



HAL
open science

New ODE Model for Diffusion MRI Signal

Hang Tuan Nguyen, Jing-Rebecca Li, Denis S. Grebenkov

► **To cite this version:**

Hang Tuan Nguyen, Jing-Rebecca Li, Denis S. Grebenkov. New ODE Model for Diffusion MRI Signal. MRPM11, Sep 2012, Surrey, United Kingdom. hal-00764195

HAL Id: hal-00764195

<https://inria.hal.science/hal-00764195>

Submitted on 12 Dec 2012

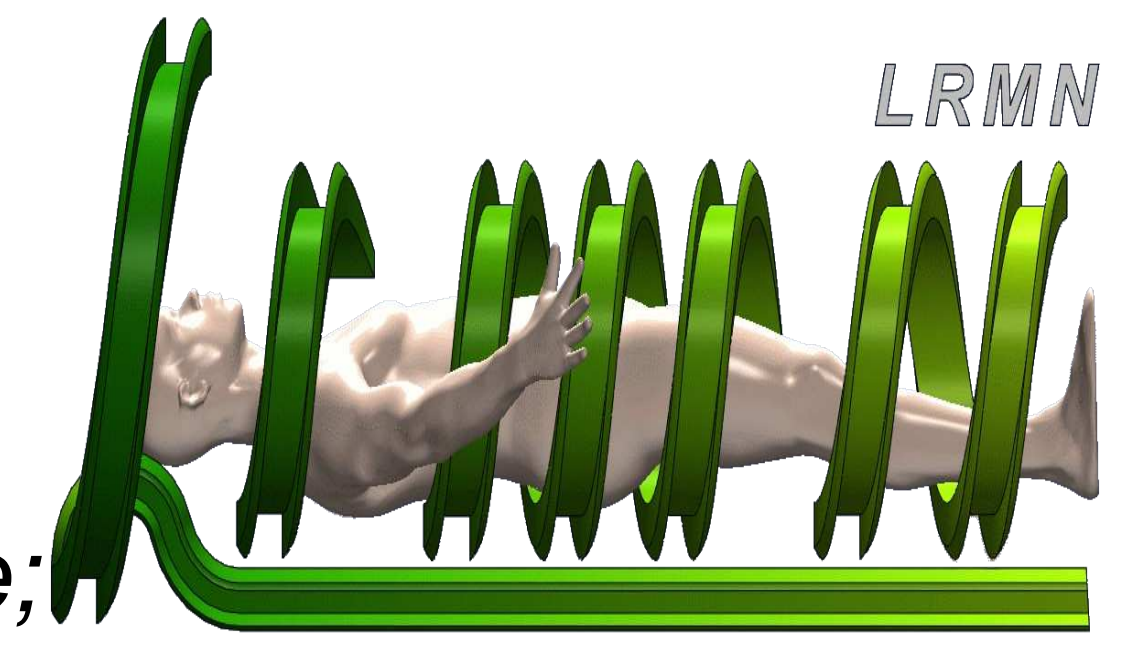
HAL is a multi-disciplinary open access archive for the deposit and dissemination of scientific research documents, whether they are published or not. The documents may come from teaching and research institutions in France or abroad, or from public or private research centers.

L'archive ouverte pluridisciplinaire **HAL**, est destinée au dépôt et à la diffusion de documents scientifiques de niveau recherche, publiés ou non, émanant des établissements d'enseignement et de recherche français ou étrangers, des laboratoires publics ou privés.

New ODE Model for Diffusion MRI Signal

*Hang Tuan Nguyen¹, Jing-Rebecca Li^{1,2} and Denis S. Grebenkov³

¹Neurospin, CEA-Saclay, Gif-Sur-Yvette, France; ²Equipe DEFI, INRIA Saclay Palaiseau, France; ³Laboratoire de Physique de la Matière Condensée, CNRS – Ecole Polytechnique, Palaiseau, France



Introduction

Water diffusion in biological tissues is not Gaussian and signal attenuation is not monoexponential with b-value [1]. Approaches to deal with this behavior include the bi-exponential model [1,2], the Karger model [3], and Kurtosis approach [4]. We formulate an ODE model for diffusion MRI signal that is more general than Karger model, valid for more general diffusion gradient shapes and gives a good approximation to the ADC and Kurtosis. Given DMRI signals before and after cell swelling, we can estimate the amount of cell swelling after numerically solving an ODE system.

