

Oblique Random Forests for 3-D Vessel Detection Using Steerable Filters and Orthogonal Subspace Filtering

– Supplementary Material –

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A Appendix

A.1 Steerability of Gaussian Derivatives

The steerability of Gaussian derivatives has been derived for the 2-D case in [3] and can readily be extended to 3-D [2]. Steerability refers to the property that the convolution of an image with a rotated version of the steerable filter template (SFT) can be expressed by a linear combination of the filter response of the image with the SFT without rotation:

$$I * G_{m,a,b}^\sigma(R\mathbf{x}) = \sum_{i=0}^m \sum_{j=0}^i \omega_{m,a,b}^{i,j} \underbrace{(I * G_{m,i,j}^\sigma)(\mathbf{x})}_{f_{m,i,j}^\sigma(I,\mathbf{x})}, \quad (1)$$

where $R \in SO(3)$ denotes a 3-D rotation matrix:

$$R_{\theta,\phi} = \begin{pmatrix} \cos \theta \cos \phi & \cos \theta \sin \phi & \sin \theta \\ -\sin \phi & \cos \phi & 0 \\ -\sin \theta \cos \phi & -\sin \theta \sin \phi & \cos \theta \end{pmatrix}. \quad (2)$$

The uniquely defined coefficients $\omega_{m,a,b}^{i,j}$ can be computed in closed form as:

$$w_{m,a,b}^{i,j} = \sum_{\mathbf{s} \in \mathcal{S}_{m,a,b}^{i,j}} (-1)^{a-v_1-w_2} \binom{m-a}{u_1} \binom{a-b}{v_1} \binom{b}{w_1} \binom{u_1}{u_2} \binom{w_1}{w_2} (\cos \theta)^{m-a-u_2+w_2} (\cos \phi)^{m-a+b-u_1+v_1-w_1} (\sin \theta)^{b+u_2-w_2} (\sin \phi)^{a-b+u_1-v_1+w_1-u_2-w_2}, \quad (3)$$

where

$$\mathcal{S}_{m,a,b}^{i,j} = \{(u_1, v_1, w_1, u_2, w_2)^T \in \mathbb{N}_0^5 \mid u_1 \leq m-a, v_1 \leq a-b, w \leq b, u_2 \leq u_1, w_2 \leq w_1, u_1 + v_1 + w_1 = i, u_2 + w_2 = j\}. \quad (4)$$

Proof. Following [3], the Fourier transformation (FT) of the rotated filter templates as defined in Equations (1) and (2) can be computed by a rotation in the Fourier domain:

$$\begin{aligned} \mathcal{F}(G_{m,a,b}^\sigma(R_{\theta,\phi}\mathbf{x})) &= (i\omega_x \cos \theta \cos \phi + i\omega_y \cos \theta \sin \phi + i\omega_z \sin \theta)^{m-a} \\ &\quad (-i\omega_x \sin \phi + i\omega_y \cos \phi + 0)^{a-b} \\ &\quad (-i\omega_x \sin \theta \cos \phi + i\omega_y \sin \theta \sin \phi + i\omega_z \cos \theta)^b \cdot \hat{G}^\sigma(\boldsymbol{\omega}) \quad , \end{aligned} \quad (5)$$

where $\hat{G}^\sigma(\mathbf{x}) = \mathcal{F}(G^\sigma(\mathbf{x}))$ denotes the transfer function of the Gaussian kernel. Repeatedly applying the binomial equation, this can be rewritten as:

$$\begin{aligned} \mathcal{F}(G_{m,a,b}^\sigma(R_{\theta,\phi}\mathbf{x})) &= \sum_{u_1=0}^{m-a} \sum_{v_1=0}^{a-b} \sum_{w_1=0}^b \sum_{u_2=0}^{u_1} \sum_{w_2=0}^{w_1} \psi_{m,a,b}^{(u_1,v_1,w_1,u_2,w_2)\text{T}} \cdot \hat{G}^\sigma(\boldsymbol{\omega}) \\ &\quad (i\omega_x)^{m-(u_1+v_1+w_1)} (i\omega_y)^{(u_1+v_1+w_1)-(u_2+w_2)} (i\omega_z)^{u_2+w_2} \quad , \end{aligned} \quad (6)$$

