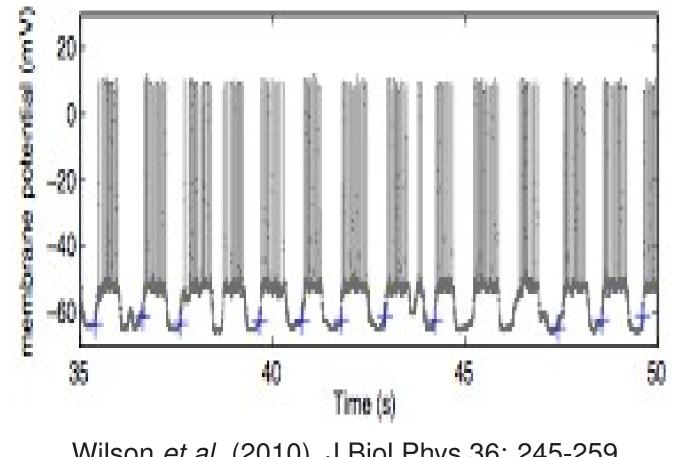
Slow oscillations of 'up' and 'down' states during general anesthesia: bi-stability in a non-linear model Pedro García-Rodríguez and Axel Hutt



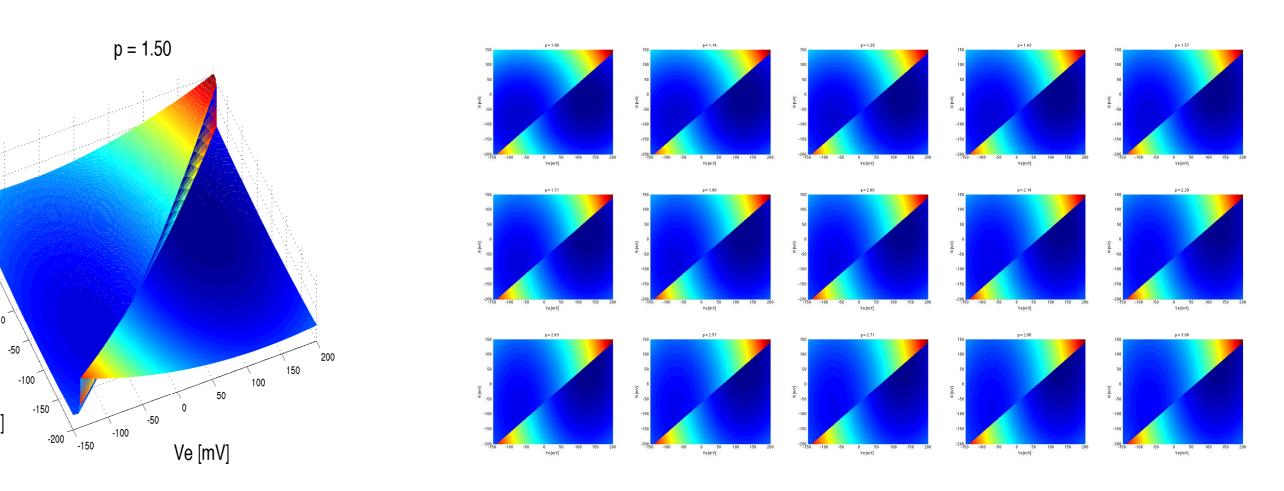
Summary

- > Sequences of alternating quiescent ('down') and bursting ('up') states in NREM sleep are found across mammalian species (Destexhe A. et al, Trends in Neurosciences 30: 334-342, 2007) and in neuronal recordings (LFP and EEG) of anesthetized animals (Hutt A. (ed.), Springer-Verlag, 2011).
- The dynamical principles underlying such phenomenon are unclear.
- > Previous theoretical attempts to understand the neural basis of anesthesia effects suggest the existence of notable non-linearities in the behavior of the neuronal membrane potential (Steyn-Ross M. et al., Physical Review E 60(6): 7299-7311, 1999; Hutt A. and Longtin A., Cognitive Neurodynamics 4(1): 37-59, 2009).
- ► Noise-induced transitions between two stable branches through which the dynamics may evolve as the concentration of the anesthetic agent (AA) increases, could explain the observed alternating sequences of 'up' and 'down' states.
- ► Nevertheless, the mathematical tractability of these non-linear scenarios is difficult due to the 2D phase space defined by the describing variables: the excitatory and the inhibitory PSPs at excitatory cells.
- Exact solutions to these problems are only known for 1D systems and, consequently, the analysis of the existing non-linear models is typically avoided.
- ▶ In this work we undertake a first attempt to solve this task, by applying known techniques on stochastic phenomena theory (Gardiner C.W., Springer-Verlag, 2004) to the Hutt & Longtin (2009) model. We consider the time the system spends in the 'up' or 'down' states as being similar to the mean exit-time needed to escape from the corresponding attractor.