New ODE Model

We propose a two-compartment model for the DMRI signal, with Ψ^e and Ψ^i , the signals from the extra-cellular and intra-cellular compartments (Ω^e, Ω^i with effective diffusion coefficients D^e, D^i). The intra-cellular and extra-cellular residence times are τ^i and $\tau^e = \tau^i v^e / v^i$ where v^i and v^e are the volume fractions. Given a diffusion gradient with profile $f(t)$ (where $f(t)$ is anti-symmetric respect to t_d , where t_d is diffusion time) and gradient strength $\vec{g} = \vec{q} / \gamma$ (γ is the gyromagnetic ratio), new ODE model is following:

$$\begin{cases} \frac{\partial \Psi^e(\vec{q}, t)}{\partial t} = -c(t) D^e \|\vec{q}\|^2 \Psi^e(\vec{q}, t) - \frac{1}{\tau^e} \Psi^e(\vec{q}, t) + \frac{1}{\tau^i} \Psi^i(\vec{q}, t) \\ \frac{\partial \Psi^i(\vec{q}, t)}{\partial t} = -c(t) D^i \|\vec{q}\|^2 \Psi^i(\vec{q}, t) - \frac{1}{\tau^i} \Psi^i(\vec{q}, t) + \frac{1}{\tau^e} \Psi^e(\vec{q}, t) \end{cases}$$

subject to initial condition $\Psi^e(\vec{q}, 0) = v^e$ where $c(t) = \left(\int_0^t f(s) ds\right)^2$
 $\Psi^i(\vec{q}, 0) = v^i$

The justification of the time dependent coefficient $c(t)$ is that in a homogeneous medium the total signal satisfies:

$$\frac{\partial}{\partial t} \Psi(\vec{q}, t) = c(t) D \|\vec{q}\|^2 \Psi(\vec{q}, t) \quad . \text{ For PGSE : } c(t) = t^2, 0 \leq t \leq \delta; c(t) = \delta^2, \delta \leq t \leq \Delta; c(t) = (t - \Delta - \delta)^2, \Delta \leq t \leq t_d$$

Measuring Cell Swelling

From DMRI signal, we obtain ADC (apparent diffusion coefficient) and KUR (Kurtosis) which are defined as the first and second order terms of the Taylor expansion in b-value of the logarithm of signal $\Psi(b) = \Psi^e(b) + \Psi^i(b)$:

$$\log \Psi(b) = 0 - ADC * b + KUR * b^2 + O(b^3)$$

where $ADC^{ODE} = v^i D^i + v^e D^e$, KUR can be obtained exactly by numerically solving ODE system or using an approximation:

$$KUR^{ODE} \approx (D^i - D^e)^2 v^i v^e \frac{e^{-k} - (1-k)}{k^2}, k := \frac{\Delta - \delta / 3}{\tau^i v^e}$$

From two DMRI signals, corresponding to times before and after cell swelling, we want to estimate the change in the intra-cellular volume fraction Δv^i . From simulations and experimental data [1] we hypothesized that both τ^i and D^i do not change much with volume fraction changes. Matching ADC and KUR, we search through all possible solution space of τ^i and D^i , then find that only a very small range of τ^i and D^i can give physically reasonable solutions of v^i (between 0-1) and D^e (between $1 \times 10^{-3} \mu\text{m}^2/\mu\text{s}$ and $2 \times 10^{-3} \mu\text{m}^2/\mu\text{s}$) and that within this range of τ^i and D^i , the estimated change in v^i is almost constant. From this, we can compute the change in v^i without knowing the true values of τ^i and D^i .

Results and Conclusion

Two simulated DMRI signals are obtained from PGSE sequences $\delta = 10\text{ms}$, $\Delta = 10\text{ms}$ (or 20ms) (Fig 1) by numerically solving the two-compartment Bloch-Torrey PDE on a sample consisting of 3D convex-shaped cells (Fig 2).

The original volume fraction is $v^i = 0.63$. Reducing the size of the extra-cellular space to obtain $v^i = 0.80$, true swelling is $\Delta v^i = 0.17$. We plot family of v^i and D^i matching the simulated ADC and KUR with expressions obtained from the ODE model. These v^i and D^i (physically reasonable for v^i and D^e) lie on 2 curves $C(v^i, D^i)$ of signals before (blue) and after cell swelling (red) in Fig 3. The difference of 2 curves (black) is an almost constant value of $\Delta v^i = 0.17$ on the entire interval of D^i . In Table 1 we show the average Δv^i for some permeabilities which is close to the true value of 0.17.