where

$$\begin{aligned} \psi_{m,a,b}^{(u_1,v_1,w_1,u_2,w_2)\text{T}} &= (-1)^{a-v_1-w_2} \binom{m-a}{u_1} \binom{a-b}{v_1} \binom{b}{w_1} \binom{u_1}{u_2} \binom{w_1}{w_2} \\ &\quad (\cos \theta)^{m-a-u_2+w_2} (\cos \phi)^{m-a+b-u_1+v_1-w_1} \\ &\quad (\sin \theta)^{b+u_2-w_2} (\sin \phi)^{a-b+u_1-v_1+w_1-u_2-w_2} \quad . \end{aligned} \quad (7)$$

Applying the inverse FT to Equation (6) and convolving with image I finally yields:

$$\begin{aligned} I * G_{m,a,b}^\sigma(R_{\theta,\phi}\mathbf{x}) &= \sum_{u_1,v_1,w_1,u_2,w_2} \psi_{m,a,b}^{(u_1,v_1,w_1,u_2,w_2)\text{T}} (I * G_{m,u_1+v_1+w_1,u_2+w_2}^\sigma)(\mathbf{x}) \\ &= \sum_{i=0}^m \sum_{j=0}^i \underbrace{\sum_{\mathbf{s} \in \mathcal{S}_{m,a,b}^{i,j}} \psi_{m,a,b}^{\mathbf{s}}}_{w_{m,a,b}^{i,j}} \underbrace{(I * G_{m,i,j}^\sigma)(\mathbf{x})}_{\mathbf{f}_{m,i,j}(I,\mathbf{x})} \quad , \end{aligned} \quad (8)$$

where

$$\begin{aligned} \mathcal{S}_{m,a,b}^{i,j} &= \{(u_1, v_1, w_1, u_2, w_2)^{\text{T}} \in \mathbb{N}_0^5 \mid u_1 \leq m-a, v_1 \leq a-b, \\ &\quad w \leq b, u_2 \leq u_1, w_2 \leq w_1, \\ &\quad u_1 + v_1 + w_1 = i, u_2 + w_2 = j\} \quad . \end{aligned} \quad (9)$$

□

A.2 Segmentation Results

The binary segmentation of the cerebrovascular networks of the test ROIs of datasets \mathcal{D}_{1-4} are compared for the different vessel segmentation approaches in Figures 1-4.