Bistability in anesthesia



Simplifications (I)...



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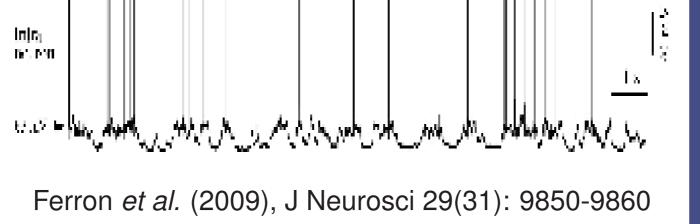
Simplifications (II)

* A 45°-rotation of the (V_i, V_e) coordinate system about the origin:

 $\begin{bmatrix} \hat{V}_{+} \\ \hat{V}_{-} \end{bmatrix} = \frac{1}{\sqrt{2}} \begin{bmatrix} 1 & 1 \\ -1 & 1 \end{bmatrix} \begin{bmatrix} V_{i} \\ V_{e} \end{bmatrix} = \frac{1}{\sqrt{2}} \begin{bmatrix} V_{+} \\ V_{-} \end{bmatrix}$

- Domain I: $\hat{V}_{-} < \theta_i / \sqrt{2}$

$\frac{d}{dt} \begin{bmatrix} \hat{V}_{+} \\ \hat{V}_{-} \end{bmatrix} = \frac{1}{2} \begin{bmatrix} -(\beta + \alpha) & \beta - \alpha \\ \beta - \alpha & -(\beta + \alpha) \end{bmatrix} \begin{bmatrix} \hat{V}_{+} \\ \hat{V}_{-} \end{bmatrix} + \frac{V_{e}^{r}}{\sqrt{2}} \begin{bmatrix} (\beta + \alpha) \\ -(\beta - \alpha) \end{bmatrix} + 2\sigma \begin{bmatrix} \dot{\eta}_{+} \\ \dot{\eta}_{-} \end{bmatrix}$



Wilson et al. (2010), J Biol Phys 36: 245-259

Hutt & Longtin (2009) model with no delay nor spatial dimension: a neural population model

1. Integral form:

$$V_{i}(t) - V_{e}^{r} = \int_{-\infty}^{t} h_{i}(t - t')S_{i}(V_{e} - V_{i} - \theta_{i})dt' + \sqrt{2}\sigma \int_{-\infty}^{t} h_{i}(t - t')dW_{i}(t')$$

$$V_{e}(t) - V_{e}^{r} = \int_{-\infty}^{t} h_{e}(t - t')S_{e}(V_{e} - V_{i} - \theta_{e})dt' + \sqrt{2}\sigma \int_{-\infty}^{t} h_{e}(t - t')dW_{e}(t')$$

where V_i , V_e are the PSPs at excitatory neurons, V_e^r the resting membrane potential, $\theta_i < \theta_e$ the threshold potentials of the pre-synaptic cells, S_e and S_i are sigmoids functions $S_k(x) = \frac{S_{max}}{1+e^{-c_k(x-\theta_k)}}$, $k \in \{i, e\}$. W_k represent Wiener processes and h_k the mean synaptic response functions:

$$h_i(t) = a_i f(p) \frac{\beta_1 \beta_2}{\beta_2 - \beta_1} (e^{-\beta_1 t} - e^{-\beta_2 t})$$

$$h_e(t) = a_e \frac{\alpha_1 \alpha_2}{\alpha_2 - \alpha_1} (e^{-\alpha_1 t} - e^{-\alpha_2 t})$$

where a_k stand for the synaptic efficacies and $f(p) = r^{-r/(r-1)}(rp)^{rp/(rp-1)}$ mimics the inhibitory action of the propofol p level, with $r = \beta_2/\beta_1$, $\beta_1 = \beta_0/p$.

2. Differential form, using the scaled (dimensionless) time $\tau = \sqrt{\alpha_1 \alpha_2} t$:

$$(\partial^2/\partial\tau^2 + \gamma_i\partial/\partial\tau + \omega_i^2)(V_i - V_e^r) = a_i f(p)\omega_i^2 S_i(V_e - V_i - \theta_i) + \sqrt{2}\sigma \dot{W}_i (\partial^2/\partial\tau^2 + \gamma_e\partial/\partial\tau + 1)(V_e - V_e^r) = a_e S_e(V_e - V_i - \theta_e) + \sqrt{2}\sigma \dot{W}_e$$

with $\gamma_i = (\beta_1 + \beta_2)/\sqrt{\alpha_1 \alpha_2}$, $\gamma_e = \sqrt{\alpha_1/\alpha_2} + \sqrt{\alpha_2/\alpha_1}$, $\omega_i = \sqrt{\beta_1 \beta_2/(\alpha_1 \alpha_2)}$.

Bifurcation diagrams of Hutt & Longtin (2009) model

where $\eta_{\{+,-\}}$ are Wiener processes. - Domain II: $\hat{V}_{-} > \theta_{e}/\sqrt{2}$

$$\frac{d}{dt} \begin{bmatrix} \hat{V}_{+} \\ \hat{V}_{-} \end{bmatrix} = \frac{1}{2} \begin{bmatrix} -(\beta + \alpha) & \beta - \alpha \\ \beta - \alpha & -(\beta + \alpha) \end{bmatrix} \begin{bmatrix} \hat{V}_{+} \\ \hat{V}_{-} \end{bmatrix} + \frac{1}{\sqrt{2}} \begin{bmatrix} (\beta + \alpha) V_{e}^{r} + (\beta_{0}a_{i} + \alpha a_{e})S_{max} \\ -(\beta - \alpha) V_{e}^{r} + (-\beta_{0}a_{i} + \alpha a_{e})S_{max} \end{bmatrix} + 2\sigma \begin{bmatrix} \dot{\eta}_{+} \\ \dot{\eta}_{-} \end{bmatrix}$$

* A non-linear transformation: X_+ = tanh \hat{V}_+ , X_- = tanh \hat{V}_- . New Langevin equations are obtained with Ito's calculus :

$$\frac{dX_{+}}{dt} = (1 - X_{+}^{2})[C_{+} - (2\sigma)^{2}X_{+}] + 2\sigma(1 - X_{+}^{2})\dot{\eta}_{+}$$

$$\frac{dX_{-}}{dt} = (1 - X_{-}^{2})[C_{-} - (2\sigma)^{2}X_{-}] + 2\sigma(1 - X_{-}^{2})\dot{\eta}_{-}$$

where

$$C_{+} = -\frac{\beta + \alpha}{4} \ln(\frac{1 + X_{+}}{1 - X_{+}}) + \frac{\beta - \alpha}{4} \ln(\frac{1 + X_{-}}{1 - X_{-}}) + \frac{\beta + \alpha}{\sqrt{2}} V_{e}^{r} + \frac{\beta_{0} a_{i} + \alpha a_{e}}{\sqrt{2}} S_{max}$$

$$C_{-} = \frac{\beta - \alpha}{4} \ln(\frac{1 + X_{+}}{1 - X_{+}}) - \frac{\beta + \alpha}{4} \ln(\frac{1 + X_{-}}{1 - X_{-}}) + \frac{-\beta + \alpha}{\sqrt{2}} V_{e}^{r} + \frac{-\beta_{0} a_{i} + \alpha a_{e}}{\sqrt{2}} S_{max}$$