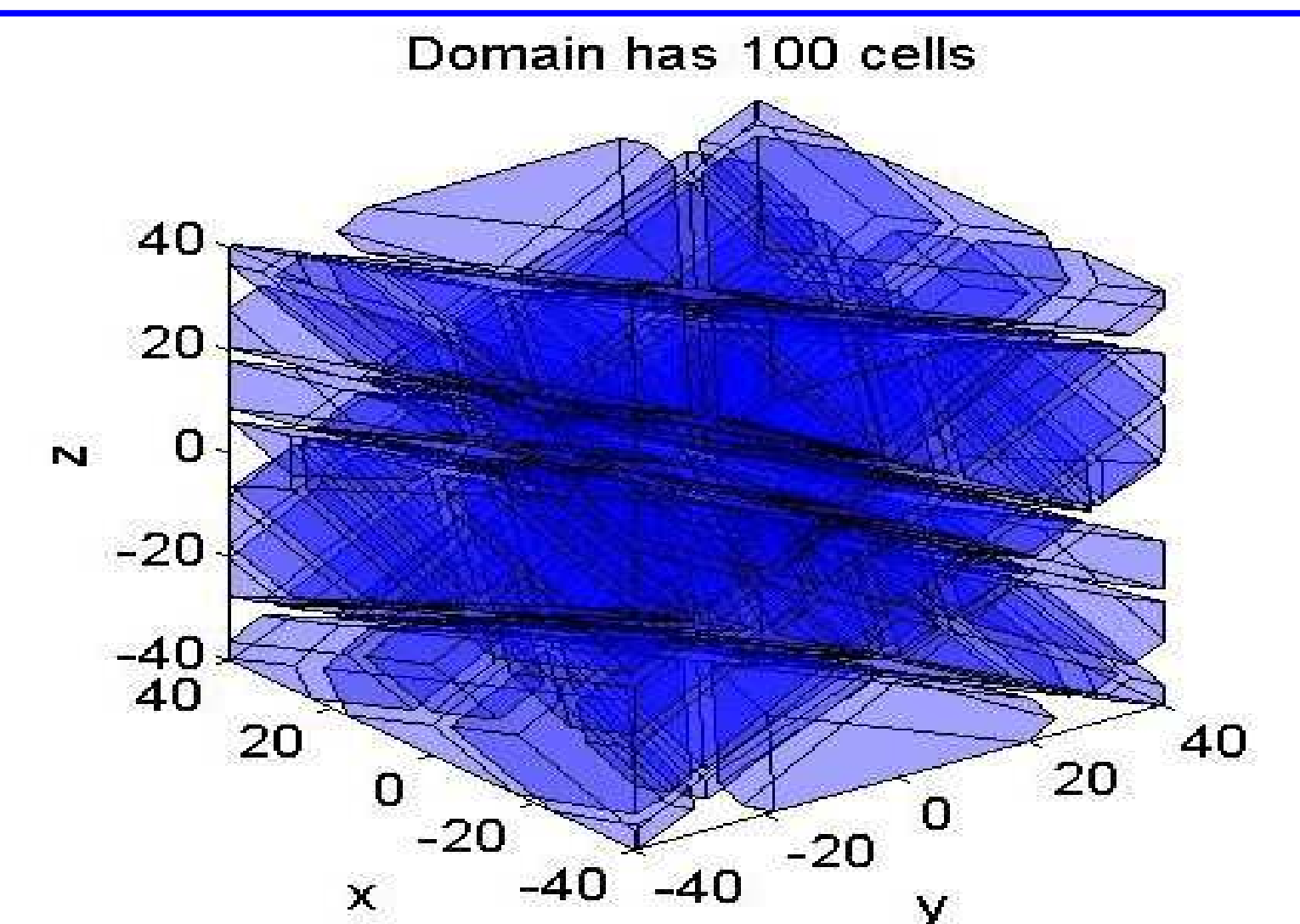