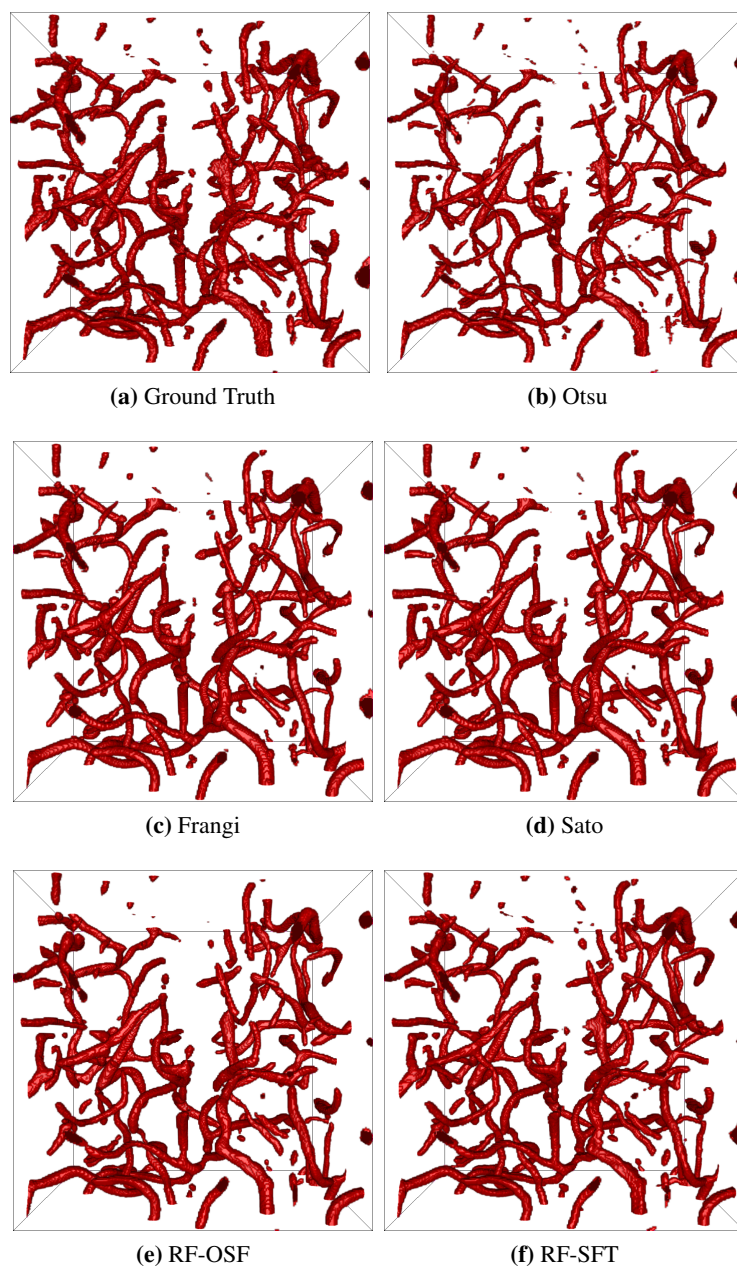


Fig. 1: Segmented cerebrovascular network for whole 3-D test ROI of dataset \mathcal{D}_1 using different segmentation techniques. (a) Ground truth. (b) Otsu's method [4]. (c) Frangi [1]. (d) Sato [5]. (e) RF-OSF ($d = 102$). (f) RF-SFT ($M = 4$). The binary segmentation maps are computed at the corresponding F_1 -optimal operating points.