Fokker-Planck equation and FPT theory

Fokker-Planck equation:

$$\frac{\partial P}{\partial t} = -\frac{\partial}{\partial X_{+}}[A_{+}P] - \frac{\partial}{\partial X_{-}}[A_{-}P] + \frac{B_{++}}{2}\frac{\partial^{2}P}{\partial X_{+}^{2}} + \frac{B_{--}}{2}\frac{\partial^{2}P}{\partial X_{-}^{2}}$$

where $P = P(X_+, X_-, t | X_+(0), X_-(0), 0)$ is the conditional probability, and

$$A_s = (1 - X_s^2)[C_s - (2\sigma)^2 X_s]$$

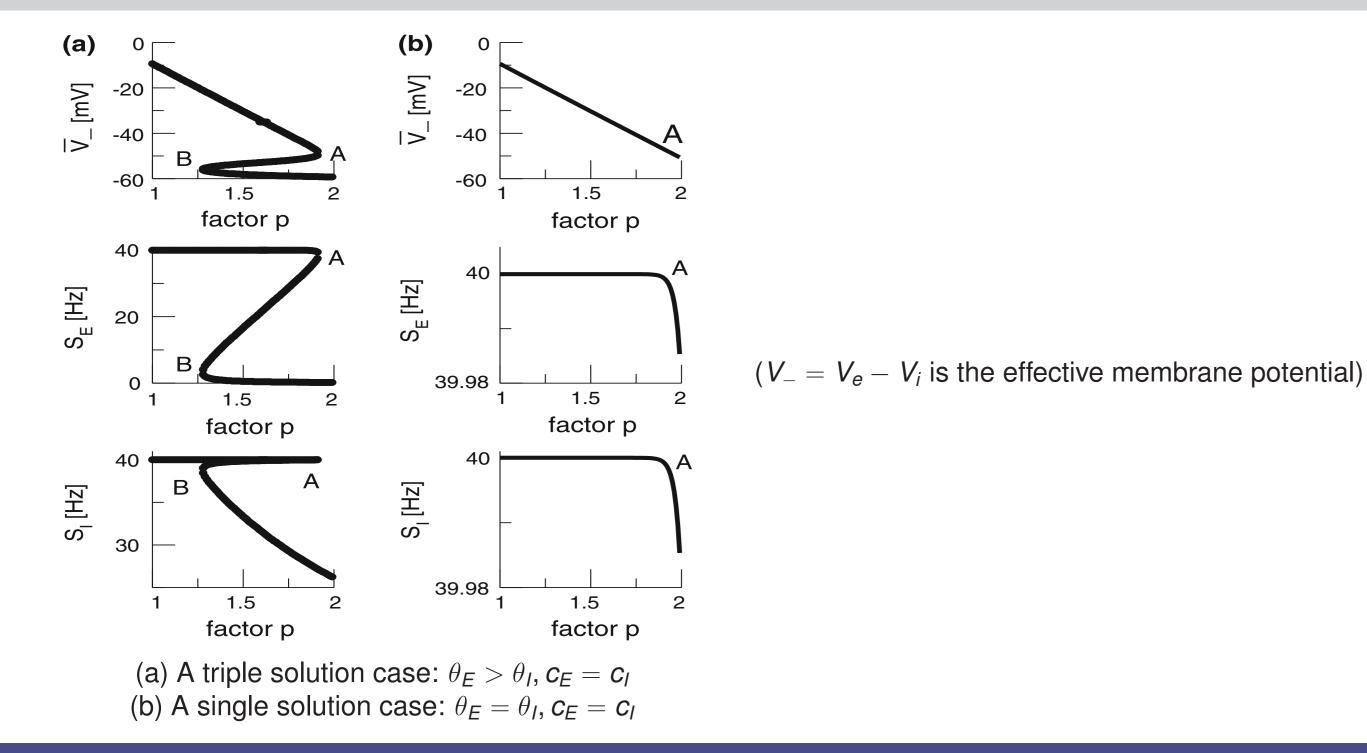
$$B_{ss} = [2\sigma(1 - X_s^2)]^2$$

are the drift and diffusion coefficients, respectively, with $s \in \{+, -\}$. Partial differential equations of FPT theory:

$$\begin{bmatrix} A_{+}\frac{\partial}{\partial X_{+}} + A_{-}\frac{\partial}{\partial X_{-}} + \frac{1}{2}B_{++}\frac{\partial^{2}}{\partial X_{+}^{2}} + \frac{1}{2}B_{--}\frac{\partial^{2}}{\partial X_{-}^{2}} \end{bmatrix} T(X_{+}, X_{-}) = -1$$