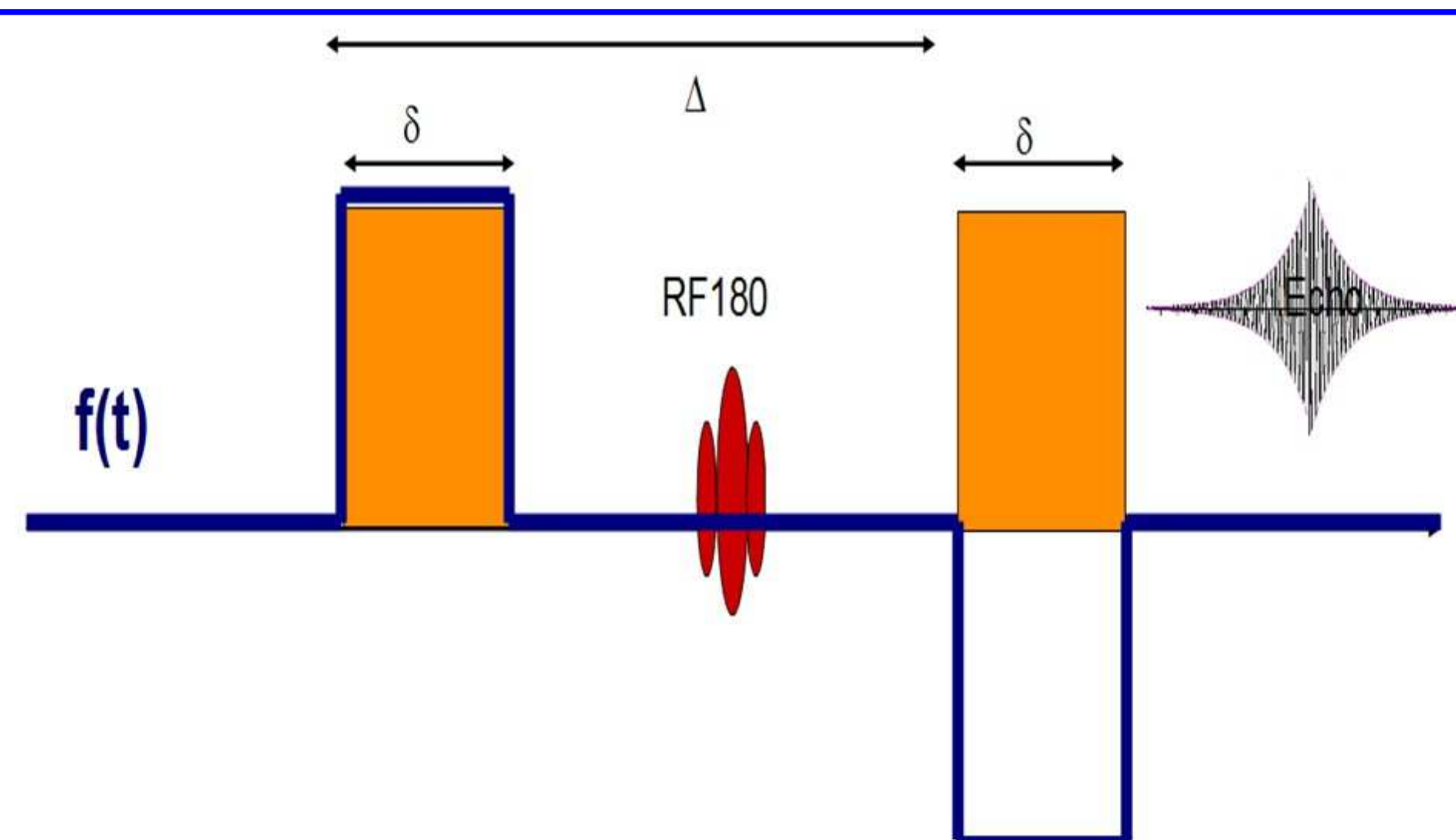