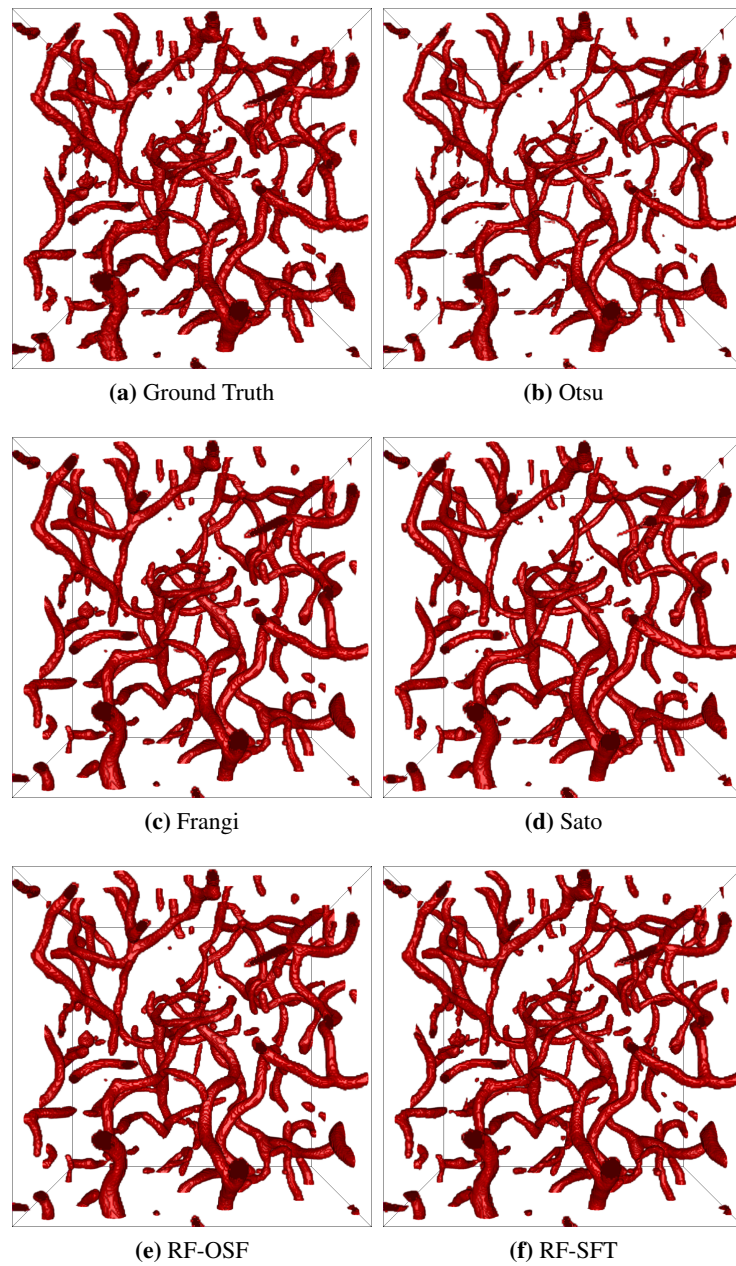


Fig. 2: Segmented cerebrovascular network for whole 3-D test ROI of dataset \mathcal{D}_2 using different segmentation techniques. (a) Ground truth. (b) Otsu's method [4]. (c) Frangi [1]. (d) Sato [5]. (e) RF-OSF ($d = 102$). (f) RF-SFT ($M = 4$). The binary segmentation maps are computed at the corresponding F_1 -optimal operating points.

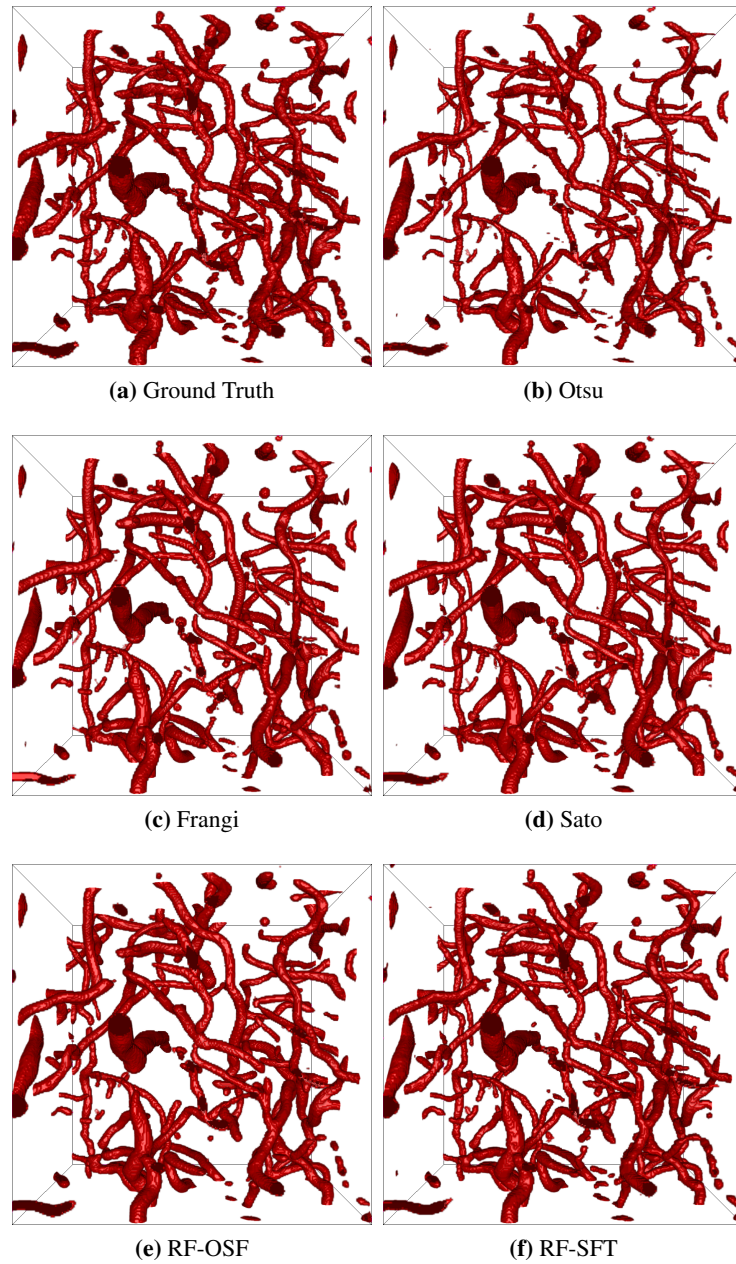


Fig. 3: Segmented cerebrovascular network for whole 3-D test ROI of dataset \mathcal{D}_3 using different segmentation techniques. (a) Ground truth. (b) Otsu's method [4]. (c) Frangi [1]. (d) Sato [5]. (e) RF-OSF ($d = 102$). (f) RF-SFT ($M = 4$). The binary segmentation maps are computed at the corresponding F_1 -optimal operating points.