$$\begin{bmatrix} A_{+}\frac{\partial}{\partial X_{+}} + A_{-}\frac{\partial}{\partial X_{-}} + \frac{1}{2}B_{++}\frac{\partial^{2}}{\partial X_{+}^{2}} + \frac{1}{2}B_{--}\frac{\partial^{2}}{\partial X_{-}^{2}} \end{bmatrix} \left[\pi(X_{+}, X_{-}, a_{+}, a_{-})T(X_{+}, X_{-}, a_{+}, a_{-}) \right] = -\pi(a_{+}, a_{-})$$

$$\begin{bmatrix} A_{+}\frac{\partial}{\partial X_{+}} + A_{-}\frac{\partial}{\partial X_{-}} + \frac{1}{2}B_{++}\frac{\partial^{2}}{\partial X_{+}^{2}} + \frac{1}{2}B_{--}\frac{\partial^{2}}{\partial X_{-}^{2}} \end{bmatrix} \pi(X_{+}, X_{-}, a_{+}, a_{-}) = 0$$



First-passage time (FPT) theory: obstacles to formulate the PDEs problem

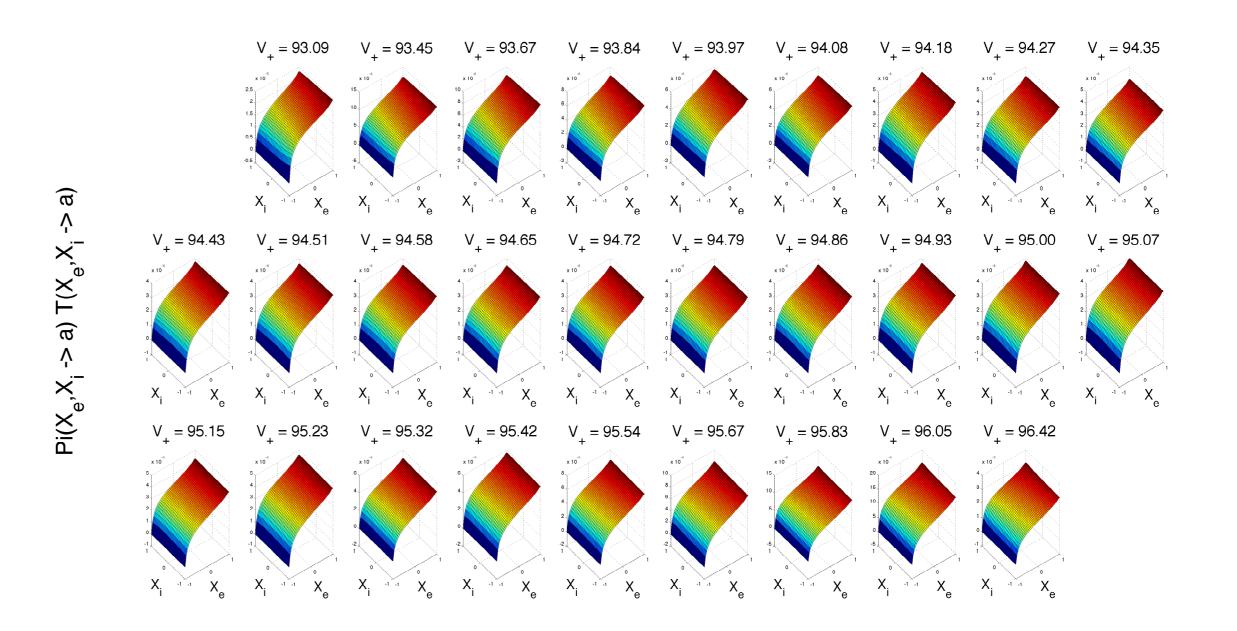
- High dimensionality, e.g., 2nd-order partial differential equations.
- ▶ No potentials to describe the vector field, due to the presence of the response functions S_k .
- Infinite regions given by the attraction basins.
- Oblique boundaries