Fig.1 PGSE: $\delta = 10\text{ms}$; $\Delta = 10\text{ms}$ & 20ms

Fig.2 Convex shaped cells $S/V = 1.9/\mu\text{m}$

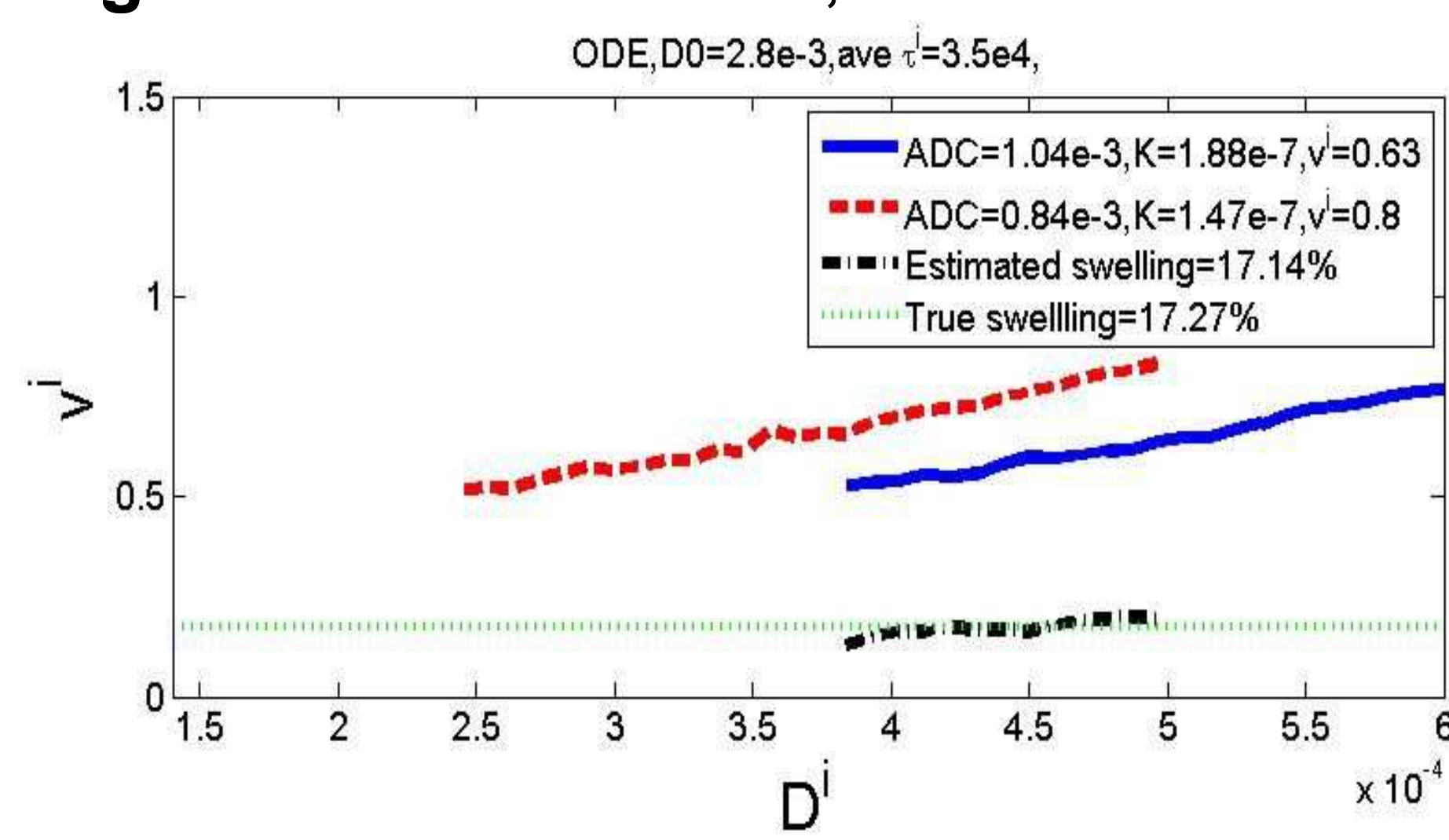


Fig.3 Cell swelling $\Delta v^i = 0.63$ to 0.8

Perm ($\mu\text{m}/\mu\text{s}$)	δ (ms)	Δ (ms)	Estimated Swelling
$\kappa = 5e-6$	10	20	0,16
$\kappa = 1e-5$	10	20	0,17
$\kappa = 5e-5$	10	10	0,14
$\kappa = 1e-4$	10	10	0,16

Table.1 Estimated Δv^i close to true 0.17

References

- [1] Niendorf Th et al. MRM (1996) 36:847-857; Clark C, Le Bihan D. MRM (2000) 44:852-859; [2] Nilsson et al. JMR (2010) 206:59—67; [3] Karger et al. Adv Mag Res (1988) 12:1—89; [4] Jensen et al. NMR Biomed (2010) 23:698—710.