \cdot n_{i1} = \sigma_q I_q \partial_t v_q + I_q I_{ion}(v)$$
 on Γ_q ,

 σ_g being the conductivity of the gap junction, $v_g = u_{i1} - u_{i2}$ the voltage between the two cells at the gap junction, I_q a one or zero operator modelling the open/closed state of the gap junction.

Conclusion and perspectives

Conclusion

- We have designed a basic model and proved existence of a unique solution;
- The hypotheses we made in this regard are consistent with the physics of the problem.

Perspectives

- Model enhancement with gap junctions and specificities of ionic channel (gating variables);
- Ongoing work on simulation, using a homemade framework;
- Enhance the model regarding what happens inside the cells;
- Discuss on the dimensions, especially the thickness of the membrane vs. the spacing between cells.