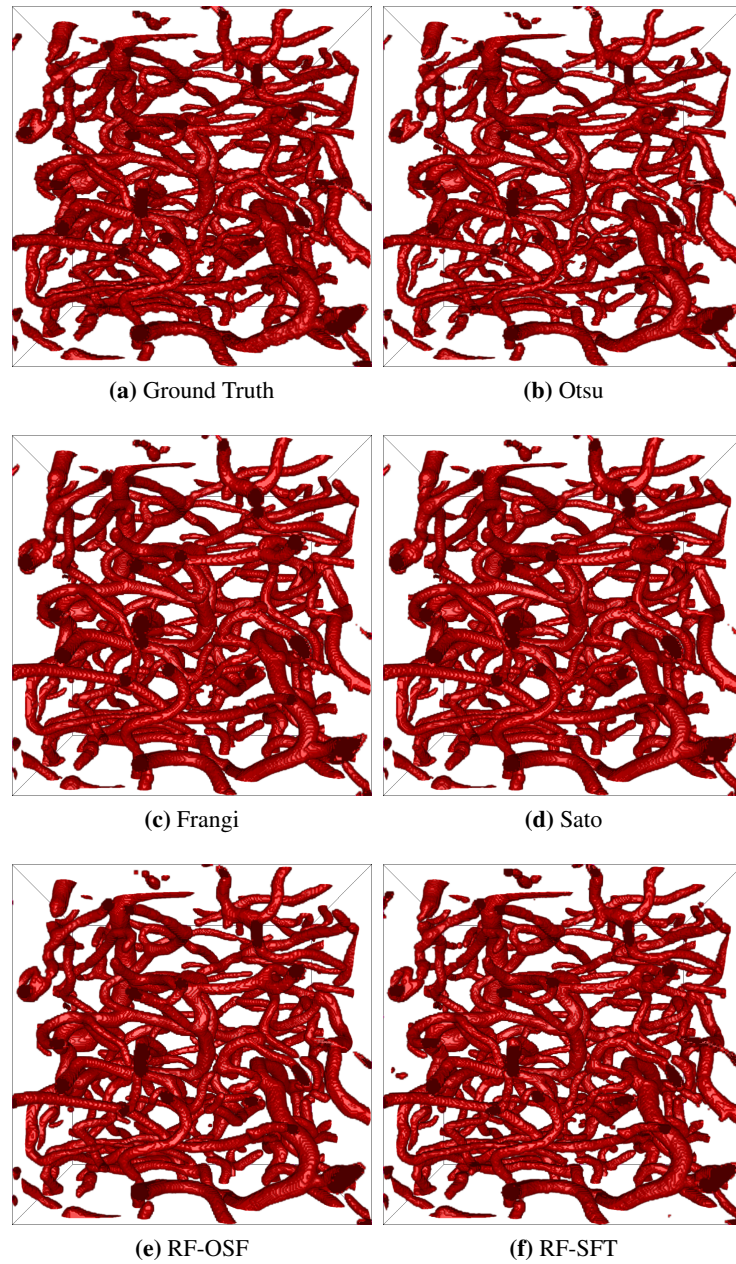


Fig. 4: Segmented cerebrovascular network for whole 3-D test ROI of dataset \mathcal{D}_4 using different segmentation techniques. (a) Ground truth. (b) Otsu's method [4]. (c) Frangi [1]. (d) Sato [5]. (e) RF-OSF ($d = 102$). (f) RF-SFT ($M = 4$). The binary segmentation maps are computed at the corresponding F_1 -optimal operating points.

References

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