Simplifications (I)

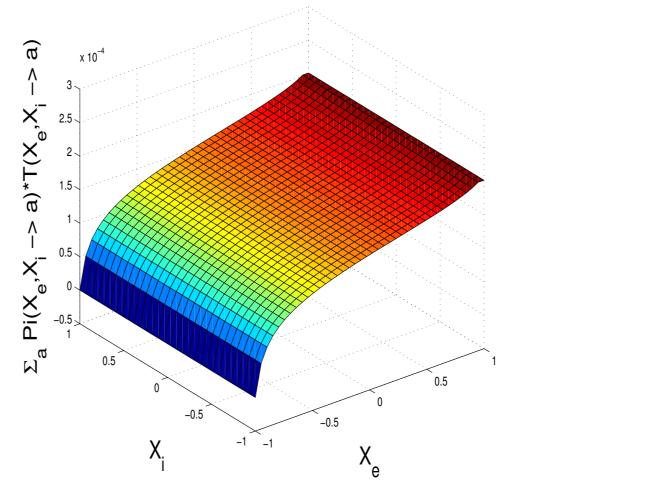
* $\beta_1 \ll \beta_2 \rightarrow r \gg 1 \rightarrow f(p) \approx p$ leads to 1st-order Langevin (SDE) equations:

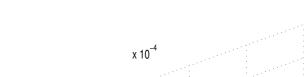
where $T(X_+, X_-)$ stands for the mean FPT when the escape occurs through any point in the saddles line $V_e - V_i - \theta_k = 0$, while $T(X_+, X_-, a_+, a_-)$ is the exit time when it happens through a specific point (a_+, a_-) . $\pi(a_+, a_-)$ is the corresponding exit probability. The formulation of the problem is completed with the following boundary conditions (BCs): Dirichlet BCs at the saddles line: $T(X_+, X_-) = 0$, $T(X_+, X_-, a_+, a_-) = 0$ and $\pi(X_+, X_-, a_+, a_-) = 0$ (absorbing boundary) Neumann BCs at the remainder boundaries: $\frac{\partial}{\partial X_s}T(X_+, X_-) = 0$, $\frac{\partial}{\partial X_s}T(X_+, X_-, a_+, a_-) = 0$ and $\frac{\partial}{\partial X_s}\pi(X_+, X_-, a_+, a_-) = 0$ (reflecting barriers).

Modelling results(I): exit through a specific point $a = X_i$ (or V_+ [mV]) at the boundary $X_e = -1$



Modelling results (II): the mean exit time from the attraction basin



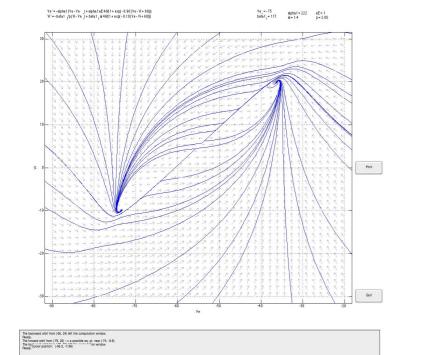


$\dot{V}_i = -\beta(V_i - V_e^r) + \beta_i a_i S_i (V_e - V_i - \theta_i) + \sqrt{2}\sigma \dot{W}_i$ $\dot{V}_{e} = -\alpha (V_{e} - V_{e}') + \alpha a_{e} S_{e} (V_{e} - V_{i} - \theta_{e}) + \sqrt{2} \sigma \dot{W}_{e},$

 $\dot{V}_i = -\beta (V_i - V_e^r) + \beta_0 a_i S_{max} + \sqrt{2}\sigma \dot{W}_i$

 $\dot{V}_{e} = -\alpha (V_{e} - V_{e}') + \alpha a_{e} S_{max} + \sqrt{2}\sigma \dot{W}_{e}$

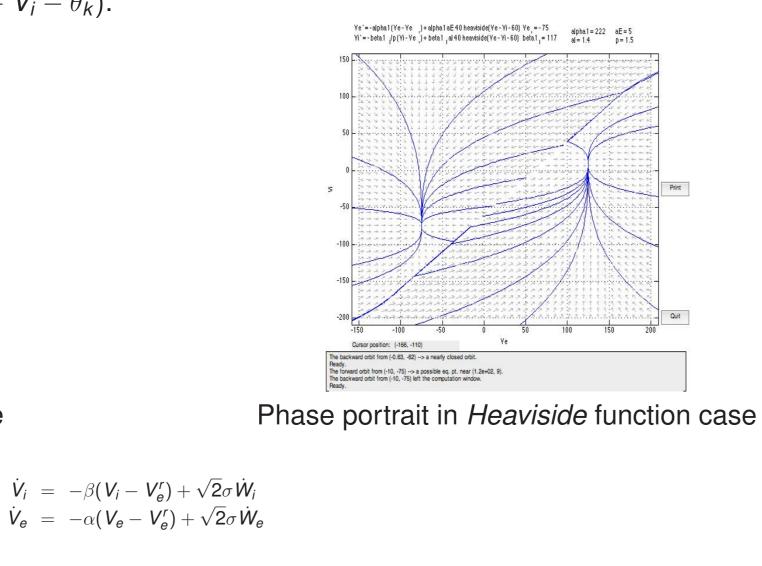
where $\beta = \beta_1$ and $\alpha = \alpha_1$. ^{*} Replacing S_k by a Heaviside function $S_k = \Theta(V_e - V_i - \theta_k)$:

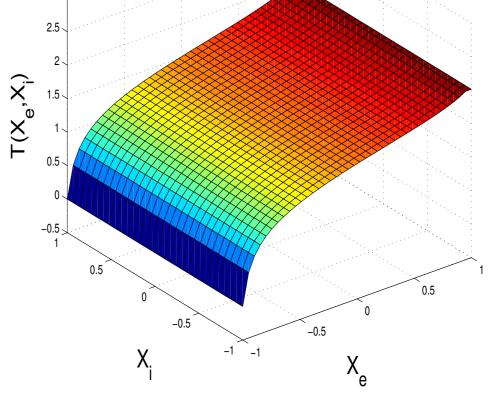


Phase portrait in *Sigmoid* function case

- Domain I: $V_e < V_i + \theta_i$

- Domain II: $V_e > V_i + \theta_e$





Exit point-averaged exit time

Mean time for exit through the boundary

Conclusions

- FPT theory is applicable to the Hutt & Longtin (2009) model for anesthesia, where a bistable (noise-driven) regime is considered to underlie the observed sequences of 'up' and 'down' states.
- ▶ The dimensionality of the system can be reduced to a pair of 1st-order differential equations.
- Neuronal response functions can be described with a Heaviside function instead of a Sigmoid, with no essential modifications of the phase-portraits.
- Infinite basins of attractions and oblique boundaries can be avoided by appropriate coordinates changes.

